Validity of a new stabilometric force platform for postural balance evaluation

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Abstract – The objective of this study was to validate a new stabilometric force platform (SFP). For this, three steps have been established: a) to determine the force threshold to reach an acceptable level of accuracy of the centre of pressure (CoP) measurement by the application of single point load; b) to determine the accuracy of the CoP measurement in the application of distributed load simulating the human feet; c) to verify the concurrent validity of the SFP by comparing it with a commercial force platform (FP). The tests performed in steps “a” and “b” were conducted by applying loads on the SFP using a universal testing machine. In the application of single point load, the mean force threshold presented by the SFP was 315.6 ± 140.5 N. The CoP measurement error in the points near the centre of the SFP was 1.04 ± 0.80 mm in medial-lateral (ML) and 1.31 ± 0.99 mm in anterior-posterior (AP) direction. In the points near the edges of the plate, the error was 2.03 ± 0.91 mm (ML) and 1.54 ± 0.96 mm (AP). In the test with distributed loads, errors of less than 1 mm were found. Additionally, no differences were found in the CoP parameters between SFP and the FP. The CoP measurement signal presented high correlation between both equipments in AP (r = 0.997 ± 0.001) and ML (r = 0.988 ± 0.003) directions. These findings suggest that the SFP can be used in scientific investigations of balance in quiet standing.

Key words: Biomechanics; Postural balance; Instrumentation.

Resumo – O objetivo deste estudo foi validar uma nova plataforma de forças estabilométrica (PFE). Para isso, três etapas foram estabelecidas: a) determinar o limiar de carga para chegar a um nível aceitável de exatidão da medida do centro de pressão (CP) pela aplicação de cargas pontuais; b) determinar a exatidão da medida do CP na aplicação de cargas distribuídas que simulam os pés humanos; c) verificar a validade concurrente da PFE comparando-a com uma plataforma de forças comercial (PF). Os testes das etapas “a” e “b” foram realizados pela aplicação de cargas sobre a PFE, utilizando uma máquina de ensaios universal. Na etapa de aplicação de carga pontual, a média do limiar de carga apresentado pela PFE foi de 315.6 ± 140.5 N. Os erros de medida do CP nos pontos próximos ao centro da PFE foram de 1.04 ± 0.80 mm na direção medio-lateral (ML) e 1.31 ± 0.99 mm na direção ântero-posterior (AP). Nos pontos próximos aos cantos da chapa, foram encontrados erros de 2.03 ± 0.91 mm (ML) e 1.54 ± 0.96 mm (AP). No teste com cargas distribuídas, os erros foram menores que 1 mm. Adicionalmente, não foram encontradas diferenças nos parâmetros do CP entre a PFE e a PF. O sinal do CP apresentou alta correlação entre os dois equipamentos, tanto na direção AP (r = 0.997 ± 0.001) quanto na direção ML (r = 0.988 ± 0.003). Os resultados sugerem que a PFE pode ser utilizada em estudos científicos do equilíbrio em postura ereta.

Palavras-chave: Biomecânica; Equilíbrio postural; Instrumentação.
INTRODUCTION

Stabilometric evaluation involves the analysis of the centre of pressure (CoP), which reflects the net motor pattern at the ankle and consequently the response of the central nervous system to correct the imbalance of the body’s center of mass\(^1,2\). Several studies\(^3,7\) use the CoP displacement as an indication of stabilization mechanisms and postural control during standing position.

Force platforms (FP), which are complex and precise systems\(^8\), are commonly used to measure the CoP. However, these equipments have a high cost, especially when imported by research groups that have limited financial resources. In order to make it possible for our group to conduct balance researches in quiet standing, a less expensive alternative was used by building a stabilometric force platform (SFP), which calculates the CoP by the measurement of the vertical reaction force, like others with the same principle found in literature\(^1,9,10\). However, a validation process of this system had to be carried out, so that it could be used in scientific studies.

Regarding the FP validity, the parameters that are usually verified are accuracy\(^11-14\) and force threshold\(^15\) of the CoP measurement. In general, these parameters are verified by the application of single point load\(^14,16\), by the application of distributed load\(^14,17\) and by comparison with a commercial FP\(^1,18\). Therefore, the objective of this study was to validate the SFP. For this, three steps have been established: a) to determine the force threshold to reach an acceptable level of accuracy of the CoP measurement; b) to determine the accuracy of the CoP measurement in the application of distributed load simulating the human feet; c) to verify the concurrent validity of the SFP by comparing it with a commercial FP.

