

Bond Strength of Experimental Root Canal Sealers Based on MTA and Butyl Ethylene Glycol Disalicylate

Marina Carvalho Prado¹, Nancy Kudsi de Carvalho¹, Rafael Pino Vitti², Fabrício Aulo Ogliari³, Luciana Moura Sassone¹, Emmanuel João Noqueira Leal Silva^{1,4}

This study investigated the bond strength of two experimental root canal sealers based on MTA and butyl ethylene glycol disalicylate: MTAe and MTAe-HA. The reference materials used for comparison were AH Plus and MTA Fillapex. Twenty human upper incisors were selected and one 1 mm slice was obtained from the cervical third of each root. On the coronal surface of each slice, four 0.9 mm wide holes were drilled through the dentine. Standardized irrigation was performed and holes were filled with one of the four tested sealers: AH Plus, MTA Fillapex, MTAe, and MTAe-HA. The filled slices were stored in a PBS solution (pH 7.2) for 7 days at 37 °C. A push-out assessment was performed with a 0.7 mm plunger tip. Load was applied at a crosshead speed of 0.5 mm/min until sealer displacement. The results were expressed in MPa. The Kruskal-Wallis test was applied to assess the effect of each sealer on the push-out bond strength. Mann-Whitney with Bonferroni correction was used to isolate the differences. The alpha-type error was set at 0.05. Significant differences among medians values obtained by materials were observed (p<0.001). AH Plus displayed the highest value of bond strength (p<0.001). In contrast, MTA Fillapex presented the lowest bond strength among all tested sealers (p<0.001). Experimental sealers showed intermediary bond strength values, with no statistical differences between them (p>0.05). In conclusion, experimental root canal sealers presented suitable bond strength outcomes when compared to MTA Fillapex.

¹ PROCLIN Department, School of Dentistry, UERJ - Universidade Estadual do Rio de Janeiro, Rio de Janeiro, RJ, Brazil
²Department of Prosthodontics, Dentistry School, UNITAU - Universidade de Taubaté, Taubaté, SP, Brazil
³Dental Materials Division, School of Dentistry, UFPel - Universidade Federal de Pelotas, Pelotas, RS, Brazil
⁴Department of Endodontics, UNIGRANRIO - Universidade Grande Rio, Rio de Janeiro, RJ, Brazil

Correspondence: Marina Carvalho Prado, Estrada do Campinho, 298, A. Campo Grande, 23070-220 Rio de Janeiro, RJ, Brazil. Tel/ Fax: +55-21-2413-1442. e-mail: marinaprado@dentistas.com.br

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Introduction

Mineral trioxide aggregate (MTA) is a calcium-silicate cement broadly used in endodontics that has vast evidence supporting this material (1). Despite presenting considerable advantages, such as the ability to set in the presence of moisture (1,2), low cytotoxicity (3), bioactivity (1,4,5), restricted microleakage (3), biocompatibility (3), and some antimicrobial activity (1), MTA is not indicated to be used as a root canal sealer with conventional root canal filling techniques, especially because of its setting time (1), working time (1), and difficult handling (1,2) and removal in cases of root canal retreatment (1,2). Thus, several associations have been proposed with the intention to extrapolate the MTA's remarkable balance between biological and physicochemical properties, creating a close-to-ideal sealer (5-8).

MTA Fillapex (Angelus, Londrina, Paraná, Brazil) is a paste-paste calcium-silicate-based sealer designed in an attempt to produce a root canal sealer with the biological and sealing properties of MTA cement (5). Basically, it is composed of MTA, salicylate resin, natural resin, bismuth, and silica. Although the manufacturer claimed that this sealer has adequate working time, easy handling, excellent

radiopacity, and low solubility, it has produced inconsistent results related to biological and physicochemical properties (5,6). MTA Fillapex presents excessive flow ability (6) and has displayed high and long-lasting cytotoxic effects (5). The presence of MTA has not shown to present biocompatibility advantages or to improve bone-tissue repair (8). Moreover, several studies revealed low values for MTA Fillapex's resistance to displacement (7,10). This sealer is used as a reference material mainly because it was the first MTA-containing sealer and it is internationally available and frequently used by clinicians (5,6,9).

