Introduction

The use of osseointegrated dental implants requires an adequate amount of bone tissue both in volume and in quality (1). However, these conditions are not always available, necessitating reconstruction with bone substitutes. Autogenous bone is regarded as the gold standard for these procedures because of its biological and physico-chemical properties, which are considered optimal (2). However, there is a need for a second surgical procedure, increasing the risk of complications (3). The bone allograft presents a reduction in surgical procedures (4), although there are risks such as disease transmission (5). Because of these difficulties, many biomaterials of xenogenous or alloplastic origin are being researched for the purpose of bone reconstruction.

Xenogenous bovine bones are used as bone substitutes, they are deproteinized and lyophilized. Biomaterials with these characteristics do not cause any immune response, so they are considered as biocompatible (6). This category includes Bio-Oss® (Geistlich-Pharma, Wolhusen, Switzerland), consisting of calcium carbonate apatite; it is osteoconductive, has a porosity between 75% and 80% and can be used to raise the maxillary sinus membrane, resulting in proper osseointegration of the dental implant in the bone tissue (7). Bio-Oss® is slowly reabsorbed, with residues found nine years after the initial graft (8).

Endobon® Xenograft Granules (RegenerOss™, BIOMET 3i, Palm Beach Gardens, FL, USA) are another bone substitute consisting of bovine bone, both deproteinized and lyophilized. According to the manufacturer, it is granular in form, has a porosity between 45% and 80% and consists of completely deproteinized hydroxypatite bovine. Moreover, it is biocompatible, bioactive, osteoconductive and not resorbable (9, 10).

Straumann® Bone Ceramic (Biora AB, company of the Straumann Group, Malmoe, Sweden) is a fully alloplastic bone substitute based on biphasic calcium phosphate (40% β-tricalcium phosphate and 60% hydroxyapatite), it is osteoconductive and is used to raise the maxillary sinus membrane surgery (11), results in trabecular bone structure with close contact with the biomaterial, thereby allowing the placement of dental implants after six months (12).

The aim of this study was to evaluate and compare bone healing in surgically prepared cavities in rabbit skulls using three different biomaterials, two of which are xenogenous, consisting of deproteinized and lyophilized bovine bone, and one alloplastic bone based on biphasic calcium phosphate.

Material and Methods

Experimental Design

Three bone substitutes were used, as follows: two xenogens consisting of deproteinized and lyophilized bovine bone in Bio-Oss® and Endobon® Xenograft Granules, and a fully alloplastic one based on biphasic calcium phosphate in Straumann® Bone Ceramic. They were surgically grafted into
bone defects prepared in the skullcaps of five rabbits. After eight weeks, the samples were subjected to morphometric and qualitative analyses. For the statistical analysis, ANOVA and Tukey’s test were conducted at a significance level of 0.05 using the statistical software SAS version 7.0 (SAS Institute, Cary, NC, USA).

Animal Study

The present study used five New Zealand male white rabbits, weighing between 2900 g and 3500 g. The study was approved by the ethics committee (protocol n° 011/12-CEP/ICS-UNIP) and was in accordance with the guidelines and rules for research involving animals according to State Law no. 11997 of August 25, 2005, which established the Code of Animal Protection of the State of São Paulo, Brazil.

The animals were kept in individual cages under the same environmental conditions before surgery and during the evaluation period. They were fed MP872 (Moinhos Primor S.A., São Paulo, SP, Brazil) and water ad libitum.

Surgical Procedures

Surgical procedures followed previously proposed methodologies by Aghaloo et al. (13). The animals were premedicated using a combination of 1 mg/kg of morphine (Cristália Produtos Químicos Farmacêuticos Ltda., Itapira, SP, Brazil), 1 mg/kg of midazolam (Cristália Produtos Químicos Farmacêuticos Ltda., Itapira, SP, Brazil), 10 mg/kg of ketamine (Symtec do Brasil Ltda, Cotia, SP, Brazil) and 2 mg/kg of xylazine (Rompun® Bayer S.A., São Paulo, SP, Brazil) administered intramuscularly. Anesthesia was induced with propofol (Cristália Produtos Químicos Farmacêuticos Ltda., Itapira, SP, Brazil) at a dose of 2 mg/kg intravenously, as well as local anesthesia with 4% articaine hydrochloride with 1:100,000 epinephrine (DFL Industria e Comercio S.A., Rio de Janeiro, RJ, Brazil), via infiltration at the site of surgery. Throughout the procedure, the animals were masked to provide 100% oxygen; they were monitored for heart rate, respiratory rate, oxygen saturation, hemoglobin, temperature and blood pressure (BP) (systolic BP, diastolic BP and PA average) in a non-invasive way with a veterinary multiparameter monitor (NeoVet®, Centaurus Medical, San Diego, CA, USA). Prophylactic antibiotic therapy was administered with enrofloxacin (Schering-Plough Saúde Animal Ind e Com Ltda, Cotia, SP, Brazil) at a dose of 5 mg/kg intravenously.

