This in vitro study evaluated the preventive potential of experimental pastes containing 10% and 20% hydroxyapatite nanoparticles (Nano-HAP), with or without fluoride, on dental demineralization. Bovine enamel (n=15) and root dentin (n=15) specimens were divided into 9 groups according to their surface hardness: control (without treatment), 20 Nanopaste (20% HAP), 20 Nanopaste plus (20% HAP + 0.2% NaF), 10 Nanopaste (10% HAP), 10 Nanopaste plus (10% HAP + 0.2% NaF), placebo paste (without fluoride and HAP), fluoride paste (0.2% NaF), MI paste (CPP-ACP, casein phosphopeptide-amorphous calcium phosphate), and MI paste plus (CPP-ACP + 0.2% NaF). Both MI pastes were included as commercial control products containing calcium phosphate. The specimens were treated with the pastes twice a day (1 min), before and after demineralization. The specimens were subjected to a pH-cycling model (demineralization–6-8 h/ remineralization-16-18 h a day) for 7 days. The dental subsurface demineralization was analyzed using cross-sectional hardness (kgf/mm², depth 10-220 µm). Data were tested using repeated-measures two-way ANOVA and Bonferroni’s test (p<0.05). The only treatment able to reduce the loss of enamel and dentin subsurface hardness was fluoride paste (0.2% NaF), which differed significantly from the control at 30- and 50-µm depth (p<0.0001). The other treatments were not different from each other or compared with the control. The experimental Nanopaste pastes, regardless of the addition of fluoride, were unable to reduce dental demineralization in vitro.
of the bovine crown and labial/lingual surfaces of the cervical portion of bovine roots, respectively. The teeth were stored in 0.1% buffered thymol solution (pH 7.0) at 4°C. The specimens were cut using an ISOMET low-speed saw cutting machine (Buehler Ltd., Lake Bluff, IL, USA) with two diamond disks (Extec Corp., Enfield, CT, USA), separated by a 4-mm thick spacer. The specimens' surfaces were ground flat using water-cooled silicon carbide discs (320-, 600- and 1200-grit Al₂O₃ papers; Buehler), and polished using felt paper soaked with diamond solution (1 µm; Buehler). After polishing, the specimens were cleaned in an ultrasonic bath with deionized water for 5 min. The initial surface hardness was measured using the mean of five indentations (Knoop diamond, 25 g/10 s for enamel and 10 g/10 s for dentin) using a microhardness tester (HMV-2; Shimadzu Corporation, Tokyo, Japan).

Prior to the experiment, the specimens were covered with nail polish in order to create control areas on both sides of a central strip of enamel or dentin. The specimens were maintained in 100% humidity until the beginning of the experiment.

The 15 enamel and 15 dentin specimens were randomly allocated to one control (untreated) and 8 test groups according to their baseline surface hardness values (328±18 and 23±2 kgf/mm² for enamel and dentin, respectively): 20 Nanop paste (20% HAP), 20 Nanop paste plus (20% HAP + 0.2% NaF), 10 Nanop paste (10% HAP), 10 Nanop paste plus (10% HAP + 0.2% NaF), placebo paste (without HAP and F), fluoride paste (0.2% NaF), MI paste (CPP-ACP), and MI paste plus (CPP-ACP +0.2% NaF). The Nanop-HAP pastes were prepared by FGM-Dentscare (Joinville, SC, Brazil) and the MI paste products (Recaldent-CPP-ACP) were from GC America (St. Alsip, IL, USA). The experimental pastes (pH 7.0) contained nanometer calcium phosphate (hydroxyapatite, 100 nm), sodium fluoride (in case of the plus pastes), potassium nitrate, distilled water, thickener, surfactant, moist, flavor, sweetener and preservative.

### Calcium and Phosphate Analysis

The soluble calcium and phosphate contents of one representative paste of each group (1 g paste/5 mL deionized water centrifuged at x5000 for 10 min) were evaluated using the colorimetric methods of Arsenazo III (19) and Fiske-Subarrow (20), respectively. Optical density measurements were carried out by a scanning spectrophotometer (Fluorstar Optima - BMG Labtech GmbH, Ortenberg, Germany), at a 660 nm wavelength, in triplicate. The absorbance values were converted in mg% using the standard curve with an r≥0.99.

