Mechanical and Tribological Properties of Ti-Containing Carbon Nanocomposite Coatings Deposited on TiAlV Alloys

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Received: September 1, 2010; Revised: December 3, 2010

Ti-doped carbon coatings were deposited on TiAlV alloys by reactive dc-magnetron sputtering in Ar/CH₄ mixed gas. When Ar flow increases the incorporation of Ti into films raises while the concentration of C decreases. The formed nanometric TiC crystals were more noticeable for coatings deposited with higher Ar flows. Hardness (H) and elastic modulus (E) of coatings were measured by nanoindentation. H values were in the range of 8.8-15.9 GPa and E of 53.4-113.7 GPa. Higher values for H and E were obtained for films containing larger amount of TiC-phase. The presence of TiC crystals increased the coefficient of friction (COF) from 0.07 to 0.28 in scratch tests. Tribological experiments were carried out by using a pin-on-disk apparatus in air and in liquid. COF values ranged from 0.10 to 0.50 for tests in air. Despite of presenting higher COF, tests performed in liquid resulted in less pronounced wear tracks.

Keywords: carbon-based coatings, depth-sensing nanoindentation, mechanical properties, tribology, wear

1. Introduction

Carbon-based films have been studied since 1971, when Aisenberg and Chabot1 produced diamond-like carbon thin films by ion-beam deposition technique. The amorphous structure may lead to coatings with a wide range of properties, once these materials can present the main characteristics of both diamond and graphite carbons. Hardness is generally linked to a C sp³-hybridized network that surrounds small C sp²-hybridized islands in amorphous-carbon. In fact, the properties of carbon-based films are mostly influenced by the content and how C sp² and sp³ hybridizations are arranged, as well as the amount of H into amorphous-carbon matrix2. Additionally, some foreign elements (for example, Ti, Si, O and F) are frequently incorporated into the amorphous matrix in order to tailor the properties of the coatings3,4. Hence a considerable variety of carbon-based films can be produced as far as the nano/micro-structure, chemical composition, optical, mechanical and tribological properties are concerned. These films are usually prepared by several deposition techniques, such as ion deposition, ion assisted sputtering, cathodic vacuum arc, sputtering, plasma deposition and pulsed laser deposition2.

Nanocomposite coatings can be formed by small crystallites embedded in an amorphous matrix5. In general, hard crystallites (for instance, carbides, oxides and nitrides) dispersed into a softer matrix material can reduce the compound hardness and elastic modulus, but the nanocomposite coating becomes tougher6,8. Therefore the presence of these crystals as a second phase is an important parameter that must be taken into account for predicting the properties of nanocomposite coatings. For example, hard titanium carbide (TiC) crystals embedded into a-C:H matrix can improve the wear resistance of coatings7,9. The small TiC crystals are, to a certain extent, responsible for the good fracture toughness of nanocomposite coatings, while the soft carbon-based matrix accounts for the self-lubrication properties6. TiC-containing carbon composite films have been widely studied by several authors for many different purposes6,10-12.

Nowadays carbon-based coatings attract interest for applications as protective coatings in many areas, such as magnetic storage disks, sliding bearings, gears, manufacturing tools, polyethylene terephthalate (PET) bottles, in textile and biomedical industries13,14. They can present low coefficient of friction15 and reduced wear rate, being good candidates for tribological applications. The interposition of wear debris between the femoral head and socket (counter-part) of total hip prostheses (THP) is one of the main factors for implants failures, as reported by many orthopaedic surgeons16. They often provoke bone-resorption (osteolysis), undesirable tissue reactions, and then aseptic loosening of THP16. A number of devices for bio-tribology studies have been employed to evaluate the wear and frictional properties of candidate materials to THP. The most common used apparatuses are pin (ball)-on-disk and pin (ball)-on-flat, which allow to control the applied normal force, angular velocity, and lubrication medium as well17,19. The development and use of more sophisticated equipments with multi-directional movements provide a better mimicking of both natural knees and hip joints20,21. Notwithstanding, cheaper and easier systems, like ball-on-disk apparatus, can be satisfactorily used as a first evaluation of wear on different materials. Several lubricants are usually applied for tribological tests in liquid, for instance: water21, Ringer’s and NaCl solutions22, natural synovial fluid23, bovine and caprine femoral serum24,25. Results from wear tests carried out in joint simulators, using bovine or caprine serum solution as lubricant medium, showed better agreement with clinical uses with respect to the wear volume of THP25.

