Influence of a Femtosecond Laser Surface Modification on the Fatigue Behavior of Ti-6Al-4V ELI Alloy

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The objective of this investigation was to evaluate the influence of surface modification by femtosecond laser (with average fluence of 0.6 J/cm² and scanning speed of 0.1 mm/s) on the fatigue resistance of Ti-6Al-4V ELI alloy. A significant reduction in the fatigue strength of the material modified by laser was observed. Residual tensile stresses generated during surface modification were negligible, presenting lower values than those found on the unmodified surface. Based on a recently developed and published prediction model, the reduction of the fatigue strength was ascribed to the surface roughness created during the laser treatment of the alloy. An evidence was that the fatigue crack nucleation occurred in the modified region, rather than at the edge of the rectangular specimens as in the untreated condition.

Keywords: Ti-6Al-4V ELI, surface modification, laser, femtosecond, fatigue.

1. Introduction

Titanium and its alloys, originally developed for aeronautical applications, have been increasingly used in applications as biomaterials because of their excellent mechanical strength, low modulus of elasticity, low density, high corrosion resistance, and the best biocompatibility among the metallic biomaterials. There are two main methods for fixation of the orthopedic implant to the bone: use of a cement with PMMA (polymethylmethacrylate) or modified implants surfaces (bio-passive and bio-active) to promote osseointegration ¹. The first method is commonly used in older patients with impaired ability to regenerate bone. Polished prostheses are used (usually stainless steel) and the result is an excellent primary fixation, i.e., no biological interaction between prosthesis/bone ².

The second method is based on the improvement of the long-term success of the implant/bone interface, that depends on the capacity to stimulate the osseointegration phenomenon, by altering the physical and/or chemical properties of the surface. The osseointegration is influenced by the following surface properties: morphology, topography, roughness, chemical composition, surface energy and wettability. Interactions between two or more properties are likely to happen and therefore to affect the implant stability, which plays a critical role for a successful osseointegration ³. Several techniques are used for this purpose and there are clinical advantages for their use as compared to the first method described ^{4,5}.

From the mechanical point of view, however, surfaces modified by conventional methods for improvement of osseointegration, such as plasma electrolytic oxidation ⁶, thermal oxidation and corundum grit blasting ⁷, can drastically reduce the fatigue resistance of prostheses, since, as it is well known, the fatigue behavior is strongly dependent on surface and near surface characteristics. The reason is that the fatigue property is typically affected by the increase in roughness, formation of notches or pores and/or emergence of residual stresses ⁸. Thus, the combination and balance between the improvement of osseointegration and mechanical behavior is a challenge for the development of orthopedic implants ⁹.

Advances in the techniques of surface modification and characterization, based on nanotechnology and its applications, indicate that modified surfaces at the nano-meter scale can promote higher osseointegration than surfaces modified by current techniques ¹⁰. The laser surface modification shows promise to improve the osseointegration since it permits precise control of parameters, geometrically defined surface features with controlled dimensions, and induces reduced mechanical and thermal damage. The femtosecond laser is particularly interesting since it uses pulses with duration of femtoseconds, which allows the creation of nano-sized features on a surface and reduces the occurrence of thermal damage ¹¹⁻¹³.

The objective of this investigation was to evaluate the influence of surface modification by femtosecond laser on the fatigue resistance of Ti-6Al-4V ELI alloy specimens, considering both the surface topography and changes induced by the heat input.

2. Materials and Methods

Dimensions of the fatigue test samples are shown in Figure 1 (according to ASTM F1160) were machined from 3 mm thick Ti-6Al-4V ELI (ASMT F136) plates maintaining the surface finish and microstructure of the initial rolled plates. Rectangular areas of $10 \times 4 \text{ mm}^2$ in the middle of the reduced section were modified by laser treatment. For the surface modification, a pulsed Yb:KYW laser was employed (Amplitude Systemes s-Pulse HP), with pulse duration lower than 500 fs and wavelength of 1030 nm. The pulse repetition rate was kept at 50 Hz and the scanning speed was approximately 100 μ m/s. The average power before and after the mirror were respectively 0.800 W and 0.770 W, with an average fluence of 0.6 J/cm².

