## ORIGINAL RESEARCH Dental Materials

# Evaluation of an antibacterial orthodontic adhesive incorporated with niobium-based bioglass: an *in situ* study

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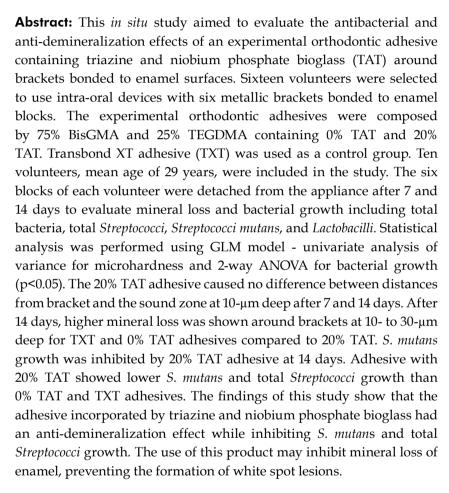
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#### Introduction

Prolonged retention of dental plaque, especially the microorganism *Streptococcus mutans*, around brackets during orthodontic treatment with fixed appliances leads to a decrease of pH and thus the development of white spot lesions (WSLs) in the enamel surface. Brackets and archwires usually create numerous retention sites hampering tooth cleaning. Current



clinical investigations<sup>2,3</sup> have reported an increase of WSLs prevalence from 46 to 59% for patients whose hygiene worsened after 12 months of orthodontic treatment. In addition, the majority of patients undergoing orthodontic treatment are teenagers who often have suboptimal manual ability and overall motivation.<sup>4</sup> These findings highlight the necessity to use supplementary preventive methods to avoid demineralization of the enamel surface.

In line with previous efforts to find novel anticaries and remineralization agents with additional or synergistic effects, some agents, such as triclosan, chlorhexidine, and silver, have been added to orthodontic adhesives resulting in antimicrobial activity.5,6,7 Although some authors have indicated a decrease in bond strength after addition of antibacterial agents, a meta-regression analysis demonstrated that this procedure has no influence in bond strength to enamel.8 Recent in vitro studies have shown inhibition of bacterial growth with methacrylatebased monomers, such as 1,3,5-triazine. 9,10 This antimicrobial agent is a small compound that mimics the hydrophobic pattern of short cationic peptides. It can decrease bacterial growth by disrupting the membrane integrity and is more selective against gram-positive bacteria.11

Notwithstanding, the use of bioactive fillers have been the reason of current studies in order to recover mineral content of dental tissues. 5,11,12 One of this materials is phosphate invert glass (PIG), which stimulates a specific biological response, resulting in a bond between living tissue and synthetic material.<sup>13</sup> Furthermore, niobium pentoxide has shown to promote mineral deposition when in contact to artificial saliva. 10,14 Its addition to PIG could enhance chemical stability15 leading to a long-term effect of bioglasses. Recent in vitro studies10,16 evaluated the performance of an experimental orthodontic adhesive incorporated with PIG and niobium pentoxide, which showed improved mechanical and chemical properties. Considering the limitations of in vitro studies in simulating daily changes of sugar exposure, pH, saliva, temperature, humidity, and bacteria colonization of the oral environment, in situ models represent an adequate approach. In situ studies are a relatively fast and clinically relevant method<sup>17</sup> to

study the behavior of antibacterial adhesives against demineralization caused by dental plaque.

Therefore, this study aimed to evaluate *in situ* the antibacterial and anti-demineralization effects of an orthodontic adhesive incorporated with triazine and niobium pentoxide phosphate invert glass (TAT). The null hypothesis was that the adhesive containing 20% wt triazine and 5% wt niobium phosphate bioglass (20% TAT) would present no difference in mineral loss and bacterial growth compared to other adhesives and its sound zone.

### Methodology

The study was approved by an Ethical Committee Board (CAAE 49445515.7.0000.5347) and followed the guidelines of the Declaration of Helsinki.

