

# THE CORRELATION BETWEEN DEXA AND CDEXA METHODS IN BONE MINERAL ABSORPTIOMETRY\*

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**Abstract** **OBJECTIVE:** To study the interchangeability of the bone mineral density results between Hologic® dual energy x-ray absorptiometry (DEXA) and Cromox® computed dual energy conventional x-ray absorptiometry (CDEXA) equipments. **MATERIALS AND METHODS:** Thirty-eight femoral necks and 31 lumbar spines of 43 patients underwent bone mineral density measured by both equipments in a diagnostic imaging center. The Cromox® equipment was calibrated with a reference Cromox® phantom for bone absorptiometry. **RESULTS:** A strong correlation between results obtained from the two devices was found for each skeletal site. The linear correlation coefficient measured for the right femoral neck was  $r = 0.920$ ,  $p < 0.0001$ , and  $r = 0.923$ ,  $p < 0.0001$  for the lumbar spine L2-L4 vertebrae. Considering the relevance of the  $T_{score}$  result in the clinical practice for bone densitometry, the mean difference of the  $T_{score}$  between devices was calculated, resulting in an arithmetic mean  $\Delta T_{score} = 0.191$  for hips and an arithmetic mean  $\Delta T_{score} = 0.228$  for the lumbar spines. The skeletal status is established according to the World Health Organization definition as normal, osteopenia or osteoporosis. The skeletal status concordance between devices was higher than 76% for hips and higher than 77% for spines; and higher than 96% when considering concordance in at least one of the two sites. **CONCLUSION:** The linear correlation coefficients obtained are very close to the international references among gold standard devices, reported as  $r > 0.95$ . For both sites, the arithmetic mean difference in  $T_{score}$  between devices is low – lower than the least significant variance.

**Keywords:** Dual energy x-ray absorptiometry; Dual energy radiographic absorptiometry; Computed x-ray densitometry; Correlation; Interchangeability.

**Resumo** *A correlação de métodos DEXA e CDEXA em absorptimetria mineral óssea.*

**OBJETIVO:** Estudar a intercambiabilidade dos resultados de densidade mineral óssea entre máquinas de absorptimetria de raios-x em duas energias (DEXA) Hologic® e de absorptimetria computadorizada de raios-x convencionais em duas energias (CDEXA) Cromox®. **MATERIAIS E MÉTODOS:** Para 38 casos de quadril e 31 casos de coluna lombar avaliados em 43 pacientes atendidos em um centro de diagnóstico por imagem, medidas de densidade mineral óssea foram realizadas em ambas as máquinas. A máquina Cromox® foi calibrada usando-se o *phantom* Cromox® de referência para absorptimetria óssea. **RESULTADOS:** Forte correlação entre os resultados obtidos nas duas máquinas foi encontrada para cada sítio do esqueleto. O coeficiente de correlação linear medido para o colo femoral direito foi  $r = 0,920$ ,  $p < 0,0001$ , e  $r = 0,923$ ,  $p < 0,0001$  para as vértebras L2-L4 da coluna lombar. Como o resultado expresso em  $T_{score}$  é importante na prática clínica em densitometria óssea, a diferença média em  $T_{score}$  entre as máquinas foi calculada, resultando em média aritmética de  $\Delta T_{score} = 0,191$  para o quadril e média aritmética de  $\Delta T_{score} = 0,228$  para a coluna. Estado esquelético é estabelecido de acordo com a definição da Organização Mundial da Saúde como normal, osteopenia ou osteoporose. A concordância de estado esquelético entre as máquinas foi superior a 76% para o quadril e superior a 77% para a coluna, e superior a 96% quando se considerou concordância em ao menos um dos dois sítios. **CONCLUSÃO:** Os coeficientes de correlação linear obtidos são muito próximos das referências internacionais entre máquinas padrão-ouro, reportados como  $r > 0,95$ . Para ambos os sítios, a diferença média aritmética em  $T_{score}$  entre as máquinas é pequena, menor que a menor variação significativa.

**Unitermos:** Absortimetria de raios-x em duas energias; Absortimetria radiográfica em duas energias; Densitometria por raios-x computadorizada; Correlação; Intercambiabilidade.

## INTRODUCTION

Dual energy x-ray absorptiometry (DEXA) is a technique widely utilized for measuring mass and bone mineral density (BMD). Computed dual energy conventional x-ray absorptiometry (CDEXA) is different from DEXA in the way x-rays absorption data acquisition is performed,

but the mathematical algorithms utilized for absorptiometry data processing are similar.

