Histomorphometric Evaluation of New Bone Formation in Diabetic Rats Submitted to Insertion of Temporary Implants

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This study aimed to quantify new bone formation in the femurs of diabetic Wistar rats. Over an eight-week period, MTI-MP® implants were evaluated in control rats and in diabetic rats. At several points during this period, various markers for bone deposit were introduced. The material was observed under fluorescent light microscopy. New bone formation in periosteal and cortical regions linked to the implant did not vary significantly between the groups. However, there were significant differences in total new bone formation in the medullar canal and in bone/implant contact area in the medullar portion. Bone deposits attached to the surface of the temporary implants demonstrated that they are biocompatible and capable of osseointegration.

Key Words: diabetic rats, bone formation, temporary implants.

INTRODUCTION

During the evaluation of the implant odontological techniques, it was found that some patients face an unpleasant situation, in which they are partially or even totally deprived of their prosthesis during the post-implantation cicatrization period. In light of this, this study investigated the idea of installing pillars (implants) for temporary use. These pillars fix a temporary prosthesis until completion of the osseointegration period for the ‘definitive’ or ‘permanent’ implants. Once the implants have served their purpose, they are removed. Their installation is performed concurrently with the permanent implant surgery. The osseointegration of these implants and their support of the functional load have been demonstrated in various clinical and histological studies (1-7).

Another problem faced by professionals is that the therapeutic use of implants is often contraindicated. Patients suffering from diabetes mellitus are at a higher risk for post-surgical infection and typically present lower cicatrization rates (8). Therefore, the use of implants is not recommended for these patients (9,10). Most studies suggest that implants may be used in diabetic patients, but only when their illness is well under control. It is therefore necessary to administer metabolic compensation and postpone surgery until ideal conditions exist (11,12).

MATERIAL AND METHODS

All experimental procedures were carried out in accordance with the ethical principles set forth by the Brazilian School of Animal Experimentation (COBEA) and with the approval of the Ethics Committee for Animal Experimentation (CEEA) of the Biomedical Sciences Institute of the University of São Paulo (ICB-USP).

In this study, ten Wistar (Rattus norvegicus) rats, weighing an average of 265 g each, were maintained in the animal facilities of the Anatomy Department of ICB-USP. The animals were maintained on a dark/light cycle (12/12 h) under control conditions of temperature (21°C), air recycling and water and chow (Nuvilab™).
ad libitum. These animals were divided into 2 groups. One group was used as the control, and, seven days prior to the surgical intervention, the other group was induced to a diabetic condition by endovenous injection of alloxan in a single dose of 30 mg/kg of body weight. Blood glucose levels of the animals were evaluated weekly. Blood samples were collected from the distal third of the tail from each animal and measured by the glycosis-peroxidase method by a digital glycosimeter (Advantage Blood Glucose Monitor™, Boehringer Mannheim Corporation, Ingelheim, Germany), whose detection limits ranged from 10 to 600 mg/dl. Only those animals in which glucose levels were maintained at 300 mg/dl or higher throughout the entire experimental period were considered diabetic.

Modified MTI-MP® (Dentatus AB, Stockholm, Sweden) implants were used. The MTI-MP® implants are made from pure titanium, threadable and for temporary use. The implants originally measured 1.3 mm in internal diameter, 1.5 mm in external diameter and 14 mm in length. However, for the purpose of this study, the length of each implant was reduced to 5 mm. Subsequently, the implants were sterilized in an autoclave.

Cetamine chlorhydrate at a dose of 80 mg/kg was used for anesthesia. For muscular relaxation, sedation and analgesia, 2% xylazine hydrochloride was used (12 mg/kg, ip, single dose). Under anesthesia, three implants were inserted into the antero-lateral side of dia-physis in the left femurs of the animals, maintaining a distance of approximately of 5 mm between implants. In order to achieve parallelism between the elements, the insertion axis of each implant was perpendicular to the long axis of the receptor bone. The implantation beds were prepared using the drills indicated by the manufacturer assembled at a surgical contra-angle, running at approximately 1500 rpm and abundantly irrigated with saline solution. In the immediate postoperative period, benzylpenicillin benzatin (0.06 ml/kg, im, single dose) and paracetamol (10 mg/kg in drops diluted in the water for consumption for 2 consecutive days and changed daily) were administered. The cicatrization period was 8 weeks. During this period, a fluorescent marker was administered weekly (10 mg/kg calcein diluted in a 2% NaHCO₃ solution).

On day 56 after surgery, the animals were submitted to euthanasia with an overdose of ketamine chlorohydrate (300 mg/kg). The soft tissues were dissected and the femurs were isolated. These were fixed in formalin for 30 days. Each sample was subjected to periapical radiography of the pellicle (odontological use), with a perpendicular incidence on the anteromedial side. The position of each implant was confirmed and the transversal cuts were made in order to obtain individual blocks.