#### Preparation of the experimental adhesives

The experimental orthodontic adhesives were prepared with 75%/25% BisGMA and TEGDMA methacrylates, and a photo-initiator (CQ: Camphorquinone, 1 mol%) and two co-initiators (EDAB: ethyl 4-dimethylaminobenzoate; DPIHFP: diphenyliodonium hexafluorophosphate, 1 mol% each) (Aldrich Chemical Co., Milwaukee, USA) were used. Also, 5% wt of fumed silica (AEROSIL 200, without silane, Piscataway, USA) were added to adjust the viscosity, as previously reported.9 The compound 1,3,5-tryacryloylhexahydro-1,3,5-triazine (TAT; Sigma-Aldrich, St. Louis, USA) was added at 20% wt as described in a recent study.14 Phosphate invert glass containing 10 mol% of niobium pentoxide (PIG-Nb) with a mean size of 74 µm was prepared as previously reported16 and added at 5% wt.

#### Study design

The study presented a double-blinded (volunteers and outcome assessor) and controlled *in situ* design. The factor evaluated was orthodontic adhesive resin: Group TXT, Transbond XT primer+Transbond XT adhesive (3M Unitek Corp, Monrovia, USA); Group 0% TAT, experimental orthodontic adhesive; and Group 20% TAT, experimental orthodontic adhesive with TAT + PIG-Nb.

#### Sample size

The sample size of 13 volunteers was calculated for a 5% significance level, 80% power, 7.4% of enamel microhardness loss as estimated standard deviation, and 7.7% as minimum detectable difference in means of enamel microhardness loss based on the demineralization data of a previous study. Three extra individuals were added expecting a dropout rate of 20%.

#### Sample preparation

Enamel blocks (n=140,  $5 \times 5 \times 2$  mm) were prepared from sound bovine teeth (CF). The teeth were stored for 1 month in distilled water then cut with a diamond saw (IsoMet, Buehler Ltd., Lake Bluff, USA) and their surfaces were ground flat with #600-, #1200-, and #2000-grit silicon-carbide papers. One hundred and eight blocks were selected after microhardness measurement by the closest values to the total average value (257  $\pm$  0.9). The mean hardness of the blocks of each appliance was similar to the total average value.

The bonding of metallic orthodontic brackets (Morelli Ltd., Sorocaba, Brazil) was performed by etching the enamel for 30 s with 37% phosphoric acid (CaiTECH Ind. Ltd, Rio do Sul, Brazil), rinsing with water, and drying with oil-free compressed air until the etched enamel showed a frosty appearance. A thin layer of Transbond adhesive primer (3M Unitek, Monrovia, USA) was applied with a micro-brush and photo-activated for 20 s before adhesive resin application. The adhesive resin of each group (TXT, 0% TAT and 20% TAT) was applied with a syringe and brackets were pressed with a 300 g needle.9 The adhesive excess was removed and the resin was photo-activated for 10 s on each side of the bracket by light-emitting diode RadiiCal (1200mW/cm<sup>2</sup>; SDI Ltd., Bayswater, Australia).

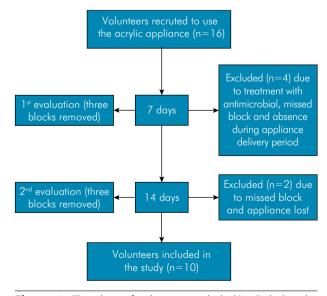
Intraoral palatal appliances were made for the upper arch with acrylic resin on plaster models. Each appliance had six wells ( $6 \times 6 \times 3$  mm), three on each side, with one well for each enamel block. The position of enamel blocks in the wells was randomly determined by a software program (Research Randomizer Form, Social Psychology Network, Middletown, USA) for each volunteer. The enamel blocks were fixed with cyanoacrylate 1 mm below

the level of the appliance surface in order to induce dental plaque accumulation (FD and CF).

#### Volunteers and In situ experiment

Sixteen volunteers of the 31 students/professors from the Faculty of Dentistry fulfilled the inclusion criteria (18+ years old; adequate oral health with no caries, erosive lesions and gingivitis/periodontitis) and were selected after verification of the exclusion criteria - medication that affects salivary glands, systemic disease influencing oral function, smoking, pregnancy, use of antimicrobials within 90 days before the start of the study, and orthodontic treatment (Figure 1). The volunteers received verbal and written instructions about the protocol. They also received a 30-mL bottle containing 20% sucrose solution, the orthodontic appliance and container, a fluoride toothpaste (1350 ppm), and a soft toothbrush.

