Crystallographic Aspects Regarding the Insertion of Ag⁺ Ions into a Hydroxyapatite Structure

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The objective of this study was to evaluate how silver can be inserted into hydroxyapatite (HA) via two distinct processes: co-doping with CO_3^{2-} via precipitation in an aqueous medium and immersion of preformed HA crystals into Ag⁺ solutions. It was concluded that although Ag⁺ and Ca²⁺ have different radii, the accommodation of Ag⁺ ions in the Ca²⁺ sites of the hydroxyapatite lattice can be explained by the models proposed for inserting monovalent ions such as Na⁺. In this case, because Ag⁺ ions are larger than Ca²⁺ ions and have a different charge, the Ag⁺ ions are stabilized in the HA structure by co-substitution with CO_3^{2-} ions in both the A- and B-type sites. This simultaneous insertion of Ag⁺ and CO_3^{2-} appears to thermally stabilize the HA phase because no phase transformation is observed after calcination. In addition, the doping of HA with Ag⁺ ions can clearly occur via two routes: co-precipitation in the presence of these ions or diffusion in preformed hydroxyapatite crystals. This result appears to indicate the possibility of doping HA with Ag⁺ using less complex routes at ambient temperature and with prefabricated implants or biomaterials, which reduces the costs of producing devices with antibacterial effects.

Keywords: hydroxyapatite, silver, doping, carbonate, diffusion

1. Introduction

In general, pathogenic bacteria survive in colonies called biofilms, which provide protection against antibiotic agents and ensure proliferation of the bacteria. The bacteria in the innermost biofilm tend to receive a lower dosage of antibiotic than those at the biofilm surface, which generates favorable conditions for developing resistance against antibiotics.

Antibiotics have systemic action, are not localized, and can affect all bacteria living in the body, even the non-pathogenic bacteria that have fundamental roles in physiology. Thus, the development of new techniques to combat bacteria has been focused on formulating drugs that can be precisely vectorized to the affected area¹. The association of these drugs with implantable devices through either adsorption or absorption has frequently been considered a method for vectorizing antibiotics to affected areas².

The use of silver as an antibiotic agent is currently experiencing a resurgence in medicine. Silver has been known to possess antibiotic activity since ancient times, and it is a viable alternative to common antibiotics because it has a broad spectrum of activity toward different types of bacteria³. The use of silver, even in small quantities⁴, provides a strong antibiotic effect that accelerates the efficacy of treatments. The use of silver is economically feasible compared to the costs for producing a new antibiotic or for modifying an existing one. Problems related to chemical and thermal stability, denaturation, and storage conditions make common antibiotics considerably more complex in terms of synthesis and handling than silver and its compounds. Consequently, several attempts have been made to associate silver and its compounds with biomaterials and implantable devices⁴⁻⁶.

Implantable devices composed of hydroxyapatite (HA), particularly those used in ostomies, are constantly exposed to bacteria, which can use these devices as body-invasion gateways. Thus, HA doped with silver or containing silver nanoparticles has been proposed as a method to reduce or avoid such contamination. However, the introduction of silver into an apatite structure can generate crystalline defects, which can lead to substantial thermal instability. In most cases, after thermal treatments of doped HA at high temperatures, phase transformations and the formation of less biocompatible phosphates and even calcium oxide, which are toxic to cells, occur.

Sygnatowicz et al.⁷ observed a phase transformation in an HA that contained 5-10 wt% Ag⁺, along with the formation of β -tricalcium phosphate (β -TCP), after calcination at 800 °C and 900 °C. Other studies also demonstrated the formation of this phase for various Ag⁺ concentrations^{8,9}. In most cases, the decrease in Ag⁺ concentration corresponds to a smaller phase transformation.

Recent reports in the literature indicate the possibility of achieving a thermally stable HA using a co-doping process, where ions with different sizes and charges are inserted into the apatite lattice. Silva et al.¹⁰ demonstrated that Sr-containing HA could be thermally stabilized by simultaneously inserting Na⁺, Cl⁻ and CO₃²⁻ into the apatite lattice. Similarly, Moreira et al.^{11,12} demonstrated that simultaneously adding Mg²⁺, Mn²⁺ and Sr²⁺ ions into the apatite lattice stabilized the crystal and prevented phase transformations after calcination at 1000 °C. Aina et al.¹³ showed that Mg²⁺ or Sr²⁺-doped apatites exhibited a phase transformation after thermal treatment, whereas the samples that contained both Mg²⁺ and Sr²⁺ did not.