After obtaining anesthesia, the surgical region was shaved and applied with 2% iodine antiseptic solution. Next a sagittal incision was made approximately 10 cm in the midline of the skull, primarily in the skin, followed by the periosteum to expose the parietal bones. Four standardized bone defects were made, two on each bone, using a sterile 8-mm diameter trephine cutter drill (Implacil Material Odontológico Ltda., São Paulo, SP, Brazil) under copious irrigation with sterile saline solution.

The defects were filled with different bovine bone substitutes. First was filled with Bio-Oss® of diameters between 250 and 1000μm. The second was filled with Endobon®Xenograft Granules of diameters between 500 and 1000 μm. The third was filled with Straumann®Bone Ceramic, a completely alloplastic-based biphasic calcium phosphate comprising 60% hydroxyapatite (HA) and 40% β-tricalcium phosphate (β-TCP), of diameters between 500 and 1000 μm. One of the defects was maintained as control (Fig. 1).

Grafting procedures were performed before the periosteum was repositioned absorbable suture (Vicryl® 4-0, Johnson & Johnson do Brasil Indústria e Comércio de Produtos para Saúde Ltda, São José dos Campos, SP, Brazil). Then, the skin was repositioned and sutured with nylon thread (5-0 Ethicon® Johnson & Johnson do Brasil Indústria e Comércio de Produtos para Saúde Ltda, São José dos Campos, SP, Brazil). After suturing, the surgical region was washed with 2% iodine solution.

After completing the surgical procedures, xylazine reversal was induced through the antagonist yohimbine (PowerVet, São Paulo, SP, Brazil) at a dose of 0.1 mg/kg intravenously. Immediate postoperative analgesia was administered via intramuscular morphine at 1 mg/kg.

Postoperatively, the animals were administered the analgesic tramadol hydrochloride (Cristália Produtos Químicos Farmacêuticos Ltda., Itapira, SP, Brazil) at 0.6 mL/12 in 12 h, the anti-inflammatory drug dexamethasone (disodium phosphate) at 0.6 ml/12 in 12 h over three days, and the antibiotic enrofloxacin 2.5% at 0.6 mL/12 in 12 h for one week.

Figure 1. Defects in the parietal bone patterned and filled with graft materials. A: Control, B: Straumann®Bone Ceramic, C: Bio-Oss® and D: Endobon®Xenograft Granules.
Assessment of bone healing in rabbit calvaria

Sacrifice of Animals

The animals were sacrificed eight weeks after the surgical procedures, initially using a combination of xylazine (20 mg/kg) and ketamine (50 mg/kg) administered intramuscularly, followed by 25 mg/kg of sodium thiopental (Cristália Produtos Químicos Farmacêuticos Ltda, Itapira, SP, Brazil) administered intravenously in the ear vein 15 minutes thereafter.

Histological Analysis

The samples were demineralized in 20% formic acid for seven days, dehydrated in alcohol with increasing concentrations (70% - 100%) for one hour each, cleared in two changes of xylene for one hour each and were paraffin embedded at 60°C for 1 h. Five micrometers were obtained, stained with hematoxylin and eosin (HE) and analyzed using light microscopy.

Morphometric Analysis

Five sections (5 μm) were obtained from the center of each sample from each animal (20x magnification). Histology slides were then obtained for histomorphometric analysis coded to be blind regarding study treatment groups. We used a system of computerized image analysis consisting of a light microscope (Axioskop 2 plus®, Carls Zeiss, Oberkochen, Germany) coupled to a camera (AxioCam HRc®, Carls Zeiss, Oberkochen, Germany) connected to a microcomputer, which used the image analysis software Axion Vision® rel 4.8 (Carls Zeiss, Oberkochen, Germany). Percentages were calculated for newly formed bone, residual graft and connective tissue in the bone marrow.