Volunteers were instructed to wear the orthodontic appliance for two weeks, 24 h a day, except during meals, avoid drinking anything that could be an additional source of fluoride, and brush the sample holders. The volunteers applied a drop of sucrose solution 8 times per day, every 2 h, and after 5 minutes,<sup>20</sup> and clean the device outside the mouth, avoiding the wells, once a day with the fluoride toothpaste. After 7 days, the three blocks of the left



**Figure 1.** Flowchart of volunteers included/excluded in the *in situ* study.

side of the appliances were removed to perform mineral loss measurements and bacterial growth assays and the sample holders were filled with wax. After 14 days, the same evaluations were performed in the blocks of the right side.

#### Mineral loss measurement

Sixty enamel blocks with bonded brackets were sectioned in the buccal-palatal direction with a diamond disk in the cutting machine. The half-blocks were embedded in acrylic resin and polished with #2000-grit silicon carbide paper and felt disc with aluminum oxide solution. Following a previous study,  $^{18}$  42 indentations were made in each half-block with a microhardness tester HMV-2 (Shimadzu Corp., Kyoto, Japan) under a load of 25 g for 5 s. Six indentations (at 10, 20, 30, 50, 70, and 90  $\mu m$  from the bracket) at 7 mesial-distal positions (at the center relative to the bracket and at 0  $\mu m$  (edge of the bracket), 100, and 200  $\mu m$  from the bracket), were made on the occlusal surface. The Knoop hardness values from two half-crowns and from each side were averaged.

#### **Bacterial composition**

The composition of the biofilm accumulated during 7 and 14 days of experiment was analyzed by the bacterial adherence assay. Six enamel blocks covered by oral biofilm of each of the 10 adhesive groups (total of 60) were removed from the appliances and transferred to a microtube containing 900  $\mu$ L of sterile saline solution (0.9% NaCl). After, biofilms were harvested and the bacterial suspensions were serially diluted (100  $\mu$ L) in saline solution. Two aliquots of 25  $\mu$ L were plated onto the mediums (n = 3) agar

sanguis, agar mitis salivarius, agar mitis salivarius + 0.2 U/mL bacitracin, and agar rogosa SL to determine the number of total bacteria, total *Streptococci*, *S. mutans*, and *Lactobacilli*, respectively. All plates were incubated under microaerophilic conditions at 37°C for 48 h, followed by counting the colony-forming units (CFUs).<sup>21</sup> The number of CFUs was visually counted by two blinded researchers (F.D. and C.F.) using an optical microscope. The mean value was scored and transformed to log CFU per milliliter.

#### Statistical analysis

Microhardness data of the four factors (time, distance, depth, and adhesive) and their interactions were evaluated by univariate analysis of variance (ANOVA) followed by Tukey's test. Bacterial composition (log<sub>10</sub>CFU/mL) was evaluated by two-way ANOVA with a 0.05 level of significance. Analyzes were performed on SigmaPlot 13.0 Software (Systat Software Inc., San Jose, USA).

#### Results

The ten volunteers (6 females, 4 males, aged 21 to 36 years) attended the university clinic at 7 and 14 days. Four volunteers dropped out of the study in the first week due to absence (n = 2), block lost (n = 1), or antimicrobial use (n = 1). Two volunteers dropped out during the second week due to lost sample or lost appliance (Figure 1).

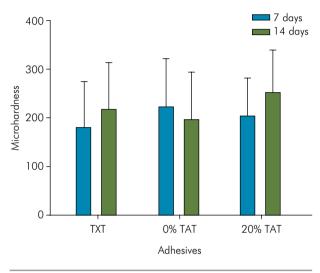
Significant effects were found for the four factors: time, distance, depth, and adhesive (p < 0.05), and for the interactions time\*adhesive and distance\*adhesive (p < 0.05; Table 1; Figure 2 and 3).

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Source	Sum of squares	Mean square	df	F	P1
Time	144.520.469	144.520.469	1	29.455	0.0001
Distance	86.121.528	28.707.176	3	5.851	0.001
Depth	2.515.204.616	503.040.923	5	102.527	0.0001
Adhesive	229.273.211	114.636.605	2	23.365	0.0001
Time*Adhesive	429.215.288	214.607.644	2	43.740	0.0001
Distance*Adhesive	62.594.327	10.432.388	6	2.126	0.048

Statistically significant (p < 0.05).