The CDEXA system present some interesting features as follows: higher spatial resolution and smaller area for locating the equipment as compared with DEXA systems; native images, allowing a radiological analysis to offer reliable densitometric

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data; lower total investment allowing a more disseminated and comprehensive use in the population; estimated radiation doses of 1.3 mSv and 2.6 mSv, respectively, for hip and spine assessment, and a probable increase in the diagnostic specificity, considering the feasibility of an individualized radiological analysis. It is necessary to know if results obtained for subjects with the CDEXA system may be reliably interchanged with results for the same subjects with a DEXA device, as previously done for comparison between absorptiometry techniques<sup>(1,2)</sup>.

The present study was aimed at comparing lumbar spine and femoral neck BMD measurements with these devices in a populational sample, regardless race/ethnicity, gender, age, body weight, or clinical status, to investigate the performance relation between both devices in a full-operational condition.

## MATERIALS AND METHODS

DEXA studies were performed with a Hologic<sup>®</sup> QDR 4500C apparatus, and CDEXA studies, with a Cromox<sup>®</sup> CXD 3.2.1 system, calibrated with a Cromox<sup>®</sup> reference phantom for bone absorptiometry.

According to Blake et al.<sup>(3)</sup>, the DEXA technology performs the scanning of the site in analysis, recording the x-ray beam power with dual kilovoltage components. This recording is performed by a solid-state sensor which detects the transmitted radiation and transfers the corresponding digital value into a computer, generating two image matrices corresponding to the two photon energies. The mathematical treatment of absorptiometry data is performed through the analysis of two transmission equations for each pixel of the double image matrix of the site of interest, one equation for each of the two x-ray beam kilovoltages. For each photon energy, an equation with exponential relation between attenuation and transmitted radiation energy is converted into a linear equation by application of a logarithmic function. Once the relation between the soft tissues attenuation coefficients for both energies is defined, and once the bone mineral component attenuation coefficients for both ener-

gies are known, the two resulting linear equations present only two unknown magnitudes corresponding to the densities per area of bone mineral component and soft tissues. The resolution of the linear algebraic system defines the two densities per area on each pixel of the image matrix. The integration in area of density of the bone mineral component, followed by the division of the integrated value by the total area, results in the BMD arithmetic mean of the site evaluated.

According to the manufacturer's information, the CDEXA technology also provides the two image matrices by exposure of the site analyzed by x-ray beams to two photon energies, through the operation of the bulb with two kilovoltages. The radiation beam energy is recorded on conventional radiographic films. Aiming at controlling variations both in the characteristics of the bulb emission and films chemical processing, calibration metal phantoms are submitted to radiological exposure simultaneously with the patient. The transference of absorptiometry data into the computer is made by means of radiographic films digitization by a scanner with solid-state sensors, which catch the luminosity transmitted and transfer the corresponding values into the computer, constructing two image matrices corresponding to the photon energies. The values of these image matrices are adjusted according to the phantoms response to radiation, so the absorptiometry data are corrected for a pattern of x-ray emission. The manufacturer informs that the mathematical treatment of the absorptiometry data is performed as previously described for the DEXA technique, until the BMD arithmetic mean for the site analyzed is obtained.

According to Steel et al.<sup>(4)</sup>, the effective radiation doses to the patient, in fan beam DEXA for studying hip and lumbar spine, are respectively 56  $\mu$ Sv and 59  $\mu$ Sv, and may reach 74,7  $\mu$ Sv, according to Maher<sup>(5)</sup>. With the CDEXA technology, where the images acquisition is made on conventional radiographic films, the estimated effective radiation doses for the hip and lumbar spine assessment are respectively 1.3 mSv and 2.6 mSv. This estimation is made because the CDEXA technique re-

quires two images from each site (generated in two kilovoltages), and the typical, individual effective dose for acquisition of lumbar spine images is 1.3 mSv, according to the U.S. Food and Drug Administration<sup>(6)</sup>, resulting in an effective radiation dose of 2.6 mSv for lumbar spine evaluation. The dose required for generation of a hip image corresponds to 50% of the dose required for lumbar spine, so the total effective radiation dose for hip assessment is 1.3 mSv.

The comparison between the absorptiometry techniques has taken into consideration the results of density/area in gram units of bone mineral component/cm<sup>2</sup> of the lumbar spine (L2 to L4 vertebrae) and right femoral neck. The anteroposterior projection was adopted for lumbar spine assessment; and for the proximal femur, the orthogonal projection (the usual positioning for bone densitometry) achieved by means of 30° internal rotation of the foot was adopted.