This work concerns the mechanical and tribological properties of Ti-doped carbon nanocomposite films. Coatings were deposited on TiAlV alloy by reactive dc-magnetron sputtering under different conditions. Nanoindentation was the main technique used to mechanical characterisations. The tribo-indenter was also used to perform scratch tests. Wear tests were carried out in air and in liquid using a pin-on-disk tribometer.
2. Materials and Methods

Carbon-based films were deposited on commercial TiAlV alloy substrates with dimensions of 20 x 20 x 1.5 mm³. Substrates were mechanically abraded with SiC paper (400, 600, 800 and 1200 grits), and then polished by using a colloidal silica suspension (Struers A/S) in order to obtain mirror-like surfaces. Reactive dc-magnetron sputtering was the technique used for deposition from a pure Ti target with a power density of 1.7 W.cm⁻². A mixture of gases Ar + CH₄ was employed with different (Ar/CH₄) gas flows: 170/50, 190/30, and 210/10 sccm, maintaining the total flow at 220 sccm. All coatings were deposited with a constant applied substrate bias voltage of ~300 V. Titanium inter-layers were deposited to improve the film adhesion on the metallic substrates. For each condition, the deposition time was previously calculated to obtain films 200-300 nm thick.

The concentrations of C, Ti and O in the deposited films were estimated by Auger spectroscopy with an equipment from Physical Electronics model PHI. Samples were previously sputtered with Ar ions of 2 keV for 70 minutes to remove surface contamination. Then measurements were performed with an electron beam of 3 keV and 5 scans for energies in the range 30-600 eV. Concentrations were calculated by using the table of sensitivity factor of elements. Grazing angle X-ray diffraction (XRD) was performed with a Bruker D500 diffractometer with Cu Kα radiation (λ = 1.5106 Å) and an incident angle (θ) of 1°. XRD peaks were identified by using the JCPDS cards nº 01-1198 (Ti), 32-1383 (TiC), and 86-2352 (TiO). The sizes of TiC crystallites were estimated from the Scherrer’s formula. Mechanical properties, namely hardness and elastic modulus, were measured by nanoindentation technique with a Hysitron tribo-indenter. A diamond Berkovich-type tip was employed for calibration, and Poisson’s coefficient of 0.25 was applied to the tribo-indenter. A total of 80 indents were performed on each sample under loads from 0.5 up to 5.0 mN. Values for hardness and elastic modulus shown herein were obtained using the Oliver & Pharr method for the load of 2.55 mN. Also elastic recovery (ER) parameter was calculated for each indentation test by applying the ratio (hₚₘₐₓ – hₚₙₐₓ)/hₚₙₐₓ, where hₚₘₐₓ is the maximum penetration depth (during loading) and hₚₙₐₓ is the final depth penetration (after unloading).

Scratch tests were performed with a Berkovich tip with a maximum applied normal load of 5.0 mN. A total number of 5 scratches (500 nm in length) were performed on each sample at a loading rate of 0.5 mN/s. Figure 1 shows the load and displacement functions applied to the tip. First, the tip was shifted to the initial position, and from this point it travelled 500 nm under a normal load of 0.3 mN in order to obtain the pre-scans (or original surfaces) profiles. Then, the tip was kept loaded under 0.3 mN for 3 sec at this point, and displaced backwards under rising loads from 0.3 up to 5.0 mN for 10 seconds. After that, the tip was unloaded to 0.3 mN during 3 seconds. Finally, the post-scans profiles were collected by displacing the tip towards the final position (500 nm) under the load of 0.3 mN.

The coefficient of friction (COF) was determined by measuring the lateral force (L) during scratching and obtaining the L/N ratio, where N is the applied normal load. Comparisons between pre- and post-scans profiles allowed calculating the elastic recovery for the applied normal loads of 0.5, 1.0, 2.5 and 4.5 mN. For each sample, values were calculated by applying the equation previously mentioned for ER, and thus the average values were obtained from the 5 scratches.