METHODS

The stabilometric force platform

The SFP is composed of two parts: the dynamometric structure and the data acquisition system. The dynamometric structure (Figure 1) was developed using two rectangular steel (AISI 1020) plates (0.5 x 0.39 x 0.0125 m), and four uniaxial load cells with capacity of up to 1 kN (Gefran® TU-K1C) placed in each corner of the plates, equidistant 0.03 m from the edges. A contact system was created to connect the two plates (Figure 1). This structure was designed to ensure that only four points of the upper plate make contact, one in each corner (approximately 1 mm\(^2\)), with the load cells placed on the lower plate, avoiding the interference of horizontal forces, thus minimizing the hysteresis effects and errors in vertical reactions.

The data acquisition system consists of a DC four-channel amplifier and a microcontroller system with 10 bits A/D of resolution. The system is supplied by rechargeable battery. The USB port is used for the data transmission to the PC. Software for data acquisition was developed for this equipment.

In triaxial FP, as the AMTI\(^9\), the CoP location, in the anterior-posterior (AP) and medial-lateral (ML) directions, is usually calculated using the following equations\(^15\):

\[
\text{CoP}_{AP} = \frac{M_{ML}}{F_z} \quad (1)
\]

\[
\text{CoP}_{ML} = \frac{-M_{AP}}{F_z} \quad (2)
\]

where \(M_{ML}\) and \(M_{AP}\) are the moments around medial-lateral and anterior-posterior components respectively and \(F_z\) is the vertical component of the force. However, for the SFP, which has four uniaxial load cells arranged in a rectangular shape, \(F_z\) is considered to be equal to the sum of vertical reaction forces of each load cell. Considering that \(\sum \text{Moments} = 0\) and \(\sum \text{Forces} = 0\), the CoP must be located exactly at the centre of the system. Thus, the CoP location was calculated by the following equations\(^19\):

\[
\text{CoP}_{AP} = \frac{x}{2}(F_1+F_4) - (F_2+F_3) / F_z \quad (3)
\]

\[
\text{CoP}_{ML} = \frac{y}{2}(F_3+F_4) - (F_1+F_2) / F_z \quad (4)
\]
where x and y correspond to the width and length of the usable area in the SFP, respectively, F is the vertical reaction force of each load cell, $F_z$ is the sum of $F_1$, $F_2$, $F_3$ and $F_4$. This equation is appropriate to systems with four uniaxial load cells arranged in a rectangular shape.

**Force threshold**

This test was performed to verify the sensitivity (force threshold) of the CoP measurement to the load applied. To do so, a test grid, with squares of 3 cm, was carefully drawn using a digital calliper (error ± 0.05 mm) performing a matrix (11 x 15) of 165 points on the usable area of the SFP surface, which were considered as the reference positions. The test consisted of the application of single point dynamic loads from 0 to 700 N at 100 mm/s on each point of the test grid using an universal testing machine (DL-3000, EMIC, Brazil), a load cell with capacity of up to 5 kN and a mechanical structure that applies the load in 1 mm² (Figure 2).

The data was acquired at a sampling frequency of 100 Hz. The force threshold was the minimal load necessary for the CoP measured to reach the reference position on the test grid (CoP predicted) with standard deviation (SD) of up to 3 mm in both directions. The error was calculated by subtracting the CoP measured from the CoP predicted. The SD range was first used by Chockalingam et al. and it was considered as an acceptable level of accuracy for the application of single point load. Figure 3 shows the method to establish the force threshold. The sensitivity of the CoP measurement to the load applied on the 165 points drawn on the test grid was classified into the following categories: 72-150 N; 151-250 N; 251-450 N; 451-650 N and undefined. The mean error of the CoP ML and CoP AP was calculated for each of the categories.

**Distributed load test**

The tests were performed to determine the accuracy of the CoP measurement during the application of distributed load to simulate the load applied by the human feet in stabilometric evaluations. For this, the same structure of the previous test was used, with the addition of two metal feet positioned on the platform (Figure 2). With this test, the CoP location was measured for five seconds with the application of a static load. This experiment was performed in four distance conditions between the two metal feet (60, 120, 180, 240 mm). The feet were aligned in relation to the center of SFP so that the expected CoP location (CoP predicted) was exactly at the geometric center of the plate (0,0). Four trials for each load and position with a 30 s interval between them were conducted. The mean
and standard deviation of CoP<sub>AP</sub> and CoP<sub>ML</sub> location in each condition were calculated to determine the accuracy of the CoP measurement.

**Concurrent Validity**

In this step, the SFP was compared with a previously calibrated AMTI® FP (Model OR6-7-2000, Advanced Mechanical Technology, INC, USA), as performed by Grabiner et al. For this, the SFP was placed on the center of the FP and a trigger was used to start the instruments with synchronism. Five volunteers (30.8 ± 11.5 years old; height of 1.71 ± 0.09 m; body mass of 69.6 ± 15.1 kg) participated of this experiment. All the procedures were approved by the Ethics Research Committee involving human beings (Santa Catarina State University, protocol number 199/2008).