### Treatment and pH Cycles

Enamel specimens were subjected to a pH-cycling model for 7 days, as described by Vieira et al. (21). For 5 days, the specimens were immersed in demineralizing solution [2.0 mmol/L Ca(NO₃)₂·4H₂O, 2.0 mmol/L Na₂HPO₄·2H₂O, 75 mmol/L acetate buffer, 0.04 ppm F, pH 4.7] for 6 h (30 mL)

### Table 1. Mean of calcium and phosphate content of the experimental pastes (mg%, mg/100 mL)

<table>
<thead>
<tr>
<th>Pastes</th>
<th>Calcium</th>
<th>Phosphate</th>
</tr>
</thead>
<tbody>
<tr>
<td>Placebo</td>
<td>3.27</td>
<td>470.4</td>
</tr>
<tr>
<td>F</td>
<td>1.66</td>
<td>380.2</td>
</tr>
<tr>
<td>10 Nanop</td>
<td>1.91</td>
<td>282.8</td>
</tr>
<tr>
<td>10 Nanop plus</td>
<td>2.09</td>
<td>256.8</td>
</tr>
<tr>
<td>20 Nanop</td>
<td>3.72</td>
<td>553.0</td>
</tr>
<tr>
<td>20 Nanop plus</td>
<td>3.57</td>
<td>424.8</td>
</tr>
<tr>
<td>MI paste</td>
<td>222.7</td>
<td>2249.3</td>
</tr>
<tr>
<td>MI paste plus</td>
<td>214.1</td>
<td>2616.8</td>
</tr>
</tbody>
</table>

### Table 2. Mean of enamel cross-sectional hardness and S.D. according to the treatment and depth (kgf/mm²)

<table>
<thead>
<tr>
<th>Depth</th>
<th>20 Nanop</th>
<th>20 Nanop plus</th>
<th>10 Nanop</th>
<th>10 Nanop plus</th>
<th>Placebo</th>
<th>F</th>
<th>MI Paste</th>
<th>MI Paste plus</th>
<th>Control</th>
</tr>
</thead>
<tbody>
<tr>
<td>10 µm</td>
<td>3±6</td>
<td>0±0</td>
<td>1±4</td>
<td>39±20</td>
<td>1±3</td>
<td>65±54</td>
<td>3±7</td>
<td>25±4</td>
<td>7±10</td>
</tr>
<tr>
<td>30 µm</td>
<td>8±21</td>
<td>0.2±0.7</td>
<td>5±6</td>
<td>54±27</td>
<td>2±5</td>
<td>186±51</td>
<td>7±11</td>
<td>42±8</td>
<td>16±24</td>
</tr>
<tr>
<td>50 µm</td>
<td>37±62</td>
<td>17±37</td>
<td>40±34</td>
<td>115±89</td>
<td>16±30</td>
<td>253±49</td>
<td>39±46</td>
<td>22±26</td>
<td>91±89</td>
</tr>
<tr>
<td>70 µm</td>
<td>133±109</td>
<td>100±90</td>
<td>127±104</td>
<td>223±92</td>
<td>91±84</td>
<td>243±53</td>
<td>144±81</td>
<td>85±69</td>
<td>169±104</td>
</tr>
<tr>
<td>90 µm</td>
<td>228±129</td>
<td>240±78</td>
<td>223±12</td>
<td>272±71</td>
<td>224±84</td>
<td>258±46</td>
<td>262±49</td>
<td>207±102</td>
<td>226±71</td>
</tr>
<tr>
<td>110 µm</td>
<td>268±110</td>
<td>282±56</td>
<td>274±11</td>
<td>292±57</td>
<td>265±71</td>
<td>267±43</td>
<td>292±38</td>
<td>248±79</td>
<td>261±52</td>
</tr>
<tr>
<td>200 µm</td>
<td>317±63</td>
<td>319±53</td>
<td>286±95</td>
<td>306±56</td>
<td>275±42</td>
<td>258±49</td>
<td>284±40</td>
<td>283±57</td>
<td>258±61</td>
</tr>
</tbody>
</table>

Treatments whose means are followed by distinct lowercase letters in the same row differ significantly (p<0.0001). Depths whose means are followed by distinct uppercase letters in the same column differ significantly (p<0.0001).
per specimen) and in remineralizing solution [1.5 mmol/L Ca(NO\textsubscript{3})\textsubscript{2}, 0.9 mmol/L Na\textsubscript{2}HPO\textsubscript{4}, 150 mmol/L KCl, 0.02 mol/L Tris buffer, 0.05 ppm F, pH 7.0] for 18 h (30 mL per specimen) at 37\textdegree C, without agitation. In the last two days, the specimens were maintained in remineralization solution only. The solutions were replaced daily.

Dentin specimens were subjected to a pH-cycling model for seven days (3, 22). The specimens were immersed in demineralizing solution [1.5 mmol/L CaCl\textsubscript{2}, 0.9 mmol/L KH\textsubscript{2}PO\textsubscript{4}, 50 mmol/L lactic buffer, pH 5.0] for 8 h (30 mL per specimen) (3), and in remineralizing solution [1.5 mmol/L CaCl\textsubscript{2}, 0.9 mmol/L KH\textsubscript{2}PO\textsubscript{4}, 130 mmol/L KCl, 20 mmol/L Hepes buffer, 5 mmol/L NaN\textsubscript{3}, pH 7.0] for 16 h (30 mL per specimen) (22) at 37\textdegree C without agitation. The solutions were replaced daily.