Kumar et al.¹⁴ observed that inserting both Zn²⁺ and CO₃²⁻ into the apatite structure diminished the formation of TCP phases after calcination at 1300 °C compared to the insertion of only Zn²⁺. The vacancies generated by the replacement of PO₄³⁻ groups with CO₃²⁻ (different charges) were compensated by the replacement of Ca²⁺ with Zn²⁺ (different sizes). Similarly, Mostafa et al.¹⁵ investigated the co-doping of HA with Na⁺, CO₃²⁻ and SiO₄⁴⁻. They demonstrated that the simultaneous introduction of Na⁺ and CO₃²⁻ could stabilize the structure, thereby preventing phase transformations, even at 1100 °C.

These studies demonstrated that inserting ions of different sizes and charges into HA could compensate for the structural stress caused by inserting a single type of ion. Thus, a method to insert ions that present stability problems into the HA structure, such as silver, is the co-doping process.

Accordingly, understanding how Ag⁺ ions can be stabilized in the HA lattice is essential for proposing appropriate mechanisms to manufacture implantable devices that are resistant to bacteria without reducing the biocompatibility caused by possible phase transformations. Thus, the objective of this study is to understand how Ag⁺ ions can be introduced into the HA structure using two methods: HA co-precipitation in the presence of Ag⁺ and CO₃⁻² and diffusion of Ag⁺ ions into preformed HA crystals.

2. Materials and Methods

2.1. Hydroxyapatite synthesis

Hydroxyapatite (HA) was synthesized using the precipitation method in an aqueous medium through a typical acid-base reaction between calcium hydroxide $[Ca(OH)_2]$ and phosphoric acid $[H_3PO_4]$ at concentrations of 0.198 and 0.119 mol /L, respectively. The acid solution was added dropwise (2.0 mL/min) to the basic solution under constant agitation. The pH value was monitored and maintained at 10 or greater during the reaction. The synthesis of the control was performed using potassium hydroxide (KOH). The temperature was maintained at 37 °C throughout the entire synthesis. The obtained suspension was aged under the same temperature and pH conditions for 24 hours. Subsequently, the suspension was filtered and washed with distilled water until the supernatant was neutral (pH \approx 7). The precipitate was dried at 120 °C for 24 hours.

The Ag⁺-doped HA was synthesized following an identical procedure. However, silver nitrate (AgNO₃) was added to phosphoric acid to obtain a final Ag⁺ concentration

of 2.5×10^{-4} mol/L. In both cases, the atmosphere was not controlled to allow free insertion of CO_3^{2-} into the HA structure.

The obtained HA powders were calcined at 1000 °C for 2 hours with a heating rate of 2.8 °C/min to determine their thermal stability at high temperature.

2.2. Ag⁺ diffusion in hydroxyapatite crystals

A suspension of pure HA (without Ag^+) was prepared using a 0.1 mol/L silver nitrate solution. This suspension was constantly stirred at 23 °C for 1, 24, 48 and 70 hours. After each time period, the suspension was filtered and washed with distilled water to remove soluble ions. The obtained powder was dried at 120 °C for 24 hours.

2.3. Composition

The synthesized samples were analyzed using wavelengthdispersive X-ray fluorescence (WDXRF) to identify the present elements and their quantity. The powders were pressed without adding boric acid to create pellets, which were analyzed directly using a WDXRF spectrometer (Bruker, Tiger S8).

The CO₃²⁻, PO₄³⁻ and OH⁻ groups were observed using Fourier transform infrared spectroscopy (FTIR). The changes in these groups were followed by calculating the relative area under the curves (deconvolution). All the curves were normalized by the intensity of the vibrational mode v_4 PO₄ at 572 cm⁻¹. The analyses were conducted in absorbance mode from 4000 to 400 cm⁻¹ (step size of 4 cm⁻¹) using a Perkin-Elmer (Spectrum BX) spectrometer.

2.4. Crystalline structure

The samples were characterized before and after calcination using X-ray diffraction (XRD) to identify the crystalline phases and possible structural and morphological changes induced by the Ag⁺ doping. The XRD patterns were obtained under the following conditions: $\theta/2\theta$ of 5-60°, continuous scan (2°/min), step size of 0.02° and radiation generated at 40 kV/40 mA ($\lambda_{COKa} = 1.7902$ Å). The analyses were performed using a RIGAKU DMAX 100 diffractometer.