Wear experiments were carried out by using a pin-on-disk tribometer (CSM/Switzerland) in two different media: in air and in bovine serum. An AISI420 steel ball of 6.0 mm in diameter was used as counter-part. An applied normal force of 1.0 N, tangential speed of 0.07 m/s and 50,000 cycles were employed. All experiments were performed at room temperature (RT) and relative humidity of 50-60%. A bovine serum solution with protein concentration of 20 mg.mL⁻¹ was employed as lubricant for tests in liquid medium. A peristaltic pump was used to circulation of liquid during the tests, with a syringe carefully connected to the experimental setup to drop the liquid on the samples. Wear was qualitatively evaluated by optical microscopy by observing the tracks formed on the coatings.

The maximum hertzian contact pressure (pₘₐₓ) for spherical-sphericalpaired surfaces is:

\[ pₘₐₓ = \frac{3}{2} \pi \cdot \frac{P}{a^2} \]  \hspace{1cm} (1)

where \( P \) is the normal applied force, and \( a \) follows the relation given by:

\[ a = \frac{\sqrt[3]{3 \cdot P \cdot R}}{4 \cdot E} \]  \hspace{1cm} (2)

In our case, e.g. spherical-flat paired surfaces, \( R \) is the sphere radius and \( E \) represents the compound elastic modulus:

\[ \frac{1}{E} = \frac{(1-\nu₁)}{E₁} + \frac{(1-\nu₂)}{E₂} \]  \hspace{1cm} (3)

where \( E₁ \) and \( E₂ \) are the elastic moduli, \( ν₁ \) and \( ν₂ \) are the Poisson’s coefficients of the sliding surfaces. From Equation 1 the calculated \( pₘₐₓ \) is around 500 MPa for our experiments, whereas it is approximately 60 MPa for a metal-metal paired orthopaedic prosthesis. Data from Jin et al. were taken in the calculations. Thus, one can conclude that the tribological conditions applied here are more severe than for clinical use.

3. Results and Discussion

Figure 2 shows the estimated concentrations of C, Ti and O obtained from Auger spectroscopy for the produced Ti-doped carbon coatings. Carbon concentration decreased while Ti increased when CH₄ flow was reduced from 50 to 10 sccm. As the CH₄ flow is decreased, argon flow increases leading to a higher sputtering rate of the target and therefore incorporating a larger amount of Ti in the forming carbon-based film. For instance, as the Ar mass flow into the chamber increased from 170 to 210 sccm, the Ti concentration grew about 5-fold in the deposited film. All coatings presented some concentration of oxygen, which may originate from contamination during deposition or post-deposition oxidation.

XRD results for the deposited carbon-based coatings and TiAlV substrate are shown in Figure 3. In general, the incorporation of Ti was responsible for formation of titanium carbide (TiC) crystallites embedded in the amorphous carbon matrix. The presence of TiC peaks is more noticeable for coatings deposited with higher Ar mass flows (210 sccm, for example), which have higher concentration of Ti (Figure 2). The formed TiC-phase has polycrystalline structure with main peaks TiC (111) at 35.9°, TiC (200) at 41.7°, and TiC (220) at 60.4°. The growth of the peak intensity is related to the increase of the amount of TiC crystals in the amorphous matrix. Additionally, films prepared with (Ar/CH₄) flows of 190/30 sccm presented a peak around 64.0°, which corresponds to pure titanium. Calculations from Scherrer’s formula showed that the TiC crystallites have nanometric sizes ranging from 2.0 to 6.0 nm, with increasing size for higher Ti concentrations. On the other hand, TiC peaks were not clearly observed for films produced at higher CH₄ mass flow (50 sccm), which presented low Ti concentration (Figure 2). The amount of TiC-phase in the carbon matrix thus seems to grow when C (Ti) concentration
is reduced (increased). It is worth mentioning that XRD peaks for Ti$_x$O$_{x-1}$ are positioned very close to the peaks for TiC. Therefore, the contribution of TiO phases in the carbon matrix for the observed XRD results cannot be ruled out. Furthermore, the assessment by the Scherrer’s formula is mostly an estimation, once the broadening of the XRD peaks is usually under influence of the instrumental- and specimen-related effects, such as the variability in shape and size of the crystallites.