Mineral loss of the 0% TAT group, after 7 days of experiment, at distances of 200  $\mu m$  and "Sound zone" was significantly lower (p < 0.05) than TXT and 20% TAT at 50, 70 and 90  $\mu m$ , and 70  $\mu m$  depth, respectively. However, after 14 days of experiment, mineral loss of the 20% TAT group was significantly



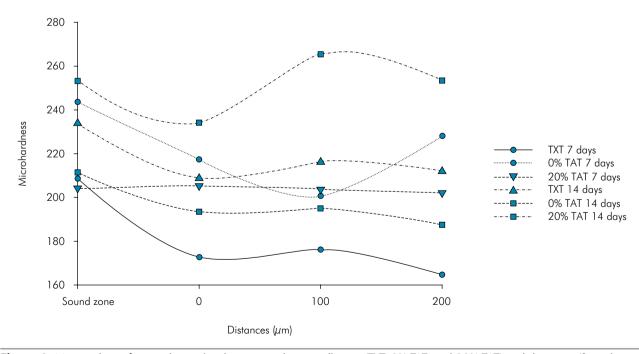
**Figure 2.** Mean and SD values of enamel microhardness according to time (7 and 14 days) and adhesive (TXT, 0% TAT, and 20% TAT).

lower (p < 0.05) than TXT (at distance of 100  $\mu$ m and 10  $\mu$ m depth) and 0% TAT (at distances of 0  $\mu$ m and 100  $\mu$ m, with 50  $\mu$ m and 30  $\mu$ m depth, respectively), as shown in Table 2. Representative images (Figure 4a to 4d) show the mineral increase of TXT and 20% TAT at 7 days compared to 14 days of the experiment.

The experimental orthodontic adhesive containing 20% TAT and 5% PIG-Nb was effective in preventing demineralization around metallic brackets bonded to enamel surface (p < 0.05) after 7 and 14 days (Figure 5a and 5b; Table 2) compared to TXT and 0% TAT groups.

Regarding mineral loss within groups among various distances, significant differences (p < 0.05) were found at 10  $\mu$ m depth. No difference (p > 0.05) was found after 7 and 14 days in the 20% TAT group. Increased mineral loss was found after 7 days in the TXT group in "Sound zone" compared to 100 and 200  $\mu$ m and in the 0% TAT group in "Sound zone" compared to 100  $\mu$ m (Figure 5a). After 14 days, increased mineral loss was found in the TXT group in "Sound zone" compared to 0 and 100  $\mu$ m (Figure 5b).

Inhibition of bacterial growth (p < 0.05) between 7 and 14 days was found only in the 20% TAT group

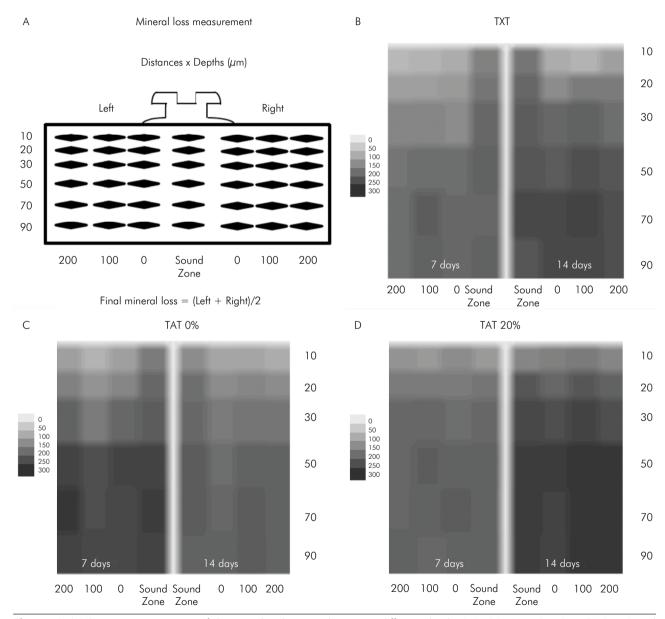


**Figure 3.** Mean values of enamel microhardness according to adhesive (TXT, 0% TAT, and 20% TAT) and distances (Sound zone, 0, 100, and 200  $\mu$ m).

