ABSTRACT

PURPOSE: To develop an experimental model for incisional hernias and to compare morphological and functional aspects of hernia repairs by suture, polypropylene mesh and collagen mesh.

METHODS: A defect measuring 7cm x 2cm was created in the anterior abdominal of 28 New Zealand male rabbits, divided into four groups (n = 7): (1) control, (2) suture of the anterior sheath of the rectus abdominal muscle, (3) setting of polypropylene mesh, and (4) setting of collagen mesh. On the 90th postoperative day, the animals were examined to verify the presence of incisional hernia. Samples of abdominal wall and scar were collected for histological study.

RESULTS: Incisional hernia was identified in 85.7% of the control group, 57.1% of the suture group, 42.9% of the collagen mesh group, and none in the polypropylene mesh group (p = 0.015). Mesh exposure could be identified in 71.4% of the animals in group 3 and in no animal in group 4 (p = 0.021). The polypropylene mesh is effective in the treatment of abdominal wall defects, causing an intense inflammatory reaction.

CONCLUSION: The collagen mesh is biocompatible, producing a minimal inflammatory reaction, but fails in the treatment of abdominal wall defects.

Key words: Hernia, Ventral. Surgical Mesh. Polypropylenes. Collagen. Rabbits.
Introduction

The incisional hernia consists of the protrusion of ofalls, through orifices or abdominal wall, abnormally weakened by congenital defects or traumas and surgical procedures. Suture repair is commonly ineffective, with reports of recurrence in 25% to 52% of cases; however, the use of mesh has decreased this recurrence to a rate of less than 10%.

The use of prostheses in fascial-defect repair has resulted in reduction of the recurrence of abdominal wall hernias. Recent data from a study on prospective, random, and controlled suture repair versus prosthetic implant revealed much better results when mesh was used. Analysis of a population demonstrated that the prostheses implant, increased from 35% in 1987 to 66% in 1999. The American Hernia Society defined the use of mesh as a standard procedure in incisional hernia repair. The setting of the mesh allows for the stress-free restoration of the structural integrity of the abdominal wall. Advantages for the use of mesh include its availability, non-dependence on integrity, as well as the resistance of the patient’s tissues. The ideal material for the implant must be atoxic, non-immunogenic, and non-reactive, aimed at using the implant and incorporating it within the surrounding tissues. The risk of infection of the mesh and enteric fistulas limit its use. The development of substances combining non-absorbable, absorbable material and biological materials is of utmost importance in an attempt to reduce the complications related to the mesh and to restore the functions of the abdominal wall.

Advances in tissue engineering technology have led to the development of biomaterials derived from human and animal tissues. These materials differ amongst themselves, as they act through a regenerative process. For those based on collagen, the extra-cellular matrix is preserved, which allows for the maintenance of the mechanical integrity, while supplying a substrate for the regeneration of the host tissue. These materials have shown a resistance to infection, tolerance to cutaneous exposure, and mechanical stability, when used in incisional hernia repair. The disadvantages include their high cost and the lack of long-term comparative studies.

The knowledge of the anatomic and physiological structure of the abdominal wall is necessary for success concerning incisional hernia repair. Relapse after mesh repair is rarely caused by an intrinsic flaw in the prosthetic material, as it is more commonly related to the non-identification of the healthy fascia and the poor setting of the mesh, frequently leading to recurrence in the fascia interface with the mesh. In view of this gap in the literature, this present study aimed to employ an experimental incisional hernia model to compare morphofunctional aspects of repairs by means of direct suture, polypropylene or collagen mesh.

Methods

This work was carried out in accordance with that recommended by the International Standards for the Protection of Animals and the Brazilian Animal Experimentation Code (1988), and was approved by the Committee of Ethics in Animal Experimentation, Universidade Federal University de Minas Gerais, protocol number 098/2011.