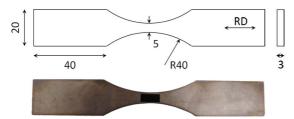


Figure 1. Illustration of the test specimen (dimensions in mm) and photograph of a treated sample. RD refers to the rolling direction.

The laser beam was focused by 100 mm focal length lens on a spot perpendicular to and at the specimen surface, with a diameter of $338 \pm 10 \mu$ m. The laser treatment was performed under standard air atmosphere by moving the specimens under the stationary laser beam with a constant scanning speed through a computer-controlled XYZ stage. To achieve complete surface coverage, consecutive laser tracks were partially overlapped by a lateral displacement of about 30% of the laser track width. All these parameters were chosen according to previous experience at Instituto Superior Técnico to produce a nanoscale modification consisting of nanoscale laser-induced periodic surface structures (LIPSS) overlapped onto microcolumns.

The roughness evaluation was carried out using both a contact perfilometer Mitutoyo SJ-201P, with two measurements in each of four samples, and a confocal laser scanning microscope (CLSM) Olympus Lext OLS 400. CLSM measurement was performed in a single specimen, chosen at random. The assessment of surface topography, the metallographic analysis of cross-sectional area and the fatigue fracture surface characterization were performed using a scanning electron microscope (SEM) FEI Quanta 400 FEG. With the same microscope, energy dispersive spectroscopy (EDS) by an Oxford INCA Energy 250 detector was employed to evaluate the oxygen content near the surface of the modified region.

Bending type fatigue tests were conducted in a Brasvalvulas BME 05 40 150 / AT MNB servo-hydraulic equipment, using the device illustrated in Figure 2 and a load applicator consisting of a roller straightened supported by self-aligning bearings. The frequency of the load application was 5 Hz and the ratio between the minimum and maximum load was 0.1. Two fatigue test programs involved seven non-treated (reference) and ten laser-modified samples, nearly uniformly replicated at four stress levels, resulting in replications of 43% and 60% for reference and modified samples, respectively. These levels of replication are suitable for research and development testing according to the ASTM E739.

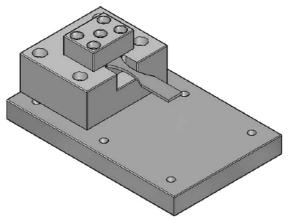


Figure 2. Device used in the bending fatigue tests.

The measurements of the in-plane surface stress component along the larger side of the selected rectangular areas of the laser modified and reference samples were carried out on a Bruker's D8-Discover X-ray diffractometer in Ψ experimental geometry (side inclination)¹⁴ with the use of Co K_{α} radiation, measuring the (114) diffraction line of α -Ti phase of samples. These radiation conditions provide nearly backscattering geometry for (114) peak's measurements (20 peak's position is about 158?). A collimated by a 1 mm circular slit X-ray beam was centered in the middle of the rectangular area of the tested samples. Each measurement consisted of a collection of (114) diffraction peaks corresponding to positive and negative values of ψ in the range from -60? to 60? with the $\Delta \psi$ step of 5?. The determination of the (411) peak positions employed a pseudo-Voigt function fit of the measured diffraction peaks corrected for background, absorption, Polarization-Lorenz factor, K_{α^2} contribution as implemented in the Stress V1.1 software from Bruker-AXS.