After routine histological processing, the blocks were immersed in containers filled with histo resin (methyl methacrylate - C₅H₈O₂) for inclusion. Transversal cuts, longitudinal to the implants, were then made with a microtome. The resulting sections were assembled on glass slides, ground down to an average thickness of 200 µm and examined under fluorescent light microscopy.

To perform the histomorphometric analysis, a millimeter grid was placed on the 20 x 25-cm amplifications of the obtained images. By counting the filled box from each target, the proportion of osseous neo-formation related areas characterized by the marker was quantified (13). It was necessary to categorize the various regions of the sections. In the areas of the bone cortex and medullar canal, the implant sections were subdivided into head, intra-cortical or intra-medullar portions (Figure 1).

The following relations were evaluated:

1. Total percentage of new bone formation (TNbF) in the entire section:

\[
\text{TNbF (in %)} = \frac{\text{Total area of marker} \times 100}{\text{Total bone area of the section}}
\]

Figure 1. Subdivisions of the implant sections.
New bone formation in temporary implants

2. Percentage of new bone formation linked to the periosteal side (NbFP) in the entire section:
   \[ NbFP \text{ (in %)} = \frac{\text{Area of marker on the periosteal side} \times 100}{\text{Total bone area of the section}} \]

3. Percentage of new bone formation linked to the endosteal side and in the medullar canal (NbFMC):
   \[ NbFMC \text{ (in %)} = \frac{\text{Area of marker on the endosteal side and in the medullar canal} \times 100}{\text{Total bone area of the section}} \]

4. Percentage of contact between bone and implant on the intra-cortical side (BIpCC)
   \[ BIpCC \text{ (in %)} = \frac{\text{Perimeter of bone/implant contact on the intra-cortical side} \times 100}{\text{Perimeter of the implant on the intra-cortical side}} \]

5. Percentage of contact between bone and implant in the intra-medullar portion (BIpCM)
   \[ BIpCM \text{ (in %)} = \frac{\text{Perimeter of bone/implant contact in the intra-medullar portion} \times 100}{\text{Perimeter of implant in the intra-medullar portion}} \]

6. Percentage of total contact between new bone formation and implant (TNbIC)
   \[ TNbIC \text{ (in %)} = \frac{\text{Perimeter of the bone/implant contact in intra-cortical and intra-medullar portions} \times 100}{\text{Total perimeter of implant in intra-cortical and intra-medullar portion}} \]

The statistical analysis was performed using analysis of variance by non-paired T test and ANOVA with specific software (GraphPad InStat – Version 3.00, GraphPad Software Inc., San Diego, CA, USA).

RESULTS

Under fluorescent light microscopy, it was possible to observe the presence of markers and, therefore, the occurrence of bone deposit. In descending order of quantity, the three markers observed were calcein, tetracycline and alizarin. In this analysis, it was also possible to distinguish the bone tissue as (4): a) primary bone: the cortical tissue already present at the time of the surgery. This tissue was not identified by the markers; b) secondary bone: bone that appears after the introduction of the implants. The markers identified apatite crystal deposits. It was possible to observe bands of different colors corresponding to the administration of each stain.

Control Group

Analysis of the sections revealed intense new bone formation. This was verified in a generalized way, encompassing the periosteal, endosteal and medullar canal regions of all samples.

The new bone formation presented lamellar characteristics. In the periosteal regions, layered deposits of new bone formation of various thicknesses were observed. The most common deposits were those marked by calcein, which were characterized by the formation of two parallel lamellae coinciding with the two periods during which this marker was administered. The other markers did not present this same characteristic.

In the endosteal region, new bone formation was less evident than in the periosteal region. Bone deposits were frequently observed running along the entire surface of implants. Formation of a trabecular pattern spreading over the medullar canal, with bone bridges connecting the endosteum to the implant surface, was also observed.

Diabetic Group

Analysis of this group showed new bone formation in all implants. In a general way, the area of new bone formation was significantly smaller than in the control group. However, new bone formation in the periosteal region was comparable to that observed in the control group.

In all samples, new bone formation that followed exactly the surface of the implant was observed. The frequently observed bone bridges linking the endosteum to the surface of the implant in the control group only appeared in 2 of 9 implants in this group (Figure 2).

Morphometric Analysis

Values of p < 0.05 were considered significant for statistical analysis. To determine whether the position of the implant resulted in any difference among the results obtained from a given animal, the data were
Figure 2. Bone bridges linking the endosteum to the surface of the implant.