According to the manufacturer's information, the Cromox<sup>®</sup> reference phantom for bone absorptiometry (Figure 1) includes four plates of oven-dried bovine bone specimens with regular thickness, whose mass and area were measured by the metrology laboratory of Instituto de Pesquisas Tecnológicas (IPT) in São Paulo, SP, Brazil. The specimens were kept in the oven for drying until their mass presented a



**Figure 1.** Cromox<sup>®</sup> reference phantom in bone absorptiometry constructed with bone specimens measured in the IPT metrology laboratory, and utilized for Cromox<sup>®</sup> devices calibration.

variation of less than 1% along an eight-hour interval. The drying process was completed in 50 hours. The mass/area ratio provides a bone density in g/cm<sup>2</sup> for calibration of absorptiometry results.

Forty-three volunteers, with no distinction of race/ethnicity, gender, age, body weight or clinical status, who had accepted the terms of agreement to participate in the present study, were evaluated during the period between March/2003 and June/2003. The patients were included in the study regardless their clinical or physical status, since the study was aimed at comparing the performance of the two equipment units under adequate operational conditions for achievement of reliable results. For the right hip, the patients' ages ranged between 48 and 84 years (mean and standard deviation = 63.0 ± 9.5), while for the lumbar spine, ages ranged between 48 and 79 years (mean and standard deviation = 60.4 ± 8.6). Forty-one pairs of results for right hip and 32 pairs for lumbar spine were obtained by the DEXA and CDEXA systems, however not all the patients contributed with results for both sites (hip and lumbar spine).

The rejection criteria adopted for exclusion of pair of results of BMD measurements by both equipment units were: a) site thickness (abdominal or coxofemoral) > 24 cm; b) interference from soft tissues: excess of gas on the lumbar spine vertebrae or overlapping of abdominal fat and femoral neck; c) results clearly non-compatible with the radiological evaluation of the site, in any of the equipment units. Additionally,

excess of gas on the Cromox<sup>®</sup> metal phantom, inherent to the CDEXA method, was considered as a rejection criterion. Once these criteria were applied, two pairs of results for hip affected by soft tissues interference (overlapping of abdominal fat and femoral neck), one pair of results clearly non-compatible with the radiological evaluation of the hip, and one pair of results of hip where the presence of excessive gas on the lumbar vertebrae was observed were excluded from the study, and the remaining 38 pairs of results for hip, and 32 pairs of results for lumbar spine were compared by regression analysis. However, some discrepancies in the positioning of the patients on both devices were observed (lack of strict observance of the 30° for internal rotation of the foot, as well as the lumbar spine alignment was not strictly reproduced). Despite the known influence of clothing elastic bands, feces and little abdominal gas on densitometry results, data from many patients have not been included since these items were not considered as rejection criteria. These occurrences may affect the correlation of results obtained by both equipment units.

Montgomery's<sup>(7)</sup> regression and linear correlation techniques were utilized for statistical data analysis calculated by supplementary regression and correlation macros<sup>(8)</sup> with Microsoft Excel and Statistic Analysis System (SAS) applications<sup>(9)</sup>, and tested by Gauss and Markov mathematical models assumptions of independence, normality and null hypothesis rejection.

## RESULTS

The comparison between BMD measurements with both densitometry devices is shown on Figure 2 for the femoral neck, and Figure 3, for the lumbar spine.

For the femoral neck, the linear regression function for the group ( $n = 38$ ,  $t$ -Student distribution) is:

$$BMD_{CDEXA} = 0.326 + 1.105 BMD_{DEXA} \quad (1)$$

where:  $BMD_{CDEXA}$  and  $BMD_{DEXA}$  are, respectively, the BMD values measured by CDEXA and DEXA; the correlation coefficient for femoral neck is  $r = 0.920$ ,  $p < 0.0001$ . The data distribution and the regression line are shown on Figure 2.