Experimental MTA and butyl ethylene glycol disalicylate-based sealers have been proposed (6). These sealers basically contain a base paste (butyl ethylene glycol disalicylate and bismuth oxide) and a catalyst paste (MTA, titanium dioxide, and N-ethyl-o,p-toluenesulfonamide [Resimpol 8], with or without the addition of a calcium phosphate such as hydroxyapatite [HA]). The butyl ethylene glycol disalicylate present in the base paste is a salicylate resin, which is a chemical compound usually found in the content of oils and anti-inflammatory creams (11). The use of derivatives of salicylates resins presenting differences in the molecular structure permit to reach resins/polymers

with different physical characteristics - as handling properties and rheological characteristics (6). Several root canal sealers also exhibit salicylate resin on its composition, such as MTA Fillapex and Sealapex (Sybronendo, Glendora, USA). The experimental sealers containing butyl ethylene glycol disalicylate showed some improved physicochemical properties when compared to MTA Fillapex, such as the working and setting time and the capacity to release calcium ions (6). Nevertheless, their bond strengths to root dentine have not been evaluated yet. This study proposed a recent method of push-out assessment that is capable of increasing the internal validity related to dentine source and standardization of root canal anatomy (9). For that, artificial holes were created in the same dentine source, instead of preparing several teeth presenting different anatomy and analyzing some root regions as it is accomplished in conventional push-out designs (13,14).

In this context, this study investigated the bond strength of two experimental MTA and butyl ethylene glycol disalicylate-based sealers – MTAe and MTAe-HA – with the aim to evaluate their performance in a relevant physical aspect for clinical application, increasing the overall knowledge about these materials that have potential to become a clinical alternative of root canal sealers. MTA Fillapex and AH Plus (Dentsply, DeTrey, Konstanz, Germany) were used as reference materials for comparison. The following hypotheses were tested: (1) There is no difference in the bond strength to root dentine among experimental sealers and commercially available sealers. (2) There is no difference in the bond strength to root dentine between both experimental sealers.

Material and Methods

Synthesis and Characterization of Butyl Ethylene Glycol Disalicylate

The transesterification reaction of methyl salicylate in two different alcohols in a molar ratio of 1:3 initiated the synthesis of 1,3-butyl ethylene glycol disalicylate. Isopropoxide titanium (Sigma-Aldrich, St. Louis, Missouri, USA) was used as a catalyst. The reaction was maintained at 200 °C for about 2 h. In order to remove the excess of methyl salicylate, the product was purified by vacuum distillation. Then, nuclear magnetic resonance spectroscopy (NMR) and Fourier transform infrared spectroscopy (FTIR) were used to characterize the butyl ethylene glycol disalicylate. The peak narrow of the hydroxyls in the spectral range from 3300 cm⁻¹ was observed (6).

Calcium Phosphate-Based Cements Formulation

Two experimental root canal sealers (MTAe, MTAe-HA) were prepared by mixing a base paste and a catalyst paste in a ratio of 1:1 according to Vitti et al. (6). The base paste

contained the synthesized component 1,3 butyl ethylene glycol disalicylate and bismuth oxide. The catalyst paste was composed of MTA, Resimpol 8, and titanium dioxide, with or without the addition of hydroxyapatite. MTA Fillapex and AH Plus were prepared following the manufacturer's instructions. The composition, manufacturers, and batch numbers of endodontic sealers are described in Table 1.

Specimen Size Calculation

Based on a previous study (12), an effect size of 0.74 was added to a power $\beta=95\%$, and a $\alpha=5\%$ inputs into an F test family for one-way analysis (G*power 3.1 for Macintosh). A total size of 16 slices specimens was required for this study.

Tooth Selection and Preparation

This study was approved by the Local Ethics Committee. Twenty freshly extracted human permanent maxillary central incisors with one circular canal, straight roots, and mature root apices were selected. Teeth with cracks, fractures, caries, and roots with small volume or calcifications were excluded from this study. As all materials were used in artificial canals created in root slices, the inclusion and exclusion criteria were evaluated by visual analysis during teeth selection and preparation. Specimens were cleaned by ultrasonic curettes and soaking in sodium hypochlorite solution (NaOCI) for 10 minutes. From the cementoenamel junction, one dentine slice (1 \pm 0.1 mm thick) was created using a low-speed saw with a diamond disc (Ø 125 mm x 0.35 mm x 12.7 mm; Buehler, Ltd. Lake Bluff, New York, USA) under continuous water irrigation. The final thickness of each slice was measured with a digital caliper with an accuracy of 0.001 mm (Avenger Products, North Plains, Oregon, USA). According to this procedure, twenty dentine slices were produced following this protocol (Fig. 1).