Hardness ($H$) and elastic modulus ($E$) of the coatings were measured by instrumented indentation at nano-scale. Table 1 displays the $H$ and $E$ values measured for a normal load of 2.55 mN, which allowed to maximum contact depths in the range of 43 – 67 nm. Both measured values for $H$ (~4 GPa) and $E$ (~120 GPa) of the polished TiAlV substrate are in good accordance to the literature. The deposited nanocomposite films present compound hardness ranged from 9 up to 16 GPa. Hardness increases when CH$_4$ flow in the gaseous mixture decreases. In fact, the films containing higher (lower) concentration of Ti (C) are the hardest ones.

Based on the XRD results (Figure 3) and the measured hardness, the greater presence of TiC-phase in the carbon matrix led to deposit harder films. When the carbon concentration increases in comparison to titanium (Figure 2), TiC crystals decrease in size, as determined from the Scherrer’s formula calculation. Moreover the TiC crystallites separation enlarges in the amorphous carbon matrix. Then the amorphous carbon-phase can dominate the mechanical behaviour, decreasing the hardness of TiC-containing carbon nanocomposite films.

Of course, in our case, other parameters can act simultaneously on the compound hardness, such as hydrogen content in the amorphous carbon matrix. Hydrogen can saturate the C = C bonds in the amorphous C:H matrix, increasing the C $sp^3$ content and therefore affecting the hardness of the coating. On the other hand, the formation of TiC grains can lead to an increasing of $sp^2$ sites into amorphous carbon matrix.

**Table 1.** Contact depth ($h$), hardness ($H$), elastic modulus ($E$), and elastic recovery ($ER$) of produced Ti-doped carbon films measured by nanoindentation for a load ~ 2.55 mN (mean value ± standard deviation)*.

<table>
<thead>
<tr>
<th>Ar/CH$_4$ (sccm)</th>
<th>$h$ ± SD (nm)</th>
<th>$H$ ± SD (GPa)</th>
<th>$E$ ± SD (GPa)</th>
<th>$ER$ ± SD (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>170/50</td>
<td>67.0 ± 3.8</td>
<td>8.8 ± 0.7</td>
<td>53.4 ± 9.6</td>
<td>87.4 ± 0.5</td>
</tr>
<tr>
<td>190/30</td>
<td>53.0 ± 1.5</td>
<td>12.1 ± 0.5</td>
<td>113.7 ± 2.5</td>
<td>85.2 ± 1.5</td>
</tr>
<tr>
<td>210/10</td>
<td>43.4 ± 3.5</td>
<td>15.9 ± 1.6</td>
<td>113.6 ± 19.5</td>
<td>82.7 ± 4.0</td>
</tr>
</tbody>
</table>

*n = 16.
Concerning the elastic modulus, the films produced with (Ar/CH\textsubscript{4}) mass flow of 170/50 sccm have the lowest value. For the films deposited in higher Ar flows, it was not found significant differences between the values, as shown in Table 1. As mentioned for hardness, the larger presence of TiC crystals again increased the elastic modulus.

Besides to hardness and elastic modulus properties, the elastic recovery (ER) is another interesting parameter that might predict, to a certain extent, the wear resistance of materials. It is worth noting that when Ti increases the ER decreases slightly (Table 1), reaching values as low as 82%. In fact, carbon-based films can have high ER values, as those previously reported by Chowdhury and colleagues\textsuperscript{33}. For tough films, Voevodin and co-workers\textsuperscript{6,7} have reported that a good value for ER would be 60%.

Nanoindenter is not only a versatile equipment for measuring \(H\) and \(E\) of materials, but also for tribological experiments at smaller scales. This is especially attractive for thin films, where the influence of substrate on the measurements must be avoided. The coefficient of friction (COF) and penetration depths during scratch tests using the nanoindenter are shown in Figure 4. Results correspond to the average value for COF (and penetration depth) calculated from 5 tests at different scratch lengths (and normal loads). For all samples, the COF increases when both normal load and penetration depth increase. COF values could be as low as 0.07 for shallow depths and increase up to ~0.27 at higher loads (4.5 mN).