For the lumbar spine, the linear regression function for the group ( $n = 31$ ,  $t$ -Student distribution) is:

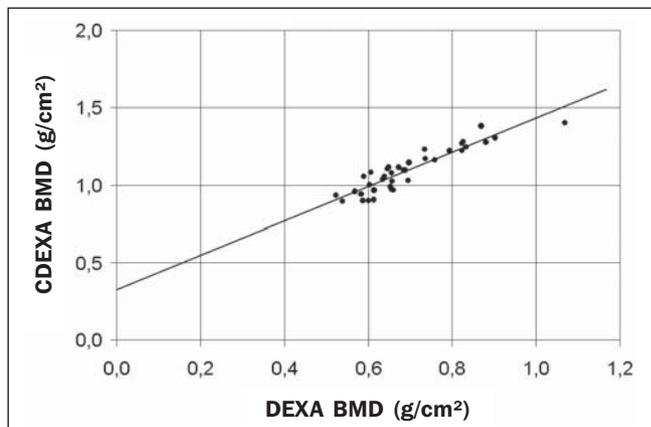
$$BMD_{CDEXA} = -0.025 + 1.616 BMD_{DEXA} \quad (2)$$

where the correlation coefficient is  $r = 0.923$ ,  $p < 0.0001$ . The data distribution and the regression line are shown on Figure 3.

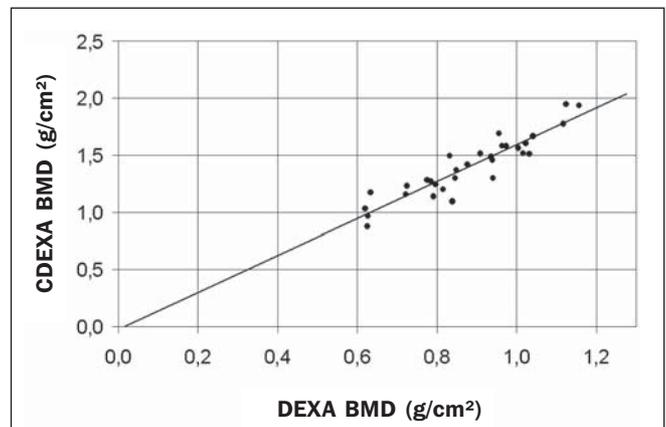
In the clinical practice, the results expressed as  $T_{score}$  are significant for evaluating bone densitometry studies, since the publication of the World Health Organization (WHO) Study Group report, according to Blake et al.<sup>(3)</sup>. The  $T_{score}$  adimensional parameter is defined by the equation:

$$T_{score} = (BMD \text{ measured} - \text{mean BMD in young adults}) / \text{young adults SD} \quad (3)$$

where: young adults SD is the standard deviation for the young adults population.



**Figure 2.** Comparison between BMD measurement of femoral neck by DEXA and CDEXA systems. The regression line is shown with  $r = 0.920$ ,  $p < 0.0001$ ,  $BMD_{CDEXA} = 0.326 + 1.105 \times BMD_{DEXA}$ .



**Figure 3.** Comparison between BMD measurement of lumbar spine by DEXA and CDEXA systems. The regression line is shown with  $r = 0.923$ ,  $p < 0.0001$ ,  $BMD_{CDEXA} = -0.025 + 1.616 \times BMD_{DEXA}$ .

Even if there is a BMD correlation,  $T_{score}$  measured in both systems are compatible only if the values for mean BMD in young adults and young adults SD are appropriate, these reference values for young adults for both systems being obtained from their respective results reports. The mean BMD calculation in young adults corresponds to the BMD/young adults percentage ratio in the site, while the young adults standard deviation corresponds to the BMD difference/mean BMD in young adults/ $T_{score}$  ratio in the site. For each site, the value obtained for each of these parameters is the respective arithmetic mean among the whole group results.

The arithmetic mean of the  $T_{score}$  difference ( $\Delta T_{score}$  arithmetic mean) is calculated for the group, the  $\Delta T_{score}$  adimensional parameter being defined as:

$$\Delta T_{score} = T_{score\ CDEXA} - T_{score\ DEXA} \quad (4)$$

and calculated for each patient, resulting in a  $\Delta T_{score}$  arithmetic mean = 0.0191 for the femoral neck and  $\Delta T_{score}$  arithmetic mean = 0.228 for the lumbar spine.

The  $\Delta T_{score}$  graphic representation is shown on Figure 4 for the femoral neck and Figure 5 for the lumbar spine, where the patients are indexed 1 to 38 (hip group), and 1 to 31 (lumbar spine group).