Preparation of Holes to Simulate Root Canals for Push-Out Assay

A 0.9 mm spherical diamond bur (Kommet, Santo André, São Paulo, Brazil) was used to drill four equidistant holes that simulated root canals in the coronal surface of each dentine slice. Each hole was drilled under constant water irrigation in a direction parallel to the root canal wall, maintaining a constant minimum distance of 1 mm between the adjacent holes, the external cementum, and the root canal lumen. These regular distances were standardized by the previous measure with periodontal probe associated with marking using a hydrographic pen. A vertical support (Dremel Workstation 220, Mount Prospect, IL, USA) ensured that drilling with diamond bur occurred perpendicularly to the axial line of coronal surface of specimens (9,12).

Subsequently, all dentine slices were immersed in a freshly prepared 2.5% NaOCl for 15 min and then immersed in distilled water to remove the traces of NaOCl solution. The smear layer was removed using 17% EDTA for 3 min. The final irrigation consisted of distilled water for 1 min, 2.5% NaOCl for 1 min, and distilled water for 1 min.

After irrigation, the holes were dried with absorbent paper, and the slices were fixed on a glass plate. Each hole was randomly filled with one of the selected endodontic sealers: AH Plus, MTA Fillapex, MTAe, and MTAe-HA (Fig. 1). The use of a hydrographic pen for marking the holes

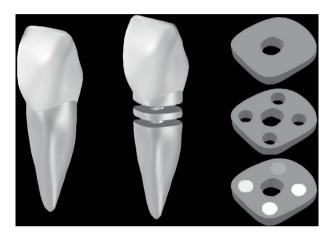


Figure 1. Selection, preparation, and filling of dentine slices.

indicated the location of each sealer. The experimental root canal sealers were handled in a ratio of 1:1 (MTA:salicylate resin). Materials were gently delivered into the holes; bubble formation was avoided by manual vibration of the glass plate, in which specimens were fixed, while placing each sealer in each slice. Then, filled dentine slices were incubated in contact with gauze moistened in a phosphate-buffered saline (PBS) solution (pH 7.2) at 37 °C for 7 days. Gauze moistened with PBS solution was replaced every 2 days to replenish the buffering capacity. This experimental setup allowed the four materials to be distributed in the same dentine slice.

Push-Out Assessment

An universal testing machine (Instron, Canton, MA, USA) was used to measure the bond strengths of endodontic sealers to root dentine specimen. Loading was performed with a plunger tip of 0.7 mm diameter that was positioned over only one of the tested sealers for each analysis. The load was applied in a coronal-apical direction with a speed of 0.5 mm min⁻¹, until filling-material dislocation occurred (Fig. 2). During the push-out test, a real-time software program (specific for the universal testing machine) was used to plot a load (N) x displacement (mm). The median value of push-out bond strength was calculated to obtain the MPa data according to the following formula (9,12):

Table 1. Composition, manufactures and batch numbers of root canal sealers used in this study

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Materials	Composition	Manufactures and batch numbers
AH Plus	Epoxy paste, diepoxy, calcium tungstate, zirconium oxide, aerosol, dye, amine paste, 1-adamante amine, iron oxide, N.N'dibenzyl-5-oxanonandiamine-1,9, TCD-diamine, calcium tungstate, silicon oil	Dentsply, Konstanz, Germany; 1410000796
MTA Fillapex	Salycylate resin, natural resin, diluting resin, bismuth oxide, nanoparticulated silica, MTA, pigments (MSDS data)	Angelus, Londrina, PR, Brazil;34373
MTAe	Base paste Bismuth oxide (60%), butyl ethylene glycol disalicylate (40%)	Vetec, Duque de Caxias, RJ Brazil; 010127-TB (Prepared at Federal University of Pelotas, Brazil)
	Catalyst paste MTA (60%) Pesimpol 8 (39%) Titanium dioxide (1%)	Angelus, Londrina, PR, Brazil; 090605 Bandeirante Brazmo, São Paulo, SP, Brazil; 81319 Vetec, Duque de Caxias, RJ, Brazil; 06092005
МТАе-НА	Base paste bismuth oxide (60%), butyl ethylene glycol disalicylate (40%)	Vetec, Duque de Caxias, RJ Brazil; 010127-TB (Prepared at Federal University of Pelotas, Brazil)
	Catalyst paste MTA (40%) Resimpol 8 (39%) Hydroxyapatite (20%) Titanium dioxide (1%)	Angelus, Londrina, PR, Brazil; 090605 Bandeirante Brazmo, São Paulo, SP, Brazil; 81319 Sigma-Aldrich, St. Louis, MO, USA, MKBC4763V Vetec, Duque de Caxias, RJ, Brazil; 06092005