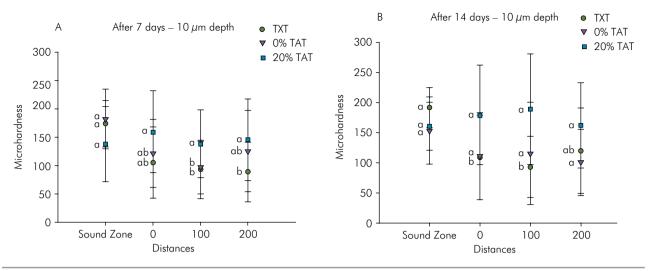
**Table 2.** Mean and SD of microhardness (depth and distance, in  $\mu$ m) of different groups after 7 and 14 days of bacterial accumulation.

\/ ·	Total b	acteria	Total Stre	eptococci	S. mi	utans	Lactobacillus		
Variable	7 days	14 days	7 days	14 days	7 days	14 days	7 days	14 days	
TXT	6.33(0.86) <sup>A,a</sup>	8.33(0.24) A,b	6.68(0.60) B,a	8.44(0.21) AB,b	2.17(0.56) A,a	3.07(0.69) B,b	2.37(1.31) A,a	3.89(1.99) A,a	
0% TAT	6.09(0.81) A,a	8.07(0.12) A,b	6.46(0.46) B,a	8.52(0.19) B,b	2.15(0.53) A,a	3.07(0.52) B,b	2.51(1.11) A,a	3.59(2.27) A,a	
20% TAT	6.06(0.57) A,a	8.35(0.29) A,b	5.97(0.50) A,a	8.01 (0.41) A,b	1.86(0.36) <sup>A,a</sup>	2.03(0.60) A,a	2.79(1.66) A,a	4.07(2.26) A,a	

Different capital letters mean statistical significance within columns for each distance (p < 0.05).



**Figure 4.** (A) Representative image of the microhardness evaluation at different depths (10, 20, 30, 50, 70 and 90  $\mu$ m) and different distances (Sound zone, 0, 100, and 200  $\mu$ m). The equation used for mineral loss measurement is shown. (B) Mineral content increased after 14 days; however, at 10 and 20  $\mu$ m deep, mineral loss may be observed comparing the different distances to the "sound zone". (C) Mineral loss may be observed between the different distances (in  $\mu$ m) and the "sound zone"; the mineral loss increased at 7 days compared to 14 days. (D) Mineral content increased at 7 days compared to 14 days and no alterations were observed between "sound zone" and the different distances (in  $\mu$ m).



**Figure 5.** (A) Comparison of microhardness at 10- $\mu$ m depth after 7 and 14 days among different distances within each group. No alteration was observed for 20% TAT group while a decrease was observed for TXT and 0% TAT groups at 100 and 200  $\mu$ m distances. (B) No alteration was observed for 20% TAT group while a decrease was observed for TXT and 0% TAT group at 0, 100, and 200  $\mu$ m.