2.4.1. Lattice parameters

The *a* and *c* lattice parameters and cell unit volume were calculated using the Rietveld method for structure refinement and a convolution-based approach for the profile fitting, which was implemented using X'Pert HighScore Plus software. CIF files corresponding to the JCPDS cards HA: 9-432; α -TCP: 29-0359; β -TCP: 9-169; Ag₃(PO)₄: 6-505; Ag: 4-783; CaO: 37-1497, were used in the structure refinement.

2.4.2. Crystallite size and asymmetry

The crystallite size (L) was estimated using the Scherrer equation¹⁶ considering the ($0 \ 0 \ 2$) plane of HA according to the following equation:

$$L = \frac{0.89\lambda}{B_{hkl}\cos\theta} \tag{1}$$

where λ is the incident radiation wavelength (nm); B_{*HKL*} is the full width at half maximum (FWHM), which was corrected by subtracting from that measured using the main

diffraction peak of LaB₆ (under identical conditions); and θ is the diffraction angle that corresponds to the (0 0 2) plane for K α Co.

The asymmetry of the crystal was determined from the relation between the peak intensities that corresponded to the $(2 \ 0 \ 0)$ and $(0 \ 0 \ 3)$ planes, *i.e.*, the $[1 \ 0 \ 0]$ and $[1 \ 0 \ 0]$ directions, respectively.

2.4.3. Crystal morphology after immersion in Ag⁺ solution

The HA powder after immersion in the Ag⁺ solution was analyzed using transmission electron microscopy (TEM) in a JEOL 2000FX microscope operated at 200 kV to evaluate possible changes in the crystal morphology of HA.

3. Results and Discussion

3.1. Doping by co-precipitation

3.1.1. Vacancy formation

Quantitative analyses using wavelength-dispersive X-ray fluorescence (WDXRF) enabled us to determine the quantities of Ag, Ca and P in the samples (Table 1). The obtained Ca/P ratio in the HA sample was consistent with the expected value for a stoichiometric hydroxyapatite (1.67). However, the inclusion of Ag⁺ (HA-Ag) slightly increased the value of (Ag+Ca)/P to 1.69. If we consider that Ag⁺ ions can only occupy the positive Ca²⁺ sites, the necessary charge balance to maintain the neutrality of the HA structure is compromised. In this case, the entry of other ions with different charges may be facilitated during crystal growth to restore neutrality.

 Table 1. Relative quantities of the elements in the samples, which were measured using WDXRF.

Sample	Composition (mol %)			$(C = 1 A = /\mathbf{D})$
	Ca	Р	Ag	- (Ca+Ag/P)
HA	13.81	8.27	-	1.67
HA-Ag	14.54	8.61	0.1	1.69

It is known that the inclusion of monovalent ions such as Na⁺ can generate favorable conditions to accommodate $CO_3^{2^-}$ in $PO_4^{3^-}$ sites¹⁷. This accommodation restores the neutrality of the solid and can also explain the increase in the (Ag+Ca)/P ratio because the quantity of $PO_4^{3^-}$ in the structure is reduced.

Because the synthesis atmosphere was not controlled in our experiments, CO_2 from the air was free to be inserted into the HA structure as $CO_3^{2^2}$. Indeed, the precipitation method for producing HA in aqueous media tends to promote the dissolution of CO_2 and the consequent insertion of $CO_3^{2^2}$ into the HA structure¹⁸⁻²⁰ when it is performed under alkaline conditions at low temperatures.

Vignoles²¹ proposed a model to describe the structure of a hydroxyapatite containing Na⁺ and CO_3^{2-} :

$$Ca_{10-X} Na_{2X/3} V^{Na}_{X/3} (PO_{4})_{6-X} (CO_{3})_{X} (H_{2}O)_{X} (OH)_{2-X/3} V^{OH}_{X/3}$$
(2)

where $0 \le x \le 3$

In this model, the insertion of a monovalent ion such as Na⁺ in the Ca²⁺ sites simultaneously generates the conditions for inserting CO₃²⁻ ions and produces vacancies in the pairs (Na⁺/OH⁻). There are reports in the literature that demonstrate that the OH⁻ infrared absorption bands decrease when the Na⁺ concentration increases in HA structures²²⁻²⁴.

