

Blood contamination effect on shear bond strength of an orthodontic hydrophilic resin

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Received: November 25, 2009 - Modification: May 13, 2010 - Accepted: May 30, 2010

ABSTRACT

Objective: The aim of this study was to assess the impact of blood contamination on shear bond strength (SBS) and bond failure pattern of metallic brackets bonded using a new hydrophilic resin. Material and Methods: Eighty human premolars were randomly allocated into 4 groups (n=20) according to the bonding material and contamination pattern. GI: brackets bonded with the Transbond XT conventional system without contamination; GII: brackets bonded with the Transbond XT conventional system with blood contamination; GIII: brackets bonded with the Transbond Self Etching Primer and Transbond Plus Color without contamination; GIV: brackets bonded with the Transbond Self Etching Primer and Transbond Plus Color with blood contamination. The specimens were stored in distilled water at 37°C for 24 h and then submitted to SBS test at a crosshead speed of 0.5 mm/min. After bond failure, the enamel surfaces were observed under an optical microscope at 40x magnification. Results: Blood contamination decreased ($P<0.05$) shear bond strength when both the hydrophobic (GII) and the hydrophilic resin (GIV) were used. However, the bond strength of Transbond Color Change group was significantly higher ($P<0.05$) than that of the Transbond XT conventional system group under blood contamination condition. Under dry conditions no difference was observed between the hydrophobic and hydrophilic resin groups. Regarding the bond failure pattern, when blood contaminated the enamel, the adhesive remnant index (ARI) showed predominance of scores 0 and 1, which indicates low adhesion to enamel. Conclusions: Although there was a significant decrease in the shear bond strength for both adhesive systems under blood contamination, the hydrophilic system showed significantly higher bond strength than the hydrophobic resin adhesive. Therefore, it is advisable to use the hydrophilic resin under risk of blood contamination.

Key words: Orthodontic brackets. Shear strength. Dental bonding.

INTRODUCTION

The appearance of orthodontic fixed appliances has been revolutionized since Newman¹⁸ (1965) suggested an orthodontic use for the enamel direct bonding technique. Over the years a great deal of attention has been paid to improve the acid-etching technique, primers and adhesives. Traditional composite resin bonding materials present hydrophobic properties and require dry surfaces

to obtain clinically acceptable bond strength¹³. Thus, contamination during orthodontic bonding process is undesirable because it interferes on the adhesive and resin properties and causes failure on the adhesive interface.

A variety of clinical conditions forbid ideal isolation of the bonding site^{9,12}, especially around second molars or partially erupted and impacted teeth submitted to surgical exposure⁶. Saliva or blood contamination are considered the most

common reason for bond failure^{8,21,22} because when etched enamel becomes wet, most of the pores become plugged, and resin penetration is impaired, resulting in insufficient resin tags²¹. Thus, it would be advantageous the ability of bonding to enamel in a wet environment. For this reason, manufacturers introduced hydrophilic primers that promised successful bonding to a contaminated enamel surface. More recently, hydrophilic self-etching primers were developed to combine conditioning and priming agents into a single acidic primer, eliminating phases in the process¹⁷. These products have the advantage of a faster and simplified technique.

However, composite resins maintained hydrophobic characteristics. Currently, in an attempt to solve contaminating problems, manufacturers introduced Transbond Plus Color Change (3M Unitek, St. Paul, MN, USA), a hydrophilic composite resin.

Some researches^{7,10,12} have reported a decline in bracket bond strength as a result of blood exposure during bond. However, these studies used hydrophilic primer with hydrophobic adhesive resin and none have investigated whether there was any difference in bond strength values when hydrophilic adhesive resin is associated with hydrophilic primer.

The purpose of this study was to evaluate the efficacy of the Transbond Plus Color Change associated with Transbond Self Etching Primer used to bond metallic brackets under blood contamination condition.

MATERIAL AND METHODS

A total of 80 human extracted premolars from the teeth bank of Pontifical Catholic University of Paraná (PUCPR), Brazil, were used for this investigation. The roots were removed and the crowns were embedded in autopolymerized acrylic resin so that the buccal surface of each tooth was parallel to the base of the polymer.

Before bracket bonding, the buccal surface of each premolar was cleaned with slurry of water and pumice (Quimidrol Ltda., Joinville, SC, Brazil) for 10 s with a rubber cup on a low-speed handpiece. The enamel surface was rinsed with water to remove pumice and debris and dried with an oil-free air stream for 10 s. Eighty specimens were randomly allocated to 4 different groups (n=20), according to Figure 1.

Orthodontic stainless-steel standard premolar brackets with a 0.022-inch slot and 14.28 mm² of bonding area (3M Unitek, St. Paul, MN, USA) were bonded to the dental enamel on the G1 and G2 using the Transbond XT[®] system (3M Unitek). The enamel surface was etched with 37% phosphoric acid for 15 s, rinsed with distilled water for 10 s, air-dried

for 10 s and conventional primer Transbond XT was applied. Then, the bracket with adhesive resin Transbond XT was positioned on the enamel surface and pressed with 400 kgf, using a dynamometer (ETM). Excess of adhesive was removed around the bracket base and the adhesive was light cured by an Ortholux XT lamp (3M Unitek, St. Paul, MN, USA) on each interproximal side for 10 s.