**Table 3.** Mean and SD of bacteria growth (Log<sub>10</sub> CFU/mL) of different groups after 7 and 14 days.

Variable	10 μm		$20~\mu \mathrm{m}$		30 $\mu$ m		50 $\mu$ m		70 $\mu$ m		90 $\mu$ m	
	7 days	14 days	7 days	14 days	7 days	14 days	7 days	14 days	7 days	14 days	7 days	14 days
Sound zone												
TXT	174.5 ± 40.6 <sup>A</sup>	191.6 ± 32.7A	192 ± 63.1 <sup>A</sup>	217.7 ± 74.4A	215.9 ± 68.7 <sup>A</sup>	232.2 ± 71.4A	226.3 ± 69.1 <sup>A</sup>	246.3 ± 73.4A	218 ± 58 <sup>8</sup>	269 ± 80.1A	224.3 ± 71.1 <sup>A</sup>	245.3 ± 64.2 <sup>A</sup>
TAT 0%	182.7 ± 52.5 <sup>A</sup>	153.4 ± 56A	214.4 ± 49.2 <sup>A</sup>	200 ± 83.3A	230.9 ± 76.2 <sup>A</sup>	210.5 ± 74.7A	275.2 ± 38.1 <sup>A</sup>	239 ± 79.3A	283.3 ± 46.7 <sup>A</sup>	237.7 ± 75.7A	275.8 ± 50.9 <sup>A</sup>	228.2 ± 79.7 <sup>A</sup>
TAT 20%	138.1 ± 66.7 <sup>A</sup>	161.1 ± 39.5A	194 ± 47.8 <sup>A</sup>	240.4 ± 32.7A	211.6 ± 50.1 <sup>A</sup>	266.6 ± 39.5A	229.8 ± 27.4 <sup>A</sup>	282.7 ± 40.7A	222 ± 29.1 <sup>B</sup>	286.1 ± 39.6A	228.8 ± 17.6 <sup>A</sup>	282.5 ± 38.2 <sup>A</sup>
0 µm												
TXT	105.6 ± 62.9 <sup>A</sup>	108.9 ± 70.1A	138.5 ± 79.9 <sup>A</sup>	155.3 ± 71A	158.5 ± 77.1 <sup>A</sup>	216.4 ± 79.1A	207.9 ± 92 <sup>A</sup>	239.8 ± 86.1AB	210.2 ± 90.6 <sup>A</sup>	269.2 ± 77.8A	215 ± 89.3 <sup>A</sup>	262.9 ± 76.5 <sup>A</sup>
TAT 0%	121.8 ± 60.1 <sup>A</sup>	111.4 ± 71.6A	163.6 ± 87.4 <sup>A</sup>	154.3 ± 104.1A	219.1 ± 104 <sup>A</sup>	189.3 ± 91.2A	270.6 ± 77.9 <sup>A</sup>	208.6 ± 81.6B	261.9 ± 76.4 <sup>A</sup>	218.1 ± 88A	267.2 ± 66 <sup>A</sup>	223.8 ± 76.8 <sup>A</sup>
TAT 20%	159.7 ± 72.4 <sup>A</sup>	178.9 ± 82.4A	184.8 ± 63.3 <sup>A</sup>	219.7 ± 70.8A	208.5 ± 51.3 <sup>A</sup>	259.7 ± 59.1A	223.6 ± 62.6 <sup>A</sup>	288.2 ± 69.3A	235.3 ± 61.9 <sup>A</sup>	278.4 ± 59.2A	220 ± 70.8 <sup>A</sup>	277.2 ± 78.7 <sup>A</sup>
100 μm												
TXT	93.7 ± 51.8 <sup>A</sup>	93.1 ± 51.3B	129 ± 82.5 <sup>A</sup>	183.4 ± 89.1A	167.9 ± 95.3 <sup>A</sup>	227.9 ± 74.3AB	207.6 ± 94.5 <sup>A</sup>	254.1 ± 82.3A	230.7 ± 89.1 <sup>A</sup>	275.1 ± 82.2A	227.3 ± 87.7 <sup>A</sup>	263.5 ± 65.5 <sup>A</sup>
TAT 0%	97 ± 46.6 <sup>A</sup>	115.6 ± 85.3B	143.2 ± 52.3 <sup>A</sup>	163 ± 99.6A	183.9 ± 76.8 <sup>A</sup>	195.6 ± 90B	253.8 ± 85.6 <sup>A</sup>	226.5 ± 71.6A	259.7 ± 66.9 <sup>A</sup>	235.3 ± 72.2A	266.3 ± 77.4 <sup>A</sup>	233.6 ± 72.5 <sup>A</sup>
TAT 20%	138.9 ± 60 <sup>A</sup>	188.6 ± 91.6A	187.3 ± 59.2 <sup>A</sup>	240 ± 83.7A	219 ± 72.3 <sup>A</sup>	272 ± 58.8A	230 ± 68.2 <sup>A</sup>	297.9 ± 67.3A	227 ± 65.5 <sup>A</sup>	296.1 ± 71.4A	218.9 ± 49.6 <sup>A</sup>	297.4 ± 71.4 <sup>A</sup>
200 μm												
TXT	89.4 ± 52.6 <sup>A</sup>	120.2 ± 71.5A	125.8 ± 58.8 <sup>A</sup>	181.1 ± 89.2A	164.2 ± 65.5 <sup>A</sup>	208.3 ± 72.1A	199.9 ± 62.9 <sup>B</sup>	244.9 ± 62.9A	204.4 ± 70.4 <sup>B</sup>	257.5 ± 53.5A	204 ± 75.9 <sup>B</sup>	259.9 ± 67.5 <sup>A</sup>
TAT 0%	125.8 ± 71.9 <sup>A</sup>	100.6 ± 54.6A	175 ± 82.4 <sup>A</sup>	156.1 ± 67.4A	221.9 ± 74.8 <sup>A</sup>	191.2 ± 79.5A	277.2 ± 65 <sup>A</sup>	226.6 ± 80.6A	292.7 ± 65.6 <sup>A</sup>	223 ± 84.8A	275.8 ± 59.9 <sup>A</sup>	226.6 ± 73.6 <sup>A</sup>
TAT 20%	145.9 ± 71.8 <sup>A</sup>	162 ± 70.6A	189.5 ± 61.9 <sup>A</sup>	221.6 ± 54.2A	211.3 ± 65.8 <sup>A</sup>	253.8 ± 49A	216.8 ± 71.8 <sup>AB</sup>	293.8 ± 57.7A	219.5 ± 59.8 <sup>B</sup>	297.9 ± 71.8A	228.9 ± 56.3 <sup>AB</sup>	290.9 ± 67 <sup>A</sup>