Fourier transform infrared spectroscopy (FTIR) analyses allowed us to verify the typical HA groups in all samples. A zoom scan in the region of 660-540 cm⁻¹ revealed details from the OH⁻ and PO₄³⁻ group vibrations (Figures 1 and 2). Prior to calcination, the insertion of Ag⁺ caused the intensity of the OH⁻ bands to decrease (Figure 1). The relative area under the FTIR curves v_LOH/v₄PO₄ calculated from HA and HA-Ag were 0.59 and 0.52, respectively. After calcination, there was no significant difference between the intensities of the OH⁻ and PO₄³⁻ bands (Figure 2). The relative area under the curves v_LOH/v₄PO₄ calculated from HA and HA-Ag were 0.96 and 0.97, respectively. Therefore, one can assume that the intensities of the OH⁻ bands of HA-Ag samples decrease prior to calcination because OH⁻ vacancies are generated. Accordingly, the Vignoles model that describes the structure



Figure 1. Zoom scanning of the FTIR spectra for the vibration regions related to the OH⁻ and PO_4^{3-} groups, which were obtained from the HA (a) and HA-Ag (b) samples prior to calcination.

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of a Na⁺-doped HA is also suitable for explaining the occupation of the Ca^{2+} sites by Ag⁺ ions in HA structures. Thus, assuming this model and considering the molar amount of Ag⁺ measured with WDXRF in our experiment, we obtain the following chemical formula:

$$Ca_{9,9} Ag_{0.07} V^{Ag}_{0.03} (PO_{4})_{5,9} (CO_{3})_{0.1}$$

$$(H_{2}O)_{0.1} (OH)_{1.97} V^{OH}_{0.03}$$
(3)

3.1.2. Occupation of A and B sites for CO_3^{2-}

If we observe in detail the region of CO_3^{2-} absorption groups (v_2 C-O), there is an adjustment problem with the last model (vacancy formation). The bands in the region of 871-880 cm⁻¹ confirmed the insertion of CO_3^{2-} at both the B-type sites (PO₄³⁻) and at the A-type sites (OH⁻) for the HA-Ag samples prior to calcination (Figure 3). The absorption bands were distributed between the two regions, indicating the presence of CO_3^{2-} at both sites. In fact, the relative area under the FTIR curves calculated from HA and HA-Ag (v₂CO₃-A/v₂CO₃-B ratio) were 0.423 and 0.425, respectively.

After calcination, these bands disappeared from the spectra, which suggests that the heat treatment can remove the majority of $CO_3^{2^2}$ groups from the HA structure (Figure 4).

Fleet & Liu²³ proposed a model to describe HA doped with monovalent cations such as Na⁺, which considers the occupation of B- and A-type sites by CO_3^{2-} groups at the same time:

$$Ca_{10-y}Na_{y}[(PO_{4})_{6-y}(CO_{3})_{y}][(OH)_{2-2x}(CO_{3})_{x}]$$
 (4)

Using the quantities of Ag⁺, Ca²⁺ and PO₄³⁻ that were calculated in our work using WDXRF, and assuming the v_2CO_3 -A/ v_2CO_3 -B ratio obtained from FTIR curves we propose the following chemical formula:



Figure 2. Zoom scanning of the FTIR spectra for the vibration regions related to the OH⁻ and PO_4^{3-} groups, which were obtained from the HA (a) and HA-Ag (b) samples after calcination at 1000 °C/2 h.



Figure 3. Zoom scanning of the FTIR spectra for the vibration regions related to the $CO_3^{2^\circ}$ groups, which were obtained from the HA (a) and HA-Ag (b) samples prior to calcination.

$$Ca_{9,9}Ag_{0,1}[(PO_{4})_{5,9}(CO_{3})_{0,1}][(OH)_{1,8}(CO_{3})_{0,04}]$$
 (5)

In both aforementioned models^{21,23}, the Ag/(Ag+Ca) ratio indicates that approximately 0.7% of the Ca²⁺ ions were replaced by Ag⁺ ions. The (Ag+Ca)/P ratio is 1.69, as calculated using WDXRF. However, this latest model does not consider the formation of vacancies in Na⁺/OH⁻ pairs that can justify the reduction in the OH⁻ infrared absorption bands, which was observed in our HA-Ag sample prior to calcination (Figure 1). Nevertheless, in this latest model, the reduction in OH⁻ groups is equivalent to the amount of monovalent



Figure 4. Zoom scanning of the FTIR spectra for the vibration regions related to the CO_3^{2-2} groups, which were obtained from the HA and HA-Ag samples after calcination.

cations that were added into the HA structure. Therefore, the observed reduction in the OH⁻ infrared absorption bands in the HA-Ag sample can be adequately explained by the replacement of these groups by CO_3^{2-} groups.