Push-out bond strength (MPa) = Maximum load (N) / Adhesion area of root canal sealers (mm²)

The adhesion area of endodontic sealers was defined by the cylinder area method, whereas π = constant 3.14; r = hole radius filled with root sealers (0.45 mm); and h = thickness of dentine slice (1.0 mm) (9,12):

Adhesion Area of Root Canal Sealers (mm²) = $2\pi r \times h$

Afterwards, specimens were examined under a stereomicroscope (Optz; Opticam Microscopy Technology, Doral, Florida, USA) at 40× magnification to determine the mode of the bond failure, which was classified into three categories: (1) Adhesive failure that occurred at the material-dentine interface. (2) Cohesive failure within the filling materials. (3) Mixed failure mode.

Data Presentation and Analysis

Preliminary analysis of the raw pooled data was unable to reveal a Gaussian distribution (D'Agostino & Person omnibus normality test); therefore, a Kruskal-Wallis test was applied to assess the effect of each endodontic sealer on the dentine bond strength. Mann-Whitney with Bonferroni correction was used to isolate the differences. The alphatype error was set at 0.05. SPSS 11.0 (SPSS Inc., Chicago, IL, USA) was used as an analytical tool.

Results

All specimens had measurable push-out values and no premature failure occurred. Significant differences among medians values obtained by materials were observed (p<0.001). AH Plus displayed the highest value of bond strength to root dentine (p<0.001). In contrast, MTA Fillapex presented the lowest value of bond strength among all tested root canal sealers (p<0.001). Experimental root canal sealers showed intermediary bond strength values with no statistical differences between them (p>0.05). Figure 3 shows the variance of the bond strength data in each

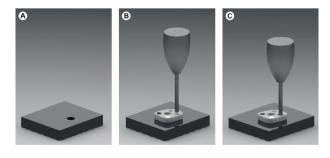


Figure 2. Push-out assessment. Device's relief for material displacement (A). Direction of the plunger tip over one root-canal sealer prior to the load application (B). Material displacement and load application in a coronal–apical direction (C).

endodontic sealer.

All specimens presented the mode of the bond failure classified in cohesive failure within the filling materials.

Discussion

The present results pointed out significantly different performances among the tested materials. AH Plus, an epoxy resin sealer, produced higher bond strengths to root dentine than both experimental calcium-silicate-based sealers and MTA Fillapex. Therefore, the first hypothesis was rejected. AH Plus outperformance has been well documented in endodontic literature and is classically considered a gold standard root canal sealer (10,13). Adhesion of AH Plus sealer results in great part from the formation of a covalent bond by an open epoxide ring to exposed amino groups in the collagen network (14). The strong sealing ability and mechanical interlocking of AH Plus with root dentine also results from its long setting time associated with creep capacity (15). Moreover, it could be argued that AH Plus presents a considerable cohesion between its molecules that can be translated to a great adhesion characteristic (13-15).

The two experimental sealers showed similar results; thus, we fail to reject the second null hypothesis. The similarity in the composition and properties of MTAe and MTAe-HA may explain these values. Both experimental sealers present two relevant chemical reactions: the progressive hydration of the orthosilicate ions and the reaction between MTA and butyl ethylene glycol disalicylate (6). The physical-mechanical characteristics and material set are dependent of these reactions.