The subjects were instructed to stand barefoot and quietly on the SFP for 20 seconds, with arms relaxed on the side of their bodies and to look at a target placed at a distance of 1.5 m from the subject, at eye level. The CoP was acquired at a sampling frequency of 100 Hz in both equipments. The following stabilometric CoP<sub>AP</sub> and CoP<sub>ML</sub> parameters were calculated for each subject with algorithms implemented in the Scilab software (v. 4.1.2; INRIA, France): root mean square (RMS), amplitude (AMP), mean velocity (MV) and area of the 95% confidence ellipse (AREA). To better analyze the CoP signal, the mean signal was removed and filtered in a low-pass filter (4th order Butterworth, 8Hz cut-off). Additionally, in the equations used to calculate the CoP of the AMTI® FP (equations 1 and 2), the height of the SFP was considered. The Wilcoxon test was used to compare the stabilometric parameters between SFP and FP. Later, the correlation between the raw CoP signal (CoP<sub>AP</sub> and CoP<sub>ML</sub>) of both systems (SFP and the FP) for each subject was verified by the Pearson’s correlation test. All statistical analyses were performed using SPSS for Windows (v. 14; SPSS Inc., USA), at a significance level of 0.05.

**RESULTS**

The force threshold of all points ranged from 73.1 N to 659.5 N (mean of 315.6 ± 140.5 N); 7.8 % of those presented force threshold of 72-150 N with CoP<sub>ML</sub> error = 1.04 ± 0.80 mm and CoP<sub>AP</sub> error = 1.31 ± 0.99 mm; 20.7 % presented force threshold of 151 – 250 N with CoP<sub>ML</sub> error = 1.67 ± 0.95 mm and CoP<sub>AP</sub> error = 1.60 ± 0.96 mm; 34.5 % presented force threshold of 251 – 450 N with CoP<sub>ML</sub> error = 1.81 ± 0.95 mm and CoP<sub>AP</sub> error = 1.66 ± 0.90 mm; 12.7 % presented force threshold of 451 – 660 N with CoP<sub>ML</sub> error = 2.03 ± 0.91 mm and CoP<sub>AP</sub> error = 1.54 ± 0.96 mm and in 24.2%, the force threshold could not be established (error > 3 mm). Figure 3 shows the distribution of all points of the test grid on the force threshold categories. According to Figure 3, when the point is closer to the edges of the platform, the CoP measurement error and the force threshold tend to increase.

In the distributed load test, the CoP measurement error for the different distances of the metal feet was smaller than that observed in the test of the application of the single point load. The force threshold of 30 ± 3 mm was 150 N and to reach CoP<sub>AP</sub> of 30 ± 3 mm was 140 N; therefore, the force threshold was 150 N.
Table 1. Mean and standard deviation of the differences (error) between CoP<sub>predicted</sub> and CoP<sub>measured</sub> in both directions in the distributed load test.

<table>
<thead>
<tr>
<th>Distance between the metal feet (mm)</th>
<th>CoP&lt;sub&gt;AP&lt;/sub&gt; (mm)</th>
<th>CoP&lt;sub&gt;ML&lt;/sub&gt; (mm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>60</td>
<td>0.24 ± 0.21</td>
<td>0.37 ± 0.20</td>
</tr>
<tr>
<td>120</td>
<td>0.35 ± 0.26</td>
<td>0.34 ± 0.32</td>
</tr>
<tr>
<td>180</td>
<td>0.37 ± 0.31</td>
<td>0.84 ± 0.48</td>
</tr>
<tr>
<td>240</td>
<td>0.17 ± 0.13</td>
<td>0.72 ± 0.36</td>
</tr>
</tbody>
</table>

The results of the concurrent validity test between FP and SFP showed that the stabilometric parameters of the CoP measured by both systems do not present significant differences, as shown in table 2.

Table 2. Comparison of the stabilometric parameters between AMTI® Force platform (FP) and Stabilometric force platform (SFP).