Different capital letters mean statistical significance within columns (p < 0.05); Different lowercase letters mean statistical significance among columns of each bacteria (p < 0.05).

for *S. mutans*. An increase in total bacteria and total *Streptococci* was found for all groups while no difference occurred for *Lactobacilli* between 7 and 14 days. Comparing groups, total *Streptococci* growth in the 20% TAT group at 7 and 14 days was lower than TXT and 0% TAT, and 0% TAT, respectively. The *S. mutans* growth of 20% TAT at 14 days was lower than TXT and 0% TAT (Table 3).

#### **Discussion**

This in situ model simulated the complexity of biofilm formation in vivo and the variability of the oral environment, thus overcoming the ethical and clinical relevance limitations of in vivo<sup>22</sup> and in vitro experiments, 16,17 respectively. For the evaluation of novel antimicrobial adhesives, appropriate test systems are required, such as multispecies biofilm models, which mimic the in vivo situation. In situ models testing materials containing antimicrobial<sup>23</sup> or remineralizing<sup>24</sup> agents have shown some evidence for reduced mineral loss. Biofilm formation in enamel surfaces claims for highly efficient biomaterials in order to prevent tooth demineralization. This method was used due to a good correlation (0.91) found between enamel microhardness and the percentage of mineral within caries lesion.25 Also, to the best of the authors' knowledge, this was the first time that demineralization of the enamel adjacent to brackets bonded with an antibacterial and bioactive adhesive was assessed in situ. In this study, the null hypothesis was rejected since the experimental orthodontic adhesive containing TAT and PIG-Nb promoted inhibition of total Streptococci and S. mutans growth and avoided demineralization of the enamel surface.

Acidogenic bacteria present in the plaque, most notably *S. mutans* and *Lactobacilli*,<sup>26</sup> are responsible for lowering pH and causing WSLs around brackets within one month after bonding. Although previous *in situ* studies<sup>27,28</sup> have shown enamel alterations within 14 days, the greater demineralization after 7 days of sucrose exposure found in this study is in agreement with a previous report.<sup>29</sup> Mineral loss of enamel within 10 µm depth, as found in this study, was well correlated to lesion progression of 1 to 2 µm per day in clinical restorations.<sup>30</sup> Mineral

loss was significantly higher in both TXT and 0% TAT groups compared to 20% TAT group after 14 days at 0 and 100 µm distances of bracket base. Furthermore, in accordance to in situ studies with similar methodology evaluating microhardness over 28 days, 18,31 demineralization of 0% TAT and TXT groups within 10 µm depth increased at 100 and 200 µm distances after 7 days, and 0 and 100 µm distances after 7 and 14 days, respectively, compared to "Sound zone". The microhardness measurement of the "Sound zone" was essential to ensure that the results observed (Table 2) were due to mineral loss caused by the acids of the plaque and not by the etching procedure. This is highlighted in Figure 4b and 4c, wherein areas with higher mineral content until 30 µm were observed at the "Sound zone". No significant difference in bond strengths between TXT and TAT (20.44±6.23 and 16.33±5.06, respectively) found in a previous study<sup>10</sup> indicated a similar adhesion between both and enamel. A limitation in this study was that authors standardized the initial microhardness found in great depths of enamel, as standardization of teeth was made only at the surface of enamel. Despite the clinical relevance of evaluating re- or de-mineralization in great depths, which could indicate fragility inside the shallow surface of enamel, these alterations were probably caused by its intrinsic characteristics. Previous studies showed no demineralization of enamel over 50 µm deep in periods of 7 and 14 days.<sup>28,29</sup>