The brackets on G3 and G4 were bonded with Transbond Self Etching Primer (SEP, 3M Unitek) associated with the composite resin Transbond Plus Color Change Adhesive (3M Unitek), which presents hydrophilic characteristic. Self-etching primer was pressed in contact to the enamel surface for 10 s. The adhesive resin Transbond Plus Color Change was inserted to the bracket base, the bracket was positioned on the enamel and pressed with 400 Kgf, using a dynamometer. The excess adhesive was removed around the bracket and the adhesive was light-cured with an Ortholux XT lamp (3M Unitek) on each interproximal side for 10 s.

The specimens of G1 and G3 were bonded without contamination and of G2 and G4 under blood contamination. The contamination was performed immediately before Transbond XT paste and Transbond Plus Color Change application. To achieve reproducible conditions, the teeth in the blood-contaminated groups were treated with fresh human blood from one female donor and blood was applied with a brush into the buccal surfaces for 10 s to permit full hydration of the surface.

Shear bond strength test

After bonding, all samples were stored in distilled water at 37°C for 24 h and then tested in a shear mode on a universal testing machine (EMIC DL 500, EMIC, São José dos Pinhais, PR, Brazil). Specimens were secured in the lower jaw of the machine so that the bonded bracket base was percentile to the shear force direction. Specimens were stressed in an occlusogingival direction at a crosshead speed of 0.5 mm *per* minute. The maximum load necessary to debond or initiate bracket fracture was recorded

Group	Contamination	Adhesive System
G1	None	Transbond XT primer and Transbond XT
G2	Blood	Transbond XT primer and Transbond XT
G3	None	Transbond Self Etching primer and Transbond Plus Color
G4	Blood	Transbond Self Etching primer and Transbond Plus Color

Figure 1- Experimental groups

Table 1- Descriptive statistic for shear bond strength

Groups	Contamination	Composite Resin	Mean (MPa)	SD
G1	None	Transbond XT	8.94	±3.97 ^A
G2	Blood	Transbond XT	2.15	±1.22 ^B
G3	None	Transbond Plus	9.91	±2.23 ^A
G4	Blood	Transbond Plus	5.24	±2.45 ^C

Different letters indicates statistical difference for Games Howell test $p < 0.05$. SD= standard deviation

Table 2- Descriptive statistics for Adhesive Reminiscent Index (ARI)

Groups	n	Contamination	Resin	Scores ARI (%)			
				0	1	2	3
G1	20	None	Transbond XT	40	30	10	20
G2	20	Blood	Transbond XT	90	10	0	0
G3	20	None	Transbond Plus	25	30	25	20
G4	20	Blood	Transbond Plus	55	25	15	5

in Newtons and then converted into MPa.

After bond failure, bracket bases and the enamel surfaces were examined under a stereomicroscope (Olympus Optical Co., Shinjuku, Tokyo, Japan) at 10x magnification. The adhesive reminiscent index (ARI) was used to assess the amount of adhesive left on the enamel surface¹.

Statistical analysis

Statistical calculations were performed by the Statistical Package for the Social Sciences Version 15.0 software (SPSS 15.0, SPSS Inc., Chicago, IL, USA) for Windows. In addition to standard descriptive statistical calculations (mean and standard deviation), Kolmogorov-Smirnov and Levene test were performed.

The one-way ANOVA was carried out for the comparison of groups. In the evaluation of subgroups, a Games-Howell multiple comparison test was performed. The statistical significance level was established at $P < 0.05$.

RESULTS

Shear bond strength

ANOVA demonstrated that material and contamination altered shear bond strength. The hydrophobic conventional Transbond XT system revealed a significant ($P < 0.05$) decrease in SBS after blood contamination. A significant ($P < 0.05$) decrease in SBS could also be detected after blood contamination using Transbond Plus Color Change (Table 1).

The bond strength of Transbond Plus Color Change group was significantly higher than for Transbond XT group under blood contamination condition ($P < 0.05$). Under dry conditions no

difference was observed between the hydrophobic and hydrophilic adhesive resin groups (Table 1).

Adhesive reminiscent index (ARI)

Groups without contaminants demonstrated balanced distribution of ARI scores. When blood contaminated the enamel, there was a predominance of ARI scores 0 and 1, indicating low adhesion to enamel. The frequency of ARI scores is presented in Table 2.

DISCUSSION

The difficulty of orthodontic bracket bonding is its semi-permanent nature. The bond strength should be sufficiently high to resist accidental debonding during treatment, but low enough to remove the bracket from the tooth without generating excessive force which might damage the periodontal tissue or the enamel surface¹⁹. Bracket undesirable debonding often results from failure in the bonding technique, low retentiveness of bracket bases and masticatory forces¹⁵. It might delay treatment finishing and increase the costs of fixed orthodontic appliances²⁰. In an attempt to minimize these problems, the dental industry has been incessantly developed hydrophilic bonding materials capable of withstanding the Orthodontic and masticatory forces.

It is important to choose the appropriate material for bonding in orthodontics, regarding factors such