The pastes were applied twice a day, before and after the demineralizing process, using a microbrush for 1 min, to simulate the daily application. The excess paste was removed and the specimens were washed in deionized water for 5 s before being immersed in the de- or remineralizing solution.

### Hardness Determination

Initially, enamel and dentin surface hardness was measured as described above (Knoop diamond, HMV-2; Shimadzu Corporation). Five indentations 100 µm from each other, were made in the center of dental surface for selection and random distribution of the specimens in the groups. After the treatment and pH-cycles, the cross-sectional hardness (CSH) was measured. The specimens were longitudinally sectioned through the center, embedded in acrylic resin, and polished. Three rows of seven indentations each were made, one at the central region of the exposed enamel and dentin area and the other two 100 µm below and above this, for 10 s under a 25 g and 10 g load, respectively. The indentations were made at 10, 30, 50, 70, 90, 110, and 220 µm from the outer enamel and dentin surface. The mean values of all three measuring points at each distance from the surface were then averaged (kgf/mm\textsuperscript{2}).

### Statistical Analysis

The GraphPad InStat version 2.0 for Windows software (GraphPad Software, Inc., La Jolla, CA, USA) was used. The assumptions of equality of variances and normal distribution of data were checked for all the tested variables, using the Bartlett and Kolmogorov-Smirnov tests, respectively. Repeated-measures two-way ANOVA followed by Bonferroni’s test were carried out, considering as criteria the treatments and the depths (GraphPad Prism 4 software; GraphPad Software, Inc.). The significance level was set at 5\% (n=15).

### Results

Calcium and phosphate contents of the pastes are displayed in Table 1. The experimental Nanop paste contained low soluble calcium and phosphate, while the commercial MI pastes presented high level of soluble calcium and phosphate.

There were significant differences among the treatments, depths, and interaction between the factors for enamel (p<0.0001 for all, Table 2). The experimental 20 and 10 Nanop pastes were unable to reduce the subsurface enamel demineralization. F paste significantly decreased the loss of enamel hardness at 30 and 50 µm compared with control, and from 30 to 70 µm compared with placebo. The 10 Nanop plus paste also significantly differed from placebo paste at 50 and 70 µm depths. At the other depths and among the other treatments there were no significant differences (Table 2). Furthermore, there was a significant increase in the hardness values with the increase of enamel depth. For the 10 Nanop, 10 Nanop plus, placebo, MI paste and control, the hardness values increased significantly up to 220 µm.
to 90 µm; for the F paste up to 50 µm (the most superficial lesion); and for 20 Nanop, 20 Nanop plus, and MI paste plus up to 110 µm depth (the deepest lesion) (Table 2).

As to dentin demineralization, there were significant differences among the treatments and the depths (p<0.0001) and no interactions between the factors (p=0.054) (Table 3). The F paste was the only treatment able to reduce the subsurface dentin demineralization compared with the control at 30 and 50 µm and to the placebo paste at the 30-µm depth. At the other depths and among the other treatments there were no significant differences. Hardness values increased with the increase of the dentin depth. For the 10 Nanop paste, the hardness values significantly increased up to 90 µm, and for the F paste up to a 50-µm depth (the most superficial lesion). For the other treatments, the hardness values changed significantly up to a 110-µm depth (the deepest lesion) (Table 3).

Discussion

The present study analyzed the effect of a new product on the prevention of dental demineralization. Currently, there is lack of knowledge about the remineralizing and desensitizing potential of biomaterials based on nanotechnology, which, in turn, may be an important preventive strategy to be applied in high-caries risk patients.

The pH-cycling model chosen for enamel and dentin was based on previous studies each focusing on one type of dental substrate (3,21,22). The models should be able to simulate the demineralization and remineralization episodes, considering the composition of the different dental substrates, in order to create a subsurface mineral loss and not an erosive lesion (10 µm deep) at the end of the experiment. It is important to clarify that the design of the present study was not focused on showing the impact of the experimental pastes on the remineralization of pre-formed enamel and dentin caries lesions, but on the prevention of demineralization.

Another important aspect is that the experimental pastes are not dentifrices that should be diluted and applied during toothbrushing; the experimental pastes present the same mode of application as the commercial MI pastes, which must be applied after oral hygiene by the patient, using finger on the affected tooth areas (23). Therefore, in the present study all pastes were applied using a microbrush applicator for 1 min. The cross-sectional hardness was chosen as a response variable, as it reflects the mechanical resilience of the hard tooth tissue, which might be indirectly related to its mineral content.