The COF values increase as the methane flow is reduced which corresponds to higher concentration of Ti into carbon films, that is, the presence of TiC crystallites into carbon matrix increased the COF values. These TiC crystals are usually covered by a-C:H layers in the amorphous carbon matrix, which is responsible for the self-lubrication, and consequently, influence the COF of carbon-based films\textsuperscript{9}. Then coatings containing lower TiC/a-C:H rate should present lower COF, as seen in Figure 4. Films prepared in Ar/CH\textsubscript{4} (210/10 sccm), which probably have larger amount of embedded TiC crystals (see Figure 3), have the shallowest penetration depths for all loads, which is related to the fact that these films are the hardest ones among those produced here (Table 1). These coatings are therefore more resistant to scratches (under low normal loads) compared to those produced with lower argon flows.

Results for elastic recovery (ER) of coatings after scratching tests are shown in Table 2. The values for ER correspond to the selected normal loads of 0.5, 1.0, 2.5, and 4.5 mN. As previously mentioned for indentation tests, all deposited coatings had high values for ER.

<table>
<thead>
<tr>
<th>Ar/CH\textsubscript{4} (sccm)</th>
<th>0.5 mN</th>
<th>1.0 mN</th>
<th>2.5 mN</th>
<th>4.5 mN</th>
</tr>
</thead>
<tbody>
<tr>
<td>170/50</td>
<td>94 ± 3</td>
<td>90 ± 1</td>
<td>85 ± 1</td>
<td>84 ± 2</td>
</tr>
<tr>
<td>190/30</td>
<td>85 ± 5</td>
<td>81 ± 2</td>
<td>81 ± 1</td>
<td>83 ± 1</td>
</tr>
<tr>
<td>210/10</td>
<td>89 ± 11</td>
<td>76 ± 4</td>
<td>75 ± 5</td>
<td>93 ± 5</td>
</tr>
</tbody>
</table>

Table 2. Elastic recovery (ER) of produced carbon coatings obtained from scratch tests for different normal loads (mean value ± standard deviation)*.

*n = 5.

![Figure 4](image-url). Variation of coefficient of friction (COF) and penetration depth of the Ti-doped carbon films submitted to scratch tests under rising loads up to 5 mN. Coatings were prepared with different (Ar/CH\textsubscript{4}) mass flows (in sccm). A total of 5 scratches were performed on each sample. Lines are guides to the eyes.

![Figure 5](image-url). Variation of coefficient of friction (COF) of produced coatings from wear tests carried out by using pin-on-disk apparatus (a) in air; and (b) in liquid. Coatings deposited with different Ar/CH\textsubscript{4} flows (in sccm).
(75 - 94%) obtained from scratch tests. In general, the ER seemed again to decrease when the presence of TiC-phase in the coatings was increased. Due to the high elastic recovering of the carbon nanocomposite coatings, it was not possible to observe the scratches, even at higher loads (or depths).

Figure 5 shows the COF of the coatings for tribological tests carried out by pin-on-disk apparatus in air and in liquid (bovine serum). Figure 5a does not show the result for the coatings prepared with (Ar/CH₄) flow of 210/10 sccm due to the strong damage observed after a few cycles of test. In general, the COF values varied in the range of 0.10 - 0.18 and 0.22 - 0.50 for coatings produced with Ar/CH₄ flows of 190/30 and 170/50 sccm, respectively. This variation could be associated to the hard debris interposed between the sliding surfaces. Despite of having higher concentration of carbon in relation to titanium (see Figure 2), films deposited with CH₄ flow of 50 sccm showed higher COF values, which probably generated larger amount of wear debris.

<table>
<thead>
<tr>
<th>Ar/CH₄ (sccm)</th>
<th>In air</th>
<th>In liquid</th>
</tr>
</thead>
<tbody>
<tr>
<td>170/50</td>
<td><img src="image1.png" alt="Image" /></td>
<td><img src="image2.png" alt="Image" /></td>
</tr>
<tr>
<td>190/30</td>
<td><img src="image3.png" alt="Image" /></td>
<td><img src="image4.png" alt="Image" /></td>
</tr>
<tr>
<td>210/10</td>
<td><img src="image5.png" alt="Image" /></td>
<td><img src="image6.png" alt="Image" /></td>
</tr>
</tbody>
</table>

**Figure 6.** Optical micrographs of tracks formed on the coatings after 50,000 cycles for the tribological tests in air and in liquid (bovine serum).
For tribological tests performed in bovine serum, the COF values appeared to increase up to 6,000 cycles, and then varied around an average value (Figure 5b). Also these values were higher compared to tests in air (Figure 5a). These findings were not expected once the bovine serum should act as a lubricant, decreasing the friction between the sliding surfaces as will be discussed hereafter.