Table 1. Comparison of new bone formation in control and diabetic groups

<table>
<thead>
<tr>
<th>Relationship</th>
<th>Control</th>
<th>Diabetic</th>
</tr>
</thead>
<tbody>
<tr>
<td>TNbF</td>
<td>44.93 ± 2.714</td>
<td>37.35 ± 5.019*</td>
</tr>
<tr>
<td>NbFP</td>
<td>28.14 ± 4.512</td>
<td>25.18 ± 4.091</td>
</tr>
<tr>
<td>NbFMC</td>
<td>43.76 ± 13.976</td>
<td>17.87 ± 3.744*</td>
</tr>
<tr>
<td>BIpCC</td>
<td>70.81 ± 11.848</td>
<td>78.13 ± 11.276</td>
</tr>
<tr>
<td>BIpCM</td>
<td>73.03 ± 14.516</td>
<td>39.00 ± 11.606*</td>
</tr>
<tr>
<td>TNbIC</td>
<td>71.56 ± 10.377</td>
<td>49.18 ± 10.056*</td>
</tr>
</tbody>
</table>

Data are reported as mean ± SD. *Significant difference between control and diabetic groups (unpaired t-test, p < 0.05).

In the present study, the system of temporary implants used (MTI-MP®) showed characteristics of osseointegration with a median of 71.56% ± 10.377 TNbIC, which is higher than the 45% found in previous studies (6). However, it is important to bear in mind that this study was performed with human material from areas where the implants had been under a masticatory load immediately following introduction of the implant, possibly accounting for these differences. The bone/implant contact values reinforce previous clinically obtained results (3-7). The rate of contact between bone and implant was equivalent to that found for implants designed for long-term use.

In the histomorphometric analysis, the head region was omitted, despite the new bone formation that had been observed in this area. This was justified by the fact that the new bone formation in this region is attributable more to the surgical technique than to the osteoconductive properties of the implant. After the periosteum has been dislocated, folded over, replaced...
and sutured, a subperiosteal space is formed that ends up being a place for formation and retention of blood clots. Later, it is replaced by bone.

Examination of the material under fluorescent light microscopy employing a prism revealed a clear difference in the new bone formation observed in the medullar canal, which normally presents no calcified tissue. After introduction of the implants, bone with lamellar characteristics was observed in the medullar canal. This bone deposit presented trabecular morphology, forming bone bridges linking the endosteum to the surface of the implant or running the length of the implant. In addition, in the qualitative analysis, well-defined formations were observed in samples from control group animals, whereas no such formations were seen in the diabetic group.

An extremely significant statistical difference was found between the two groups in the percentage of new bone formation in TNbIC. This is in agreement with the findings of other authors (16,18). A similarly significant difference has been shown during the cicatrization period, at 14 days and 84 days post-implantation (15,18). In these previous studies, the animals in the diabetic groups received no diabetic control.

The values obtained for BIpCM were extremely significant, similar to those from other studies (15,16). Analysis of the TNbIC revealed increased new bone formation in comparison with the control group; however, the differences between the groups remain significant (17). Comparison of BIpCC values showed a non-significant difference (15).

For the other relationships evaluated in the present study, the results were not in agreement with those reported by other authors. Comparing new bone formation data from the different regions, we can conclude that metabolic alterations resulting from clinical diabetic conditions led to lower osteogenic activity. This phenomenon has been previously described (15,17,19-20).

The initial expectation of the authors of the present study was that there would be a generalized reduction in bone deposit. The non-significant difference in NbFP and BIpCC between the two groups was a surprising finding. We can hypothesize that the surgical trauma caused by rotation, cutting or heating (despite the care in irrigation) of the area during the creation of the implantation beds stimulated a cicatrization process different from that typically promoted by the osteoconductive characteristics of titanium. On the other hand, considering the deposit in the periosteal side, this finding may be attributable to the apposition phenomenon that occurs during normal bone formation. Therefore, this may occur independently of the introduction of the implant. All other regions evaluated were created as a result of the installation of the implants.

Thus, the bone deposits attached to the surface of temporary implants demonstrated that they are biocompatible and capable of osseointegration.

RESUMO
Este estudo se propôs a quantificar a neoformação óssea nos fêmures de ratos Wistar diabéticos. Implantes MTI-MP® foram avaliados por um período cicatrial de 8 semanas durante as quais foram administrados marcadores de deposição óssea. O material foi observado sob microscopia de luz fluorescente. A neoformação óssea nas regiões periostal e na cortical junto ao implante não mostraram diferença significativa entre os grupos. Essa mostrou-se significativa quando avaliado o canal medullar, na avaliação do tecido neoformado como um todo e na área de contato entre osso e implante quando analisada sua porção intramedullar. A deposição óssea analisada junto à superfície dos implantes temporários demonstrou que os mesmos são biocompatíveis e passíveis de osteointegração.

REFERENCES
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Accepted April 25, 2004