Accordingly, all pastes with calcium phosphate were unable to reduce the dental demineralization using this model, regardless of the type of compound (CPP-ACP or Nano-HAP) and dental substrate. Therefore, the tested hypothesis was rejected.

It was expected that the Nanop, which presents hydroxyapatite particles with characteristics similar to the dental apatite, would have the ability to provide calcium and phosphate in an adequate concentration and velocity to react with the dental structure (8), repairing or promoting the dental crystal growth (24).

In respect to remineralization, a previous study (9) showed that different concentrations of Nano-HAP (1, 5, 10, and 15%) were effective compared with placebo on enamel remineralization, with 10% HAP nanoparticles being the best concentration. The effect of 20-24% Nano-HAP on dentin remineralization was also similar to enamel in another study (6). It has been suggested that Nano-HAP leads to more mineral deposits on the outer layer than in the body lesion. Therefore, mineral diffusion could be inhibited by the highly mineralized surface layer, making full remineralization not achieved by application of Nano-HAP (4,8). This phenomenon has been previously discussed; initial caries lesions can be rehardened by the deposition of hydroxyapatite that first happens near the surface layer, but then it is gradually transferred inward and finally precipitated in the dark zone during the long-term remineralization. From this perspective, Nano-HAP might have a good potential to promote remineralization (9) with regular daily use as proposed by the previous studies (6,9). However, the present study was focused on demineralization, showing that the regular application of Nano-HAP pastes was unable to prevent demineralization regardless of the Nano-HAP concentration and the lesion depth. Additionally, the experimental pastes presented low calcium and phosphate content in water that might be related to its low solubility. Therefore, the experimental pastes could not react appropriately with the tooth. Another possible mechanism of action of the Nano-HAP would be a mechanical imbrication of the pastes into the porous dental surface due to the size of the particles; but regardless of this, the experimental pastes were ineffective to reduce demineralization.

Since previous studies have shown a positive effect of Nano-HAP on enamel and dentin remineralization (4,6,8,9), there might be a different result if a pH-cycling model focusing on the remineralization of pre-formed lesions (remineralization>>>demineralization) rather than demineralization (remineralization>>demineralization) had been performed. The remineralizing potential of the experimental pastes (Nanop-HAP) on pre-demineralized hard dental tissue should be tested in future assays.

The addition of fluoride did not have any positive influence on the effect of the experimental Nanop-HAP pastes for both enamel and dentin. In vitro experimental conditions cannot encapsulate all the complexities of a
living oral cariogenic environment (23). Therefore, in further studies, the effect of the experimental pastes must be tested in situ to show whether the reaction between Nanop or Nanop plus and the dental surface would be better in the presence of human saliva and acquired pellicle. In addition, it would be interesting to check if the effect might also be modulated by the time of application and the procedure to remove the pastes from the dental surface. The amount of product retained on the dental substrate after water washing in this in vitro model could be not enough to have any effect against demineralization; while in the presence of human saliva the results might be different.

On the other hand, the only treatment able to reduce the dental subsurface demineralization was F paste, which lost its positive effect when incorporated into Nanop paste. Such result may be attributed to a possible reaction between NaF and HAP, reducing the quantity of soluble fluoride. The constant presence of low fluoride concentration in the oral fluids during an acidic challenge favors its absorption to the surface of the apatite crystals, inhibiting demineralization. When the pH is reestablished, traces of fluoride in oral fluid will make it highly supersaturated with respect to fluorhydroxyapatite, which will speed up the process of remineralization (25). Further studies should be performed to test the remineralizing effect and the dentin obliteration potential of the experimental F paste.

Prospec MI pastes (CPP-ACP, with or without F) were included in the study as commercial controls, since they present a similar mechanism of action and application mode of the Nanop pastes. CPP-ACP products have shown an ability to prevent dental demineralization and increase remineralization of enamel and dentin in vitro (12,13), as well as to arrest initial enamel caries lesions in vivo (15–17). However, due to the lack of clinical trials, there is no consensus about the cariostatic effect of CPP-ACP. The present study shows lack of a CPP-ACP effect on the prevention of dental demineralization, in spite of the commercial pastes presenting high level of soluble calcium and phosphate. Further studies using different protocols should be performed to confirm the present results, which might be explained at least partially by the pH-cycling models. In conclusion, the experimental Nanop pastes, regardless of the concentration and presence of fluoride, were unable to reduce enamel and dentin demineralization under this in vitro protocol. Fluoride paste is still the best option to reduce dental demineralization in vitro.

Acknowledgements

The authors would like to thank FAPESP (Proc. 2009/08518-3 and 2010/07001-4) for its financial support.

References


Received February 1, 2013
Accepted May 6, 2013