Figure 6 shows the optical micrographs of typical tracks formed on the coatings submitted to tribological tests in air and in liquid. For tests in air, accumulation of wear debris along the tracks is observed on the samples. Further, the tracks become wider when the argon flow increases, that is, films prepared with lower methane flows are less wear-resistant. This could explain the substantially high COF obtained for the coatings deposited with Ar/\text{CH}_4 flows of 210/10 sccm, which were completely damaged. In all cases, the tracks formed on the coatings are narrower for tests in liquid compared to tests in air. This indicates that coatings were less damaged in tests in bovine serum, despite of having higher COF values in liquid (Figure 5). The proteins crystallization in bovine serum possibly influences the tribo-chemical reactions, increasing the COF between the sliding surfaces. For the tribological parameters used here, the coatings deposited with Ar/\text{CH}_4 flows of 170/50 sccm are thus more wear-resistant.

Comparing the results for ER from Tables 1 and 2 with the results from Figure 6, one can observe that those coatings with higher ER values were less damaged. Therefore one could speculate that ER and wear of the nanocomposite coatings are related, once high ER values implies a more elastic material. But one must be careful of predicting wear by using the elastic recovery data, because the tribological system involves several important parameters that influence the final results, such as lubrication, environment, sliding surface pairs, load, velocity, etc.

Some works have pointed out that the presence of hard TiC crystals can improve the tribological properties of carbon-based films. In fact, the arrangement and size of the TiC crystals, as well as the growth mode of the carbon films (columnar or compact, for instance) are responsible for the changes on the final properties of coatings. In our experiments, the presence of larger TiC nano-crystals did not seem to contribute to the wear resistance of coatings, as reported in the literature for TiC/a-C coatings. The thicknesses of films about 300 nm possibly played an important role on the wear behaviour, once the applied hertzian contact pressure was considerably high. Hence a greater improvement of wear due to the presence of TiC crystals would be probably observed for thicker nanocomposite coatings. Even so, by taking into account the severe tribological conditions that they were submitted to, the nanocomposite coatings could be considered to tests on load bearing surfaces, such as hip joint simulator systems.

4. Summary and Conclusions

In this work, Ti-containing carbon coatings were prepared by reactive dc-magnetron sputtering. According to the (Ar/\text{CH}_4) mass flows applied to deposition, the concentrations of C and Ti into nanocomposite coatings changed. For higher Ar flows, the concentration of Ti (C) raised (decreased) and the presence of nanometric-sized TiC crystals was observed. Hardness (H) values were in the range of 8.8 – 15.9 GPa, and elastic modulus (E) of 53.4 - 113.7 GPa measured by nanoindentation tests. Higher H and E were obtained for nanocomposite films containing larger amount of TiC-phase. The presence of TiC crystals into carbon matrix increased the obtained coefficient of friction (COF) from 0.07 to 0.28 during scratch tests under low loads. All nanocomposite coatings had elastic recovery (ER) of at least 75% for both nanoindentation and scratch tests. COF values obtained for wear tests in air varied in the range of 0.10 – 0.18 and 0.22 - 0.50 for films produced with Ar/\text{CH}_4 flows of 190/30 and 170/50 sccm, respectively. The deposited films presented higher COF values for wear tests in bovine serum, but the wear tracks were less marked in all cases. In addition, coatings with larger presence of TiC crystals had wider wear tracks formed on their surfaces. Notwithstanding, the produced TiC-doped carbon coatings could be tested as protective coatings on load bearing surfaces in aqueous medium.

Acknowledgments

Authors are grateful to the financial support from CNPq, CAPES and FAPERJ Brazilian funding agencies. Also thanks are due to Dr. D. Martínez-Martínez and Dr. O. Kubová for their experimental helping.

References