3. Results and Discussion

The samples were subjected to femtosecond laser nonstationary irradiation, with an energetic fluence of 0.6J/cm2, which did suffice for the formation of micro-columns, as shown in Figure 3. It is noted in Figure 4 a bimodal surface of nanoscale laser-induced periodic surface structures (LIPSS) covering all these micro-columns. The spatial periodicity of the LIPSS was approximately 700 nm, i.e., substantially lower than the equipment wavelength of 1030 nm. Typical of stationary irradiation, the LIPSS structure is usually formed with fluences near the melting threshold, more specifically when fluence is lower than the threshold fluence for microcolumns formation and larger than the melting threshold fluence. This difference could be explained by the formation of nanostructures during the first pulses of laser, which increase the real part of refractive index of the material ¹¹.

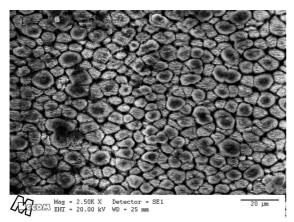


Figure 3. SEM micrograph of the overall appearance of microcolumns formed.

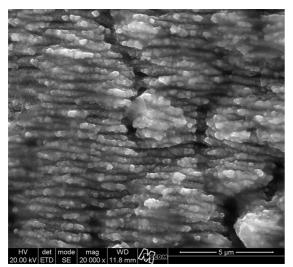
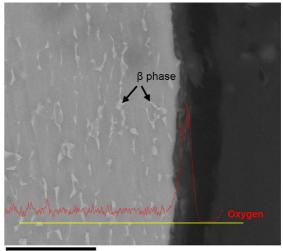


Figure 4. SEM micrograph of LIPSS covering all micro-columns.

During non-stationary irradiation, each point of the specimen is subjected to different energetic fluences, because the energy profile in cross section of the laser beam follows a Gaussian distribution and depends on, among other factors, the beam diameter, the average value of fluency and the scanning speed. Thus, the LIPSS are developed immediately after the formation of micro-columns, when the material is exposed to the lower energy intensity of the beam ^{11,12}. Due to the processing in air, modification by laser also induced the formation of a surface oxide, as shown in Figure 5. Depending on the parameters used in the equipment, different oxides such as rutile, anatase and even alumina can be expected ^{15,16}. It is known that the formation of these oxides provides higher corrosion resistance and enhances the wettability of the surface, an essential property in the process of osseointegration ¹⁶. The observation by SEM of cross sections of the specimen showed no severe microstructural changes on the alloy close to the modified surface.



10 µm

Figure 5. SEM micrograph of the cross-section showing the surface oxide layer.

This is an important issue to be addressed, because, from the decades of 1960-1970 on, it is recognized the strong influence of α -case formation on reducing the fatigue strength of Ti alloys. When heated in solid state, the surface of Ti-6Al-4V reacts with oxygen, which is an α -stabilizer element, resulting in a structure predominantly of α phase. Oxygen is soluble in Ti up to 3.5%wt. at 673K and has a significant hardening effect ¹⁷. The oxygen-enriched surface forms an α -case and allows oxygen to diffuse through the underlying matrix of the base alloy. Depending on the time and temperature, this diffusion layer can reach ~200 µm after isothermal heat treatment in air at 700°C for 500 hours ¹⁸. In investment cast parts, this layer can be even thicker and reach 500 μ m¹⁹. Such α -case is detrimental to Ti-6Al-4V due to its brittle nature, and can result in early surface cracks under cyclic tension²⁰. Therefore, in order to allow a reliable interpretation of the fatigue results, it is of utmost importance to identify the presence or absence of α -case.

By a careful observation of Figure 5, it is observed that no microstructural alterations occurred since the β -phase distribution was unchanged through the sample thickness. In addition, the EDS scan line on the cross-section showed that the oxygen content remained constant and only changed over the oxide layer. This endorses that no α -case was formed, regardless of the presence of the oxide layer, and that any change in the fatigue strength must not be ascribed to it. The formation of α -case is not expected due to the very fast cooling rates prevailing in the femtosecond laser processing (higher than 10⁶ K/s) ¹⁶. Although oxygen is available, the diffusion time is very short, in the range of 10⁻³s. The thickness of the α -case can be estimated by the following relationship ²¹:

$$\delta_{\alpha} = (D.t)^{1/2}$$

where *D* is the diffusion coefficient for oxygen in the β phase (7,98x10⁻¹² m²s⁻¹) and *t* is the time for diffusion. Considering t = 10⁻³s, which is a rough estimation for the cooling down from the melting temperature (~1730°C to ~500°C), the latter meaning the temperature below which the diffusion mechanism is negligible, the thickness of the α -case can be calculated as around 9 nm. In spite of the rough calculation of the possible α -case thickness, its size is indeed in the nanometer scale, thus justifying the impossibility of observing it with the available techniques. In this size scale, there is no related effect on the fatigue properties so far, and this influence can be safely excluded in this work to justify the fatigue performance.

The fatigue tests showed that, despite of the bending test type and of the device with self-compensating bearings in order to ensure alignment, all reference specimens showed fatigue crack nucleation at the edge. River patterns emanating from the point with an arrow, as observed in Figure 6, indicate that this is the probable nucleation site. On the other hand, all specimens with surface modified by femtosecond laser showed nucleation of fatigue crack in the middle third of the width, or approximately in the center of the modified surface, as shown in Figure 7. The accurate nucleation site is hardly distinguished in this case: although faintly seen, the river patterns denote the crack initiation in the aforementioned position.

Figure 8 shows the S-N curves obtained for the two conditions evaluated. The untreated material presented an approximated fatigue strenght of 725 MPa, whereas the laser-treated material presented a fatigue strenght of around 650 MPa. The dotted lines comprise the 95% confidence band

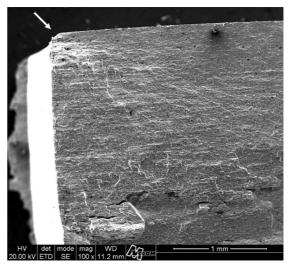


Figure 6. SEM micrograph of the fatigue initiation region of a reference sample. The arrow points at the crack initiation at the edge.

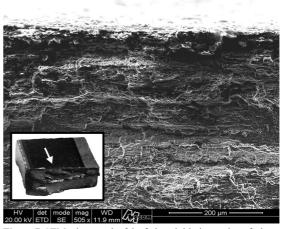


Figure 7. SEM micrograph of the fatigue initiation region of a lasertreated sample. The inset image is a macrograph of the fractured sample, and the arrow indicates the probable initiation site.

computed in accordance with the ASTM E739 standard. Since there is no intersection between the bands, it is possible to conclude that the difference in the fatigue behavior of both conditions is statistically significant. There is therefore an irrefutable deleterious influence of the femtosecond laser on the fatigue response of the material.

Due to the well known influence of surface residual stresses on the fatigue limit, measurements were conducted to determine their value on the surface of modified and reference samples. Figure 9 shows the curves obtained and the results at the geometric center of the samples. The residual stresses at the surface are very small and, moreover, with smaller values of the modified samples (around 20 MPa against 46 MPa of the unmodified material). Hence, these results cannot explain the smaller values for the fatigue strength of the laser modified samples.

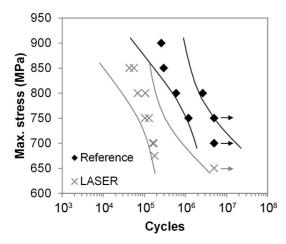


Figure 8. S-N curves for the untreated (reference) and laser-treated conditions.

The results of surface roughness of modified and reference samples are presented in Table 1. There is a difference in the results obtained with the techniques, although the standard deviation values indicate that such difference is not significant.

Table 1. Results of Rz roughness measurements (in $\mu m)$ for both surfaces.