Qualitative Analysis

Qualitative analysis of the samples was conducted using cone-beam computer tomography obtained with the scanner Gendex CB500®, (Gendex Dental Systems, Des Plaines, IL, USA) under the following settings: 120 kVp, voxel 0.125 mm and acquisition time of 23 s. For the three-dimensional reconstructions, the software INVIVO 5® (Anatomage, San José, CA, USA) was used, with axial DICOM thickness of 1 mm.

Statistical Analysis

The histomorphometric data showed homoscedasticity of variances after application of the F test. Analysis of variance was performed, which showed differences between the treatments at a significance level of 0.05. Then was applied the Tukey’s test, which compared the different treatments (coagulum, Bio-Oss®, Endobon® Xenograft Granules and Straumann®Bone Ceramic) according to different factors (newly formed bone, residual graft and connective tissue in the bone marrow). SAS 7.0 (SAS Institute, Cary, NC, USA) was used for the statistical analyses.

Results

Histological Analysis

After eight weeks, histological analysis showed the presence of new bone tissue in all cavities filled with different biomaterials. Presence of residual graft was also observed in the surgical defects filled with Straumann®Bone Ceramic and Bio-Oss® (Fig. 2).

Morphometric Analysis

Morphometric analysis showed the following amounts of newly formed bone: Bio-Oss® (57.00±7.76), Endobon® Xenograft Granules (58.42±6.29) and Straumann®Bone Ceramic (78.06±8.95). The percentage of new bone formation

Figure 2. Bone formation in defects in the parietal bone of a rabbit filled with different biomaterials. A: Control, B: Straumann Bone Ceramic, C: Bio-Oss®, and D: Endobon®Xenograft Granules (black asterisk = new bone, blue asterisk = residual graft, Original magnification, 100x; HE).
was greater ($p<0.05$) in the bone defects filled with Straumann® Bone Ceramic than in those grafted with Bio-Oss® or Endobon® Xenograft Granules (Table 1). Residual graft material displayed the following levels: BioOss® with 27.58±6.16, Endobon® Xenograft Granules with 25.42±8.82 and Straumann® Bone Ceramic with 6.28±1.79, with the last one showing significantly lower levels ($p<0.05$) (Table 1). The presence of connective tissue in the bone marrow was not significantly different ($p>0.05$) among the biomaterials used for filling bone defects (Table 1).

**Qualitative Analysis**

The qualitative analysis was based on images of three-dimensional reconstructions obtained by cone-beam computer tomography. They showed that the cavities filled with Bio-Oss® and Endobon® Xenograft Granules presented higher hyperdensity and better homogeneity. Cavities grafted with Straumann® Bone Ceramic showed greater qualitative irregularities. The control (coagulum) showed hypodense images of the defects (Fig. 3).

**Discussion**

When the study objective is to evaluate bone healing in an animal model using bone substitutes, it is essential to verify whether the substituted material complied with the concept of “critical size defects”. This concept has different thresholds according to the animal species and the site of the defect. Using standardized defects of 8 mm diameters in the parietal bones of rabbit calvariae allowed large increases in their interface with bone graft materials used in this study. This was a reasonable choice with previously shown experimental results (14). This region was also important because of its similar embryological origin and morphology to the maxilla, as well as its limited anatomic area of mechanical stress and relative stability of the neighboring structures, both of which make it ideal for evaluating osteogenesis induced by biomaterials (15). A period of eight weeks was appropriate to assess late repair, including new bone tissue resorption of the graft material, bone remodeling and bone regeneration (16).

In the present study, morphometric analysis and cone-beam computed tomography showed that the biomaterials induced new bone formation after eight weeks, indicating that they have osteoconductive properties. In addition, alloplastic biomaterials presented greater levels of newly formed bone in compared to deproteinized bovine bone. These results are similar to that obtained when Bio-Oss® was compared over the same observation period, which is based on biphasic calcium phosphate with the same composition (HA/β-TCP in a proportion of 60/40) in shapes of “donut” granules at the submicron level (i.e., from 300–400 μm pores for central particles 0.8 mm) (MegaGen Implant, Kyungsan, Korea) (17). However, different results were observed in studies assessing maxillary sinus membrane elevation (11, 18) and in those studying rabbit calvariae after eight weeks involving defects of standard 6.5mm diameter (5). These studies found no statistically significant differences in the levels of newly formed bone tissue induced by these biomaterials.