Aiming at investigating how the results provided by both devices can agree as regards the classification of the patient's skeletal status according to the WHO criteria, as normal, osteopenia and osteoporosis, as

reported by Blake et al.<sup>(3)</sup>, the results for each site were compared through the skeletal status parameter (SkS):

$$\begin{aligned} \text{SkS} &= \text{normal, when } T_{score} \geq -1.00 \\ \text{SkS} &= \text{osteopenia, when } T_{score} < -1.00 \text{ and } \\ &\quad T_{score} \geq -2.50 \\ \text{SkS} &= \text{osteoporosis, when } T_{score} < -2.50 \end{aligned} \quad (5)$$

Agreement as regards skeletal status is defined as the same skeletal status classification for results obtained by both systems for a same patient, according to the mentioned mathematical criterion. Based on this definition, agreement as regards skeletal status was found in 76.3% of pairs of results for hips ( $n = 38$ ), and in 77.4% for lumbar spine ( $n = 31$ ). It is important to note that some pairs of BMD results present differences of decimals or centesimals of  $T_{score}$  unit, but they are sufficient for determining different skeletal status.

Another alternative method for evaluating agreement as regards skeletal status is considering the results of a same skeletal status obtained in both devices for a same patient and for at least one of the sites evaluated. In this case, agreement as regards skeletal status was found in 96.2% of pairs of results for hips and/or lumbar spine of the 26 patients submitted to measurements of both sites.

**DISCUSSION**

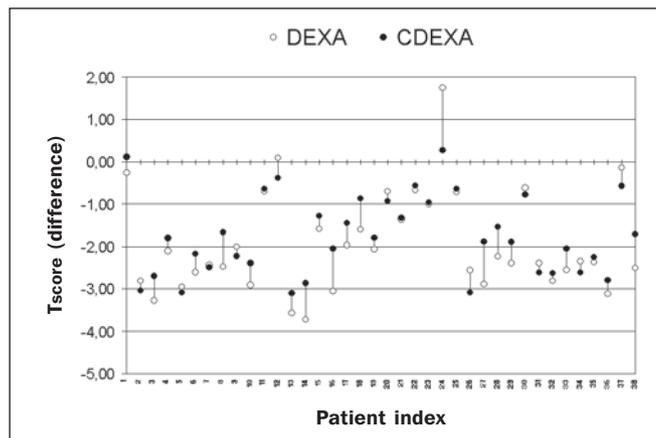
BMD results were linearly correlated with  $r = 0.920$  for femoral neck and  $r =$

0.923 for lumbar spine, similarly to the correlation coefficient  $r \geq 0,95$  reported by Faulkner et al.<sup>(10)</sup> in a comparison between DEXA Lunar and Hologic systems. Statistically, a correlation coefficient  $> 0.9$  is very significant, expressing a small dispersion for results obtained in both devices for the same patients. Therefore, measurements performed in a device may be obtained in the other with small mean statistical differences. The correlation occurs at the same level both for hip and lumbar spine, since the correlation coefficients for both sites are very similar. This means that the significant correlation between the two methods is non-specific for the other site.

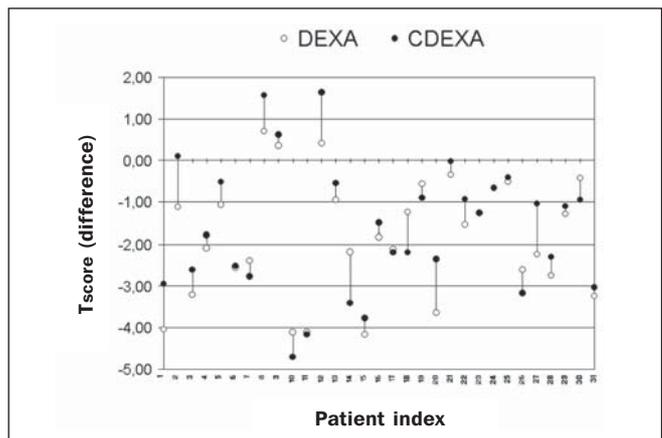
The  $\Delta T_{score}$  arithmetic means for hip and lumbar spine are very low, and not statistically significant, since these values correspond to a BMD variation lower than the least significant change (LSC) which is the lower BMD variation considered as statistically significant according to the International Society for Clinical Densitometry (ISCD). Using the algorithm offered by the ISCD<sup>(11)</sup>, the LSC is determined for each device and for each site. For the CDEXA device, with 30 pairs of results, the LSCs were 0.088 g/cm<sup>2</sup> for hip, and 0.123 g/cm<sup>2</sup> for lumbar spine, resulting in  $\Delta T_{score\ LSC} = 0.39$  for hip, and  $\Delta T_{score\ LSC} = 0.62$  for lumbar spine., according to the equation:

$$\Delta T_{score\ LSC} = \text{LSC} / \text{young adults SD} \quad (6)$$

According to the same algorithm, the LSC corresponds to 2.77 times the variance



**Figure 4.** Graphic visualization of  $T_{score}$  and  $\Delta T_{score}$  for femoral neck demonstrates little differences in  $T_{score}$  between DEXA and CDEXA results ( $\Delta T_{score}$  arithmetic mean = 0.191), except for some few cases, probably because of operational errors like ROI variations and patients positioning (internal rotation of the foot).