Hydroxyapatite has been added in the composition of root canal sealers to improve the biological and physicochemical properties of these materials, such as the setting time and bioactivity (2,6). In the present study, the addition of this component in experimental sealers did not

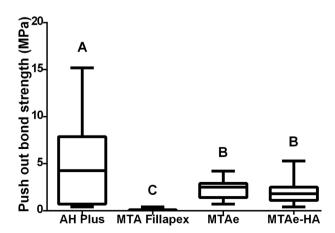


Figure 3. Box-plot with the median, the range and the minimum and maximum push-out values of the tested materials.

influenced dentine bond strength results. The percentage of hydroxyapatite (weight 20%) included in catalyst paste of MTAe-HA may have been insufficient to interfere on its push-out values. However, some issues regarding the addition of second sources of calcium phosphate besides MTA, such as hydroxyapatite, should be explained. When a second source of calcium phosphate is included in the composition of experimental sealers, MTA has to be removed in equal proportions. MTA and butyl ethylene glycol disalicylate-based materials need to be mixed in a ratio of 1:1 (MTA:salicylate resin) to have a complete setting reaction. As regards the variance in the material's amount in this ratio, MTA's percentage may be higher than salicylate resin's without affecting setting reaction and physical-mechanical characteristics (6). Nevertheless, if salicylate resin is added in higher proportions than MTA, the material setting reaction cannot be fully achieved. Therefore, as MTAe-HA presents a MTA:salicylate resin minimum ratio of 1:1, the addition of 20% hydroxyapatite was the maximum practicable; because the removal of MTA to increase weight of this component would lead to higher proportions of salicylate resin than MTA, and thus interfere in the material's performance.

Experimental sealers MTAe and MTAe-HA demonstrated intermediary results, presenting superior dentine bond strength outcomes when compared to a commercial MTA-based sealer, MTA Fillapex. The performance of both experimental MTA-based sealers could possibly be supported by MTA bioactivity, that is, the capacity to spontaneously produce an apatite layer when in contact with phosphatecontaining physiological fluids (16). Moreover, MTA is also known to interact with dentine to cause intratubular Ca and Si incorporation (17) and cause dentine remineralization (18), intrafibrilar apatite deposition (19), and the formation of tag-like structures (10,20) in the presence of PBS. The ability of nucleate calcium-phosphate by calcium silicatebased materials in contact with phosphate-containing fluids is strictly correlated to the chemical composition and calcium-releasing properties (4). The nucleation of apatite at the interface produces a micromechanical bonding system to dentine that may improve the displacement resistance (21). Experimental MTA and butyl ethylene glycol disalicylate-based sealers present a higher proportion of MTA (weight 40-60%), which may be associated with an increase in levels of biomineralization that allow for a major quantity of tag-like structures and a more-effective micromechanical bonding system when compared to MTA Fillapex. This is consistent with Vitti et al. (6) who observed that experimental sealers significantly released more calcium than MTA Fillapex.

MTA Fillapex showed the lowest value of dentine bond strength when compared to the other sealers (p<0.05).

These findings are in accordance with previous reports that revealed inferior results for MTA Fillapex regarding push-out bond strength outcomes (7,10). The chemical composition is one important factor that affects adhesion characteristics of an endodontic sealer. MTA Fillapex has a higher resin/MTA proportion compared to that of experimental sealers (6). It has been observed that to MTA Fillapex complete setting reaction, a ratio of 1:1 is necessary (MTA:salicylate resin) (6). Thus, this unbalanced resin/MTA ratio may explain the lower bond strength and the properties of extended setting time and working time, excessive flow ability, and solubility as disturbance in calcium-silicate properties, which has been reported in previous studies (5,6,22).

Root canal sealers containing salicylate present an initial volumetric shrinkage during setting that increases the contraction factor (23). Although manufacturers claim that MTA Fillapex presents setting expansion due to the presence of MTA, this endodontic sealer may have a higher percentage of resinous components (salicylate, diluting and natural resin) predominating over the expansion coefficient. As MTA Fillapex has an extended setting time (6), the contraction factor might increase gradually and raise the formation of gaps and channels among the sealer-dentine interface. Moreover, the excessive flow ability and solubility of MTA Fillapex may also increase dimensional changes and interfere in the sealer penetration into dentinal tubules, anatomical irregularities, or accessory canals, producing a material detachment from dentinal walls. This is consistent with previous findings that MTA Fillapex presents a considerable quantity of gaps between the sealer-dentine interface (22). In addition, this sealer has a wide range of particle sizes and an external surface with porosities (24), which represents low adhesion characteristics (1).