In addition, a question arises: why did the intensity of the OH⁻ infrared absorption bands of the samples not decrease after calcination?

3.1.3. CO₃²⁻ release

To answer the last question, it is necessary to recall that the release of CO_3^{2-} groups from the structure of a carbonated HA generates CaO as a byproduct²⁰. When the CO_3^{2-} groups replace the PO_4^{3-} groups, the excess Ca^{2+} ions tend to react with oxygen to form CaO at temperatures above 600°C.

The release of CO_3^{2-} from an A- and B-type carbonated HA, such as that obtained in our work, can be described according the following reaction:

$$\begin{array}{l} \operatorname{Ca}_{10-\gamma}\operatorname{Ag}_{\gamma}[(\operatorname{PO}_{4})_{6-\gamma}(\operatorname{CO}_{3})_{\gamma}][(\operatorname{OH})_{2-2\chi}(\operatorname{CO}_{3})_{\chi}] \to \\ (1-\gamma/6)\operatorname{Ca}_{10}(\operatorname{PO}_{4})_{6}(\operatorname{OH})_{2} + (x+\gamma)\operatorname{CO}_{2} + \gamma\operatorname{CaO} + \gamma\operatorname{Ag} \end{array}$$
(6)

After CO₃²⁻ is released from the HA structure, the excess Ca²⁺ tends to form CaO, the inserted silver tends to form metallic silver^{9,25}, and the remainder generates a stoichiometric hydroxyapatite. Thus, after calcination, the vibrational modes from OH⁻ groups may be remarkably enhanced because of the better lattice organization and release of CO₃²⁻ from the structure. Indeed, the main peak that corresponds to the (2 0 0) plane of CaO (d = 0.2405 nm) (ICDD 37-1497) is not observed in the X-ray diffraction pattern of HA (Figure 5), but it is found in HA-Ag after calcination (Figure 6). The Rietveld results indicated the presence of 0.9 wt.% of CaO. However, the presence of metallic silver could not be



Figure 5. X-ray diffraction pattern of the HA sample after calcination at 1000 $^{\circ}$ C/2 h. Only the hydroxyapatite phase (HAp) was identified by Rietveld refinement. The residue generated from the refinement is show in the graphic (bottom).

determined because the main peak that corresponds to its $(1 \ 1 \ 1)$ plane was absent (d = 0.2359 nm) (ICDD 4-0783). One can assume that the low quantity of Ag⁺ did not enable the generation of a significant amount of metallic silver to be detected in the experimental conditions of this work. This result can also indicate that Ag⁺ ions were confined in the HA structure even after calcination.

To support this latest hypothesis, it is necessary to assume another CO_3^{2-} release model that can consider the formation of only Ag-doped hydroxyapatite and CaO. Thus, we can rewrite the decarbonation reaction as follows:

$$\begin{array}{l} \operatorname{Ca}_{10-y}\operatorname{Ag}_{y}[(\operatorname{PO}_{4})_{6-y}(\operatorname{CO}_{3})_{y}][(\operatorname{OH})_{2-2x}(\operatorname{CO}_{3})_{x}] \rightarrow \\ (1-y/6)\operatorname{Ca}_{10-y}\operatorname{Ag}_{y}(\operatorname{PO}_{4})_{6}(\operatorname{OH})_{2} + (x+y)\operatorname{CO}_{2} + y\operatorname{CaO} \end{array}$$
(7)

If this model is correct, Ag^+ ions that are inserted into the HA structure should change the lattice parameters of HA because Ag^+ ions (0.128 nm) have a different size and charge from Ca^{2+} ions (0.099 nm) for identical coordination numbers.