Xenogenous biomaterials showed similar behavior, both in the amount of newly formed bone, as the amount of residual graft. The results can be explained by the origin of the materials tested, as both were of bovine origin, were deproteinized and lyophilized, had similar granule diameters (Bio-Oss®, 250–1000μm and Endobon® Xenograft Granules, 500–1000 μm) and had similar porosity (Bio-Oss® between 75% and 80% 8 and Endobon® Xenograft Granules between 45% and 85% (BIOMET 3i ™).
The results of the present study were similar to those reported by Tovar et al. (19), which compared the Bio-Oss®, OsteoGraf N-300® (Dentsply International, York, PA, USA), and two variations a newly developed biomaterial (Dentsply International, York, PA, USA). After eight weeks of evaluation, no statistical difference in the amount of newly formed bone was observed.

The biomaterial based biphasic calcium phosphate showed a lower amount of residual grafting (p<0.05) compared with biomaterials consisting of deproteinized bovine bone. The result was similar to that found in a study that evaluated the behavior of the Straumann®Bone Ceramic and Bio-Oss® in elevation of the floor of the maxillary sinus surgery (11).

Several studies have shown that the presence of residual graft when using biomaterials based on deproteinized bovine bone is due to its slow resorption (8,10,20,21). Traini et al. (20) suggest that the difficulty of resorption of Bio Oss® is related to its high content of calcium and absence of proteins. In the study by Ramirez-Fernandez et al. (21), performed in tibiae of rabbits, Endobon®Xenograft Granules was less absorbable than from swine OsteoBiol®mp3 (TECNOSS srl, Giaveno, Italy). In the alloplastic biomaterials based biphasic calcium phosphate (HA/β-TCP ratio 60/40), the β-TCP constituent is quickly resorbed and replaced with natural bone provided faster remodeling, while the HA constituent slower resorbed, allowing the preservation of the bone volume (11,12). Other studies showed an increased resorption of β-TCP compared to HA (ratio 60/40) (22, 23) and no change in the ratio of 20/80 (24).

Cavities filled with blood clot had morphometrically greater amount of newly formed bone tissue than the cavities filled with biomaterial-based bovine bone (p<0.05) and similar to the amount found in cavities filled with biomaterial-based phosphate biphasic calcium (p>0.05). This result was also observed by Rokn et al. (5), which suggest that this may be related to the repositioning and suturing of the periosteum during surgical procedures, acting as natural membrane, inducing guided tissue regeneration. Other studies in rabbits calvaria, also showed neofomed bone tissue similar between the clot and the platelet-rich plasma (13) and between the clot and biodegradable gelatin hydrogel (25). Borie et al. (15) shows that the clot had lower bone formation compared to autogenous bone and human bone allogenic in rabbit calvaria.

Despite the differences with the control group, only the coagulum is not effective in the clinical setting. In augmentation procedures involving implant placement, thickness or height of the alveolar bone is important; as such, coagulum is less than ideal because it lacks resistance to compression from the soft tissue. For such procedures, it is essential for the graft material to have osteoconductive properties (i.e., it should be able to create structural support for new bone formation), suggesting the importance of evaluating biomaterials used for this purpose.

Three-dimensional reconstructions by cone-beam tomography showed that the cavities with bovine bone presented higher hyperdensity, more homogeneous and smaller amount of new bone, while cavities with biphasic calcium phosphate showed greater irregularities, but larger amounts of new bone. These results may be related to the greater amount of residual graft present in areas that received xenogenous biomaterials. The presence of more such biomaterials, which have slow resorption (20), could provide images with greater regularity than in areas with the greatest amount of new bone. These reconstructions have also shown that cavities with blood clot showed no filling at the center of the surgical defect. These results suggest that the newly formed bone is concentrated at the edges surgical defect, reinforcing the clinical argument that in cases of bone reconstruction a bone substitute with osteoconductive feature is necessary.

The results of this study showed that there is a need for further studies to assess biomaterials that are more effective in the process of bone induction than those used in this study. Both qualitative and quantitative techniques are warranted to better interpret the results as they relate to clinical applicability. In conclusion, the obtained outcomes suggest that all biomaterials induced bone formation after eight weeks. Although the alloplastic biomaterial induced more bone formation, further studies are essential to prove what type of biomaterials is more effective in bone induction.

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