Twenty-eight New Zeland male rabbits, three months of age and with weights of above two kilograms, acquired from the Experimental Veterinary Farm were studied. All of the rabbits were identified and placed in the Biotherapy of the School of Medicine, one animal per cage. They received rations for rabbits and filtered water ad libitum.

The rabbits were anesthetized with an intramuscular injection in the gluteal region of 5% ketamine hydrochloride (Ketamin-S® (+), Cristália, Itapira-SP) at a dose of 35 mg/kg (0.7 ml/kg), coupled with 2% xylazine hydrochloride (Rompun®, Bayer, Sao Paulo-SP) at a dose of 6 mg/kg (0.3 ml/kg). When necessary, half of the initial dose of the anesthesia was applied. During the entire period of anesthesia, the heartbeats and respiration were observed, as were the voluntary movement of the rabbits, in an attempt to detect complications.

After the trichotomy of the abdomen, antisepsis was carried out, using a 2% degerming chlorhexidine solution followed by a 70% alcohol and the setting of surgical fields. A defect measuring 7cm x 2 cm was created in the ventral abdominal wall with removal of a muscle-aponeurotic sheaf, using single card template for all animals. The defect was closed at the same time. The rabbits were divided into four groups by a random drawing (n=7):

- Group 1: Control – only a skin suture with no reconstruction of the abdominal wall;
- Group 2: Anterior sheath suture of the abdominal rectus muscle with a continuous 3-0 monofilament polypropylene suture;
- Group 3: Setting of polypropylene mesh, 10 cm x 4 cm on the borders of the anterior sheath of the abdominal rectus muscle, with a 3-0 monofilament polypropylene suture (Figure 1A).
- Group 4: Setting of the polymerized and purified type I collagen mesh, 10 cm x 4 cm, on the borders of the anterior sheath of the abdominal rectus muscle, with a 3-0 monofilament polypropylene suture (Figure 1B).
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After the surgery and during the entire follow-up period, the rabbits received rations and filtered water *ad libitum*, and were kept in individual cages, under appropriate conditions of hygiene, ventilation and natural illumination.

Before being killed, the animals were evaluated by means of ectoscopy (aspect of the surgical wound area, with the animal in orthostatism) to verify the presence of incisional hernia.

At the end of the follow-up period, on the 90th post-operative day, the animals were killed with an intramuscular injection of 3 ml of 19.1% potassium chloride, after an intramuscular injection of 3 ml of ketamine hydrochloride (50 mg/ml).

A laparotomy in U, released a quadrangular portion of the abdominal wall, to study the incisional hernia and to evaluate the repairs. The removed abdominal wall was then prepared for histological study and stained with hematoxylin and eosin (HE) and Masson trichrome staining. The microscopic evaluation with HE staining was performed to quantify the foreign body gigantic cells, polymorphonuclear (PMN) cells, and mononuclear (MN) cells. Masson’s staining was performed in groups 3 and 4, to characterize the collagen fibers in a qualitative manner.

The analyses were performed using R, version 2.7.1, and Epi Info, version 6.04, softwares, both of public domains. The variable categorical responses were compared with the overall group by means of contingency tables to which the Fisher exact test was applied. To make a comparison between the weight and the groups, the F test was used (ANOVA), given that the supposition of normality was verified by the Shapiro-Wilk test. The comparisons between the two to two groups were performed using the Tukey *post hoc* method. The values were considered significant for *p*<0.05.

**Results**

All of the animals recovered spontaneously from the surgeries and survived the three-month experiment. The incisional hernia was identified in 100% of the rabbits from the control group, in 57.1% from the suture repair group, and in 42.9% from the biological mesh group (Table 1). No rabbit from the polypropylene mesh presented incisional hernia (*p*=0.015).

No difference in the presence of abscesses among the groups could be observed. Mesh exposure could be identified in 71.4% of the animals from group 3 and in no animal from group 4 (*p*=0.021). Therefore, it could be observed that mesh exposure and the group are in fact associated, with the rabbits which received a polypropylene mesh closure exhibiting a greater chance of presenting mesh exposure than those which received the biological mesh closure (Table 1).