**Figure 5.** Graphic visualization of  $T_{score}$  and  $\Delta T_{score}$  for lumbar spine demonstrates little differences in  $T_{score}$  between DEXA and CDEXA results ( $\Delta T_{score}$  arithmetic mean = 0.228), except for some few cases, probably because of variations in the abdominal gas and feces distribution and L2 to L4 vertebrae alignment.

coefficient (VC) at 68% confidence level. for the DEXA system, VC = 1.8% is reported by Blake et al.<sup>(3)</sup>, allowing the calculation of the LSC for each site, resulting in  $\Delta T_{score\ LSC} = 0.45$  for the hip, and  $\Delta T_{score\ LSC} = 0.49$  for the lumbar spine, by means of the equation (6). The  $\Delta T_{score}$  arithmetic mean = 0.191 for the femoral neck and  $\Delta T_{score}$  arithmetic mean = 0.228 for the lumbar spine are lower than  $\Delta T_{score\ LSC}$  values for these sites in both systems, that is to say, they are sufficiently low to consider as adequate the interchangeability between  $T_{score}$  results found through both systems.

Figures 4 and 5 show constant, very little differences in  $T_{score}$ , except for some few cases of patients with indices 14, 16, 24 and 27 for hip, and patients with indices 2, 12, 14, 20 and 27 for lumbar spine. For these cases, the not so little differences in  $T_{score}$  probably occur as a result of operational errors such as variation in the definition of regions of interest (ROIs) and patient positioning (internal rotation of the foot, for the hip), variations in abdominal gas and feces distribution, and vertebrae L2 to L4 alignment (for the lumbar spine). In CDEXA devices, the inaccuracy of lumbar spine results because of the presence of abdominal gas and feces may be minimized if the images are rejected upon visual inspection of the radiographs, and the patient is submitted to a new radiographic exposure after appropriate intestinal preparation.

The skeletal status parameter is introduced for the understanding of the interchangeability between the two methods in the clinical practice, since the first clinical interpretation of densitometry results is performed according to the WHO definitions. Considering the strictness of the WHO classification as regards status transition (normal/osteopenia,  $T_{score} = -1.00$ ;

osteopenia/osteoporosis,  $T_{score} = -2.50$ ), an eventually non-elevated level of agreement is expected, even in comparisons between results from the same device, as a function of results deviation because of the device accuracy. With results classified according to the WHO categorization for each site, agreement as regards skeletal status does not occur for 24% of patients who had their hips evaluated, and for 23% of patients who had their lumbar spine evaluated. The agreement rate increases as the results are non-specifically classified for each site, i.e., considering as agreement as regards skeletal status the agreement in at least one of the two sites evaluated. Agreement as regards skeletal status is not found in only 4% of the patients evaluated by both systems when at least one of the two sites (hip or lumbar spine) is considered.

For conversion of BMD values measured by CDEXA into DEXA scale, the appropriate equation obtained by linear regression for the femoral neck group is:

$$BMD_{DEXA} = -0.143 + 0.767 BMD_{CDEXA} \quad (7)$$

with  $p < 0.0001$ , while for the lumbar spine group the appropriate equation is:

$$BMD_{DEXA} = 0.143 + 0.527 DMO_{CDEXA} \quad (8)$$

with  $p < 0.0001$ .

However, there is a necessity for additional studies involving a higher number of cases and with a more strict control over patients positioning and definition of ROI in the software for BMD measurement by both equipment units to evaluate the correlation between the devices when submitted to tests with a higher reproducibility of operational procedures.

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ing technical information and license for utilization of the software during the study, allowing the processing of paired densitometric studies and those performed in the Hologic<sup>®</sup> QDR 4500C system owned by the author. The present study has been developed as a previous condition for the evaluation and acquisition of the Cromox<sup>®</sup> CXD 3.2.1 system by the author.

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