<table>
<thead>
<tr>
<th>Variables</th>
<th>(mean ± SD)</th>
<th>FP</th>
<th>SFP</th>
</tr>
</thead>
<tbody>
<tr>
<td>RM5 - CoP&lt;sub&gt;AP&lt;/sub&gt; (mm)</td>
<td>3.84 ± 2.35</td>
<td>3.76 ± 2.37</td>
<td></td>
</tr>
<tr>
<td>AMP - CoP&lt;sub&gt;AP&lt;/sub&gt; (mm)</td>
<td>18.57 ± 14.06</td>
<td>17.88 ± 14.07</td>
<td></td>
</tr>
<tr>
<td>VM - CoP&lt;sub&gt;AP&lt;/sub&gt; (mm/s)</td>
<td>13.00 ± 2.30</td>
<td>12.48 ± 1.94</td>
<td></td>
</tr>
<tr>
<td>RM5 - CoP&lt;sub&gt;ML&lt;/sub&gt; (mm)</td>
<td>2.03 ± 0.88</td>
<td>2.01 ± 0.91</td>
<td></td>
</tr>
<tr>
<td>AMP - CoP&lt;sub&gt;ML&lt;/sub&gt; (mm)</td>
<td>9.96 ± 3.23</td>
<td>9.89 ± 3.58</td>
<td></td>
</tr>
<tr>
<td>VM - CoP&lt;sub&gt;ML&lt;/sub&gt; (mm/s)</td>
<td>13.25 ± 2.78</td>
<td>12.78 ± 2.50</td>
<td></td>
</tr>
<tr>
<td>AREA (mm²)</td>
<td>187.59 ± 127.50</td>
<td>183.90 ± 128.44</td>
<td></td>
</tr>
</tbody>
</table>

Root mean square (RMS), amplitude (AMP), mean velocity (MV) and area of the 95% confidence ellipse (AREA).

Additionally, the raw CoP signal of FP and SFP presented a high correlation for all subjects in the AP (r = 0.997 ± 0.001) and ML (r = 0.988 ± 0.003) direction.

**DISCUSSION**

In relation to the force threshold obtained in the application of the single point load, the SFP system showed good sensitivity, however, it was not as sensitive as the commercial FP analyzed by Chockalingam et al.15, which presented a vertical force threshold ranging from 50.5 to 113.7 N, considering the entire area of the FP. For the SFP, it was observed that the sensitivity is higher along the center of the plate, ranging from 72 to 150 N (Figure 3) and lower as it approaches the limits of the usable area, which is a characteristic found by other authors in strain-gauge and piezoelectric FP14,15. The CoP location error also seems to increase in the points farther from the center of the SFP, and the results indicate that the highest error in the majority of points occurs in the ML direction, except for the points in the threshold category ranging from 72 to 150 N. These findings agree with the results found by Chockalingam et al.15 and Gill and O’Connor21, who analyzed an extensometric FP, and Schmiedmayer and Kastner20, who analyzed a piezoelectric FP. This probably occurs due to the AP dimensions, which are smaller when compared to the ML dimensions, influencing the bending stiffness of the FP15,20.

Figure 3 also shows that some points near the limits of the usable area did not reach the established level of accuracy (< 3 mm of SD). This characteristic can be explained by the SFP design, in which the upper plate is not set to the load cells. Thus, when a force is applied in one point on these areas, the load is not well distributed on the plate and, consequently, not well transferred to the four load cells, probably due to imperfections on the plate. This characteristic appears to be negative; however, a system designed in this manner avoids the interference of horizontal forces and reduces the hysteresis effects. Furthermore, to assume that the error found in the tests of application of the single point load will be the same when an individual is standing on the FP might be a mistake, considering that when a distributed load, such as the human feet, is applied on the FP surface, the CoP measurement error tends to decrease12,14. For this reason, in some cases such as the SFP, correction equations of the CoP determined by the application of the single point load, as proposed in some studies16,20, do not seem to be necessary.

This can be confirmed in the distributed load test, which was designed to measure the accuracy of the CoP measurement in a condition that was the closest to reality in the stabilometric evaluations. Table 1 shows errors of less than 1 mm in the CoP location, which are similar to those found by Middleton et al.14 and very close to the mean error values (0.7 ± 0.4 mm) found in the study of Cedraro et al.21, after an AMTI® FP underwent a complex recalibration system. As in the application of the single point load, in the application of distributed load, a higher error in the CoP measurement was also observed in the ML direction; however, not greater than 1 mm, which is within the acceptable error indicated by reference studies.

In the tests performed in the concurrent validity step, no significant differences were found in the CoP parameters measured between SFP and FP (Table 2). Additionally, the raw CoP signal from both systems showed high correlation. Grabiner et al.1 compared a dinamometric system (Chattecx Balance System) with a similar principle as the...
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SFP with a AMTI® FP, obtaining high linearity results, close to those found in the present study. It is important to assert that stabilometric platforms commonly described in literature do not adopt this procedure. The fact that AMTI® FP has been lately considered a reference equipment is important for future studies, so that the results can be compared.

CONCLUSION

In conclusion, despite the difficulties and challenges of building the SFP, it showed an acceptable response. It was possible to verify that even though it presents a higher force threshold than a commercial force platform, which limits the evaluation of individuals with body mass higher than 30 kg, it has acceptable errors for its use in scientific investigations of balance in quiet standing. Additionally, we expect that this work may provide assistance for other research groups that also have limited financial resources, but have enough human resources to develop a force platform similar to that described in the present study.

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REFERENCES


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