The XRD analyses indicated that HA was formed in all samples (Figures 5 and 6). The three most intense peaks in the diffractograms correspond to the (2 1 1), (1 1 2) and (3 0 0) planes, which are typical for HA. For the pure HA, no phase transformation was observed after calcination. If one considers the FTIR results of the HA prior to calcination, in which the presence of A- and B-type carbonated HA are observed in similar quantities, the only method to produce a stoichiometric HA after calcination is the generation of Ca²⁺ vacancies in identical proportions to the PO₄³⁻ that is replaced by CO₃²⁻, which will maintain the HA stoichiometry (Ca/P = 1.67) even after the release of CO₃²⁻ from the structure. Therefore, the model proposed by Vignoles²¹ can be used to describe this behavior:

Counts

$$Ca_{10-X+U}V^{Ca}_{X-U}(PO_{4})_{6-X}(CO_{3})_{X}[(OH)_{2-X+2U-2Y} (CO_{3})_{Y}V^{OH}_{X-2U+Y}$$
(8)

where (0 < x < 2), (0 < 2u < x) and (0 < y < 2-x+2u)

In this case, to have the quantity of Ca^{2+} vacancies notably close to the amount of PO_4^{3-} replaced by CO_3^{2-} , the value of *u* must tend to zero. Therefore, the release of CO_3^{2-} is described as follows:

$$Ca_{10-X+U}V^{Ca}_{X-U}(PO_{4})_{6-X}(CO_{3})_{X}[(OH)_{2-X+2U-2Y} (CO_{3})_{Y}V^{OH}_{X-2U+Y} \rightarrow (1-y/6)Ca_{10}(PO_{4})_{6}(OH)_{2} + (9) (x+y)CO_{3} + uCaO$$

This mechanism can properly explain the observations from both the FTIR and XRD analyses. In fact, the obtained lattice parameters of HA after calcination were similar to those observed for a standard hydroxyapatite (Table 2). In addition, the lattice parameters of HA-Ag exhibited a slight increase in the *a* and *c* axes relative to the pure HA.

3.1.4. Structural changes

Rameshbabu et al.⁵ and Badrour et al.⁶ reported that the insertion of Ag⁺ into the HA structure occurred preferentially at the Ca I site, which is the only site in which Ca²⁺ ions are

Table 2. Comparison between the lattice parameters calculated by Rietveld refinement for the synthesized samples after calcination at $1000 \text{ }^{\circ}\text{C/2}$ h.

Sample	Lattice parameters				
Sample	а	b	с	V(Å ³)	
HA	9.4070	9.4070	6.8722	526.64	
HA-Ag	9.4072	9.4072	6.8730	526.70	



Figure 6. X-ray diffraction pattern of the HA-Ag sample after calcination at 1000 °C/2 h. The phases hydroxyapatite (HAp) and calcium oxide (CaO) were identified and quantified by Rietveld refinement. The residue generated from the refinement is show in the graphic (bottom).

confined among the rigid PO_4^{3-} tetrahedral groups. In contrast, according to Singh et al.⁹, Ag⁺ ions tend to be incorporated more easily into Ca II sites. In this case, the insertion of Ag⁺ is favored by the mobility of the bond between Ca²⁺ and hydroxyl groups in the HA channels. The accommodation of Ag⁺ ions in the Ca II sites causes the unit cell to expand, which is directly related to the increase in the *a* and *c* lattice parameters. If we consider that the CO₃²⁻ ions are completely eliminated after calcination (as suggested by the FTIR data), the increase in the *a* and *c* lattice parameters observed is directly associated with the insertion of Ag⁺ ions into the HA lattice. The slight change in the *a* and *c* observed in this work could be explained by the small quantity of Ag⁺ replacing Ca²⁺. In fact, less than one Ca²⁺ was replaced by Ag⁺ ions in a unit cell.

The Rietveld analysis of the respective diffraction pattern included the refinement of the occupancy parameters for the Ca sites, which could be occupied by Ca and Ag atoms under the stoichiometric constraints in the HA phase. The result of the refinement confirmed the Ag atoms in the HA phase, as the replacement of Ca by Ag in the HA phase indeed improved the goodness of fit indices.

The presence of Ag⁺ ions in the HA structure slightly decreases the crystallite size of the samples prior to calcination (Figure 7). After calcination, the crystals grow in a similar method, regardless of the presence of Ag⁺ ions. The asymmetric nature of these crystals, i.e., their tendency to grow in a preferential direction, was measured. Prior to calcination, the pure HA exhibited more elongated crystals than the HA-Ag samples, which suggests that the insertion of CO_3^{2-} ions induces a preferential crystal growth in the c direction (Figure 8). Simultaneously, the insertion of Agions reduced this growth in the c direction and generated conditions to produce more spherical crystals. It is known that the insertion of CO₃²⁻ into the B-type sites of HA can decrease the (h k 0) distances and increase the (0 0 l) distances. The opposite behavior is observed when CO₂²⁻ ions are placed in the A-type sites^{20,26,27}. However, these distortions are much more remarkable when CO₃²⁻ is confined in the hydroxyl channels of HA, which may explain the behavior observed in this work.