Push-out tests have become widely used to evaluate the quality of filling materials and to provide better understanding of the obturation process since occurrence of bond failures is an important concern in endodontic treatment (13,14). Conventional push-out tests such as methodology used in De-Deus et al. (13) and Fisher et al. (14) include the chemomechanical preparation and obturation of extracted human teeth, followed by analysis in different root regions of these several specimens. This method present a major drawback of creating a reliable baseline since the variable morphology of the dentinal substrate and the intricate anatomy makes standardization challenging. In this context, the present study used a standard holes method, recently suggested by Silva et al. (9) and Scelza et al. (12), that has aspects that deserve to be addressed. To increase the internal validity of the push-out model, four artificial standard holes were created in dentine slices, providing the same dentine source to all root canal sealers. In this way, confounding factors associated with dentine

heterogeneity – such as tooth age, mineralization, and hardness – present in different teeth and in different regions of the same root were eliminated (12). Also, a cylindrical standardized final shape with a 0.9 mm diameter for all holes allowed the standardization of the internal root canal anatomy among the experimental groups, which is well known as a critical confounding factor and biological bias.

Nevertheless, this study design present drawbacks, as in all *in vitro* methodologies, that should be indicated. The standardization of holes with a bur may dilute variables that are present in root canal anatomy in clinical situations. Additionally, to only provide a better control on the type of failure mode, the root canal space was filled only with the sealer. The advantage of this model is that the compressive load is applied on the sealer and not on the resilient material, such as gutta-percha, as the latter procedure would lead to erroneous interpretations. This also truly reflects the bond strength between the sealer and dentine (9,12). However, the use of both root canal sealer and gutta-percha would present the benefit of reflecting more closely the clinical procedures in this respect.

At the present study, bond strength of root canal sealers have been evaluated in cervical third because this region presents a larger area that allowed the preparation of the four holes with 0.9 mm wide, respecting a constant distance of 1 mm between the adjacent holes, the external cementum, and the root canal lumen. The endodontic literature presents different results concerning push-out bond strength values according to root canal thirds. Studies have reported higher values of bond strengths in apical third compared to cervical third, as higher values in cervical area and similar results between root canal regions (25). In the present push-out design, dentine bond strength of sealers could not be evaluated in middle and apical regions. However, the analysis of root canal thirds was not an objective of this study.

In conclusion, experimental MTA and butyl ethylene glycol disalicylate sealers presented suitable bond strength outcomes when compared to MTA Fillapex. Therefore, the present finding adds to experimental sealers based on MTA and butyl ethylene glycol disalicylate satisfactory bond strength performance for clinical application and increases the overall knowledge about these materials that have potential to become a clinical alternative of root canal sealers.

Resumo

Esse estudo investigou a resistência de união de dois cimentos endodônticos experimentais à base de MTA e butiletilenoglicol dissalicilato: MTAe e MTAe. Os materiais de referência utilizados para comparação foram os cimentos endodônticos MTA Fillapex e AH Plus. Vinte incisivos superiores humanos foram selecionados e um slice dentinário de 1 mm de espessura foi obtido do terço cervical de cada raiz. Na superfície

coronária de cada slice, quatro orifícios com 0,9 mm de diâmetro foram confeccionados através da dentina. Uma irrigação padronizada foi realizada e os orifícios foram preenchidos com um dos guatro cimentos endodônticos avaliados: AH Plus, MTA Fillapex, MTAe, e MTAe-HA. Os slices preenchidos foram armazenados em solução PBS (pH 7,2) durante 7 dias a 37°C. O ensaio de push-out foi realizado por meio de um dispositivo com 0,7 mm de diâmetro. A carga foi aplicada com a velocidade de 0,5 mm/min até a obtenção de deslocamento do material obturador. Os resultados foram expressos em MPa. O teste de Kruskal-Wallis foi aplicado para avaliar o efeito da resistência de união de cada cimento endodôntico. O teste de Mann-Whitney com correção de Bonferroni foi utilizado para isolamento das diferenças. O erro do tipo-alfa foi fixado em 0,05. Diferenças significantes entre os valores de medianas obtidos pelos materiais foram observados (p<0,001). O AH Plus demonstrou os maiores valores de resistência de união (p<0,001). Em contraste, o MTA Fillapex apresentou a menor resistência de união entre todos os cimentos testados (p<0,001). Os cimentos experimentais demonstraram valores intermediários, com ausência de diferenças estatísticas entre si (p>0,05). Em conclusão, os cimentos endodônticos experimentais à base de MTA e butiletilenoglicol dissalicilato apresentaram resultados adequados de resistência de união quando comparados ao MTA Fillapex.

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