Equipment	Reference	Laser	
Perfilometer	3.55 ± 0.71	7.55 ± 0.94	
CLSM	2.45 ± 0.71	$\boldsymbol{6.37 \pm 0.63}$	

It is well known, that the effect of roughness on the fatigue strength may be evaluated by the fatigue notch factor $K_{\rm f}$. This factor is essentially different from the monotonic concentration factor $K_{\rm t}$, since it depends on the material, and, below a certain tip radius of the notch, its effect decreases and becomes negligible. This factor may be calculated from a constant, typical of a certain material, which is determined experimentally from fatigue results of notched specimens, with known geometrical notches. This calculation for Ti-6AI-4V ELI was recently published by da Silva et al. ²², and thus a prediction method was established.

The differences of surface roughness obtained in the present work (Table 1) were analysed through this predition method, and the results are summarized in Table 2. For each roughness value, K_f was obtained in the aforementioned reference ²². The value of the fatigue limit expected with K_f

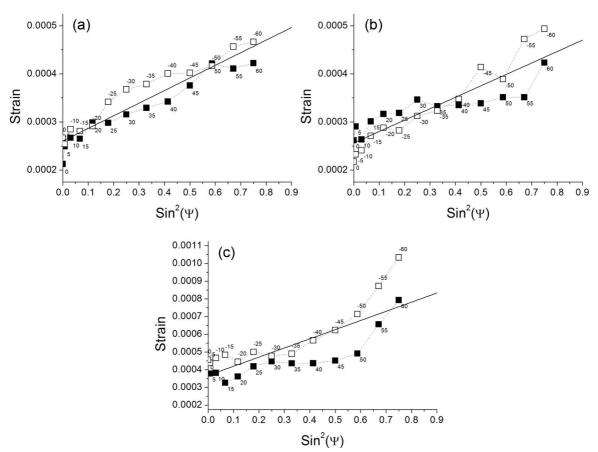


Figure 9. Curves of strain in function of $\sin^2(\Psi)$: (a) surface 1 of modified sample (residual stress of 23 MPa), (b) surface 2 of modified sample (residual stress of 21 MPa) and (c) surface of reference sample (residual stress of 46 MPa). White and black squares represent the Ψ angles used for the measurements (black are positive angles and white are negative angles).

= 1 (smooth surface) was taken as 850 MPa, the best value according to several previous measurements in cylindrical specimens of Ti-6Al-4V ELI alloy of the same production lot ^{8,23}. For the laser-treated samples, the expected and measured fatigue limits are noticiably in good agreement, with small errors of 0.7% and 6.2% respectively for the perfilometer and CLSM measurements. In the case of the reference samples, a strong reduction in the fatigue limit was observed, and this is due to the effect of the corner of the square cross section.

Table 2. Summary of the fatigue test results and analysis.

Surface	Equipment	$\begin{array}{c} R_{_z} \ (\mu m) \end{array}$	Theoretical K _f	L _f expected (MPa)	L _f measured (MPa)
Reference	Perfilometer	3.55	1.06	802	725
Reference	CLSM	2.45	1	850	725
Laser	Perfilometer	7.55	1.35	630	625
Laser	CLSM	6.37	1.28	664	625

In summary, the notches from the reference surface finish have a negligible effect; those resulting from laser treatment have a significant effect and the predictable fatigue resistance is consistent with the experimental results. Therefore, the diminished value of the fatigue resistance of treated specimens may be attributed to the notch effect of the laser treatment. As shown throughout the text, neither residual stress nor α -case formation influences the fatigue strength in the present study.

4. Conclusions

With the process parameters employed, the femtosecond laser provided a regular surface with a bimodal distribution of LIPSS (with around 700 nm of periodicity) and micro-columns. A surface oxide also resulted from the laser processing. However, the mechanical behavior under cyclic stresses was negatively affected, with a reduction in the fatigue resistance being observed, and must be considered in the design of a load bearing implant. As there was a negligible difference in the residual stresses among modified and non-modified surfaces, the deleterious effect on the fatigue response was ascribed to the increased roughness of the laser treated region, where crack nucleation always occurred after the surface modification.

5. Acknowledgements

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