The mineral content of enamel in the 20% TAT group at 14 days, as shown in Figures 3 to 5, was a consequence of two main factors: antibacterial activity and mineral deposition. As previously reported,9 incorporation of 20% TAT into an experimental orthodontic adhesive has led to a reduction of *S*. mutans growth, also observed in this study (Table 3) within 14 days. TAT has shown to copolymerize its methacrylate radical with the adhesive's monomers preventing over-time leaching.14 The antimicrobial mechanism of TAT is through the mimicking of the hydrophobic pattern of short cationic peptides and is more selective against gram positive bacteria, leading to disruption of Lactobacilli and S. mutans membrane integrity.<sup>32</sup> Moreover, the surface roughness of restorative materials plays a role in pellicle formation

and biofilm adhesion.<sup>33</sup> The smaller inorganic fillers from the phosphate invert glass of 20% TAT adhesive may have resulted in lower surface roughness<sup>34</sup> and less bacterial accumulation. However, no inhibition and no difference against total bacteria and *Lactobacilli* growth was found among the tested adhesives. *Lactobacilli* growth increased 4 to 10 times more than *S. mutans* in biofilms formed under exposure to sucrose.<sup>35</sup> This may explain their great growth after 14 days, as well as the high total bacterial count, outperforming the antibacterial activity of the 20% TAT adhesive. Another limitation of this study was that plaque collection was not done in different areas to study bacteria specifically from each distance.

Nonetheless, the incorporation of niobium pentoxide phosphate invert glass into the adhesive has promoted mineral deposition in artificial saliva.<sup>14</sup> Figure 2d illustrates the higher mineral content at 14 compared to 7 days. This could be explained by the presence of bioactive glass promoting the leach of ions resembling those from enamel and their diffusion through the lesion. There is evidence that WSLs are remineralized by the use of bioactive glasses in shortterm evaluation.36 Indeed, the increase of mineral content shown in Figure 2b may have occurred due to the higher filler content, such as quartz, silica, and glass, than the 0% TAT. Also, the addition of niobium pentoxide was done to improve chemical stability of the bioglass and thus increase the duration of mineral deposition.<sup>37</sup> No previous study with orthodontic antibacterial adhesive has demonstrated the in situ antibacterial efficacy to use it as a positive control group. Previous antibacterial studies of Triazine and phosphate invert glass showed satisfactory results9 consistent to antibacterial long-term effects of quaternary ammonium adhesives<sup>38</sup> instead of chlorhexidine added to the adhesive, which loses protection after 2 h<sup>6</sup>. Regarding the limitations of the adhesives studied, such as their hydrolytic property39 and the microbial<sup>40</sup> degradation of the polymer matrix, the antibacterial and mineral deposition properties of the experimental 20% TAT adhesive may result in a tougher adhesive.

*In situ* models are known to be faster than clinical models and have higher clinical relevance than *in* 

vitro models. However, they have some disadvantages as patients are required to wear and care for the appliances.<sup>17</sup> Aiming to maintain a good oral health and achieving a high compliance of the volunteers during the study, this in situ model recruited students and professors from our dental school. Although a dental-related population is not representative of the general population,41 intricate instructions and lack of compliance may lead to exclusion of volunteers. In this study, despite six volunteers excluded from the study, only two were due to compliance issues (delivering absence). Nevertheless, the inclusion of 10 volunteers was in agreement with previous studies having demineralization as outcome.42 In this study, all volunteers were submitted to a highly cariogenic substance, which would put them at "high caries risk". However, demineralization did not occur in all groups, showing that other patient factors, e.g. bacterial composition, sugar consumption and saliva, were influencing such prevention, as previously described.20

This *in situ* study was valuable as it evaluated the inhibition of demineralization process<sup>43</sup> and allowed direct comparison between materials. The adhesive system with antibacterial and bioactive component (20% TAT) resulted in less total *Streptococci* and *S. mutans* growth, which might be attributed to the antibacterial properties of the adhesive and reduced filler size. Due to the study design, the demineralization of enamel may also have been influenced by individual habits, different oral pathogens within the biofilm, and material composition.<sup>20</sup>

#### **Conclusions**

As a conclusion, bonding brackets to enamel with adhesives containing triazine and niobium phosphate invert glass leads to inhibition of demineralization and/or contributes with the recovery of the enamel mineral content under adverse conditions of oral hygiene.

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