According to Hwang et al.²⁷, the limit distance of Ag^+ diffusion is notably short in HA, which can induce its presence only on the crystal surface depending on the type of synthesis. In our case, the Ag^+ ions were present in the solution during the entire synthesis, which leads us to conclude that this ion is not confined on the surface. Furthermore, if the Ag^+ ions were confined only on the crystal surfaces, the crystal asymmetry might be significantly changed, which was not detected here.

3.2. Doping by ion-exchange

To evaluate the diffusion of Ag^+ ions in previously formed HA crystals, we immersed a pure HA into a solution containing Ag^+ . The obtained transmission electron microscopy images allowed us to confirm the presence of nano electro-dense clusters on the HA crystal surface, which may be related to a Ag^+ -rich phase (Figure 9). After 1 hour of immersion, elongated HA crystals was observed without many electro-dense agglomerates. After 24 hours, the amount of agglomerates



Figure 7. Crystallite size calculated from the X-ray diffraction patterns of the samples before and after calcination.



Figure 8. Crystal asymmetry calculated from the X-ray diffraction patterns of the samples before and after calcination.

increased, and they were homogeneously distributed on the HA crystals. The agglomerate size increased until 70 hours, when the particle morphology became notably different from the originally observed morphology.

According to the X-ray diffraction patterns of the HA samples and the Rietveld refinement after 1, 24, 48 and 70 h of immersion, a new crystalline phase of Ag_3PO_4 (ICDD 06-0505) was formed on the original HA crystals (Figure 10), which suggests that the Ag^+ ions reacted with the PO_4^{3-} groups on the surface to form the new Ag_3PO_4 phase. Even within 1 hour of immersion, some Ag_3PO_4 clusters were observable in the samples.

The changes in the crystal morphology of HA during immersion, which were revealed using transmission electron microscopy, suggest that the Ag⁺ ions were not confined only



Figure 9. TEM images showing the HA crystals, which were covered with electron-dense clusters after immersion in a $AgNO_3$ solution for 1 (a), 24 (b), 48 (c) and 70 h (d). Bar = 200 nm.



Figure 10. X-ray diffraction patterns of the HA samples after immersion for 1, 24, 48 and 70 h in a silver nitrate solution. Hydroxyapatite (HAp) and silver phosphate (Ag_3PO_4) phases were identified and quantified by Rietveld refinemet.

on the surface. To evaluate the possible insertion of Ag^+ ions into the HA structure as a function of the immersion time, the lattice parameters were calculated from the Rietveld refinement for each immersion time. The results indicated that the immersion for 1 hour was sufficient to remarkably change the *a* and *c* lattice parameters compared to the original HA (Figure 11). After this time, the values remained almost constant until 70 h. Therefore, we conclude that Ag^+ ions can be inserted into the HA lattice either during the synthesis in the presence of these ions or by ionic diffusion from an aqueous solution that contains Ag^+ , which allows us to propose less complex routes for doping hydroxyapatite implantable devices with Ag^+ and avoid phase transformation problems at high temperatures.



Figure 11. Changes in the lattice parameters of the HA after immersion in a silver nitrate solution for 1, 24, 48 and 70 h.

4. Conclusion

Despite having different radii, the accommodation of Ag^+ ions in the Ca^{2+} sites of the hydroxyapatite lattice can be explained by the models proposed for inserting

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monovalent ions such as Na⁺. In this case, because Ag⁺ ions are larger than Ca²⁺ ions and have different charges, Ag⁺ ions are stabilized in the HA structure because of a co-substitution with $CO_3^{2^-}$ ions in both the A- and B-type sites. This simultaneous insertion of Ag⁺ and CO₃²⁻ appears to thermally stabilize the HA phase because no phase transformation was observed after calcination. In addition, hydroxyapatite can be doped with Ag⁺ ions using two routes: co-precipitation in the presence of these ions or diffusion in preformed hydroxyapatite crystals. This result appears to indicate the possibility of doping HA with Ag⁺ using less complex routes at ambient temperature and with prefabricated implants or biomaterials to reduce the production costs of devices with antibiotic action.

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