**TABLE 1** – Comparison among the control, suture repair, polypropylene mesh, and collagen mesh groups concerning the percentage of the incidence of mesh exposure and incisional hernia.

<table>
<thead>
<tr>
<th>mesh exposure and incisional hernia</th>
<th>Mesh exposure</th>
<th>Incisional hernia</th>
</tr>
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<tbody>
<tr>
<td>Control</td>
<td>-</td>
<td>100%</td>
</tr>
<tr>
<td>Suture repair</td>
<td>-</td>
<td>57.1%</td>
</tr>
<tr>
<td>Polypropylene mesh</td>
<td>71.4%</td>
<td>0%</td>
</tr>
<tr>
<td>Collagen mesh</td>
<td>0%</td>
<td>42.9%</td>
</tr>
</tbody>
</table>

*1 p = 0.015;  *2 p = 0.021

The present study highlighted a greater proportion of rabbits from the control group with a zero count in the average PMN number (100%), as well as greater proportions from the suture repair, polypropylene mesh, and biological mesh groups concerning PMN numbers with average counts of higher than 10 (71.4%, 71.4%, and 57.1%, respectively) (*p*=0.043). All of the rabbits from the control and polypropylene mesh groups presented more than 10 monocytes. By contrast, all of the rabbits from the suture groups presented from 1 to 5 monocytes, while 28.6% of...
the rabbits from the biological mesh closure group presented from 1 to 5 monocytes, and 71.4% presented more than 10 monocytes (p<0.001). Finally, the rabbits from the control, suture repair, and biological mesh groups presented no foreign body gigantic cells, while the rabbits of the polypropylene mesh group presented more than 10 foreign body gigantic cells (Table 2).

**TABLE 2** – Comparison among the control, suture repair, polypropylene mesh, and collagen mesh groups concerning the percentage of the incidence of polymorphonuclear monocytes and foreign body gigantic cells.

<table>
<thead>
<tr>
<th>Percentage of the incidence of polymorphonuclear, monocytes and foreign body gigantic cells</th>
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<tbody>
<tr>
<td><strong>Polymorphonuclear</strong></td>
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<tr>
<td>Average number of cells</td>
</tr>
<tr>
<td>Control</td>
</tr>
<tr>
<td>Suture repair</td>
</tr>
<tr>
<td>Polypropylene mesh</td>
</tr>
<tr>
<td>Collagen mesh</td>
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*1 p = 0.043; *2 p<0.001

In the collagen mesh group, a more homogeneous aspect could be observed, associated with a more ordered architectural arrangement of the collagen fibers, possibly stemming from the manner in which they were created. In the polypropylene mesh group, the gigantic cell reaction led to a diffuse architectural distortion of the collagen fiber pattern, as compared to the normally observed architecture, alterations which also occurred in the animals with abscess in their wounds (Figure 2).

**FIGURE 2** – Photomicrograph of **A** - group 3 - polypropylene mesh and **B** – group 4 – collagen mesh, stained with Masson trichrome (x100). Observe the more homogeneous aspect associated with a more ordered architectural arrangement of the collagenous fibers (collagen mesh) and gigantic cell reaction with a diffuse architectural distortion of the collagen fiber standard regarding the observed architecture (polypropylene mesh).

**Discussion**

The animals used in this work were rabbits, concerning the observation of their anatomy and feasibility of the surgical procedure without the need for special materials, in addition to the lower degree of complexity in caring for the animals during the entire post-operative period. The formulated experimental model, represented by group 1, presented an incisional hernia in 100% of the animals, demonstrating an effective model of abdominal wall hernia.

In this study, the mesh exposure presented as a complication of the surgical site. The animals from group 3 presented a polypropylene mesh exposure in five cases (71.4%), which did not occur in the other groups (p<0.005). However, none of the animals from group 3 presented an incisional hernia, with the secondary mesh exposure mainly representing the intense inflammatory reaction of the organism against the implant, without being associated, in this study, with the increase in the incidence of hernias.

The polypropylene mesh proved to be effective in abdominal wall repair, given that no animal from group 3 developed an incisional hernia, confirming the use of implants, more specifically polypropylene mesh, in the treatment of incisional hernias as a standard procedure. No statistically significant difference among the other groups could be observed regarding the incisional hernia.

The biological mesh studied herein presented 42.9% of failure hernia repair. One factor that may well have collaborated in
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bringing about this result was the use of the inlay technique for the setting of the mesh. Jin et al. demonstrated that the relapse was reduced when the separation of the components was combined with the setting of the biological implant and, inversely, when the biological mesh was set as a bridge (inlay), without bringing the borders of the hernia orifice closer together (recurrence rate of 80%). The Ventral Hernia Working Group (VHWG) recommend that the majority of biological implants must be implanted under the proper stress to prevent the further loosening of the material, as well as with different inlay techniques.

In the present study, the intensity of the inflammatory reaction was evaluated by the average count of the polymorphonuclear cells, monocytes, and foreign body gigantic cells. As expected, all groups presented some degree of inflammatory reaction; however, an intense reaction of the foreign body could be identified in group 3, represented by the average count of foreign body gigantic cells, presenting a statistically significant difference as compared to the other groups. The polypropylene implant caused an intense foreign body reaction. This microscopic result was in accordance with macroscopic findings regarding the mesh exposure (p<0.05) and may well explain the absence of incisional hernias in this group. The inflammatory reaction of the host against the polypropylene implant produced a fibrous and rigid scar, hindering herniation; however, the continuous activation caused by the presence of the foreign body led to the chronicity of this inflammatory process, in turn causing the exposure of the mesh in an attempt to eliminate the organism. Mesh exposure might be related with the thickness of subjects’ abdominal wall, however such intense inflammatory and foreign body reaction, causing mesh extrusion, did not occur with the use of type I collagen mesh. Thus, indicating a stronger response due to type of mesh material rather than the choice of research subjects.

By contrast, it could be observed that the type I collagen mesh behaved similarly to the host tissue by not unleashing an inflammatory reaction upon the foreign body. In addition, it was impossible, by optical microscopy and by the methods used in this study, to differentiate between the collagen of the biological implant and that of the host. This can be explained by the fact that the mesh collagen was substituted by the host collagen both partially and completely or that it had been reabsorbed. This differentiation is important to verify whether or not the mesh had been identified as “self” or “not-self”, which may well explain the observed failures. If the mesh is identified by the host as a “self”, regeneration and integration of the mesh to the original tissue occurs, demonstrating that the mesh is biocompatible, but needs a greater tensile strength, be it by increasing the number of layers of collagen or by using the cross linking method. If it is identified as “not-self”, the mesh would be reabsorbed with a reduction in tensile strength before the complete healing and relapse of the hernia. Accordingly, cross linking can also be used to hinder the reabsorption of the mesh, increasing the time for the growth of the host tissue and producing a more resistant healing process.

This study, using animal as main subjects, shows that polypropylene mesh is effective regarding the correction of abdominal wall defects and prevention of hernia recurrences, as seen in humans. The same cannot be said about type I collagen mesh, since this material was not used in studies with humans. Nevertheless, the results might be used as an indication of material behavior in humans when combined for better outcomes, such as in collagen coated polypropylene implants. Future studies are required to evaluate this matter.

Conclusions

The polypropylene mesh is effective in the treatment of abdominal wall defects, but causing an intense foreign body inflammatory reaction. The collagen mesh is biocompatible, causing a minimum inflammatory reaction, but it was not effective in the treatment of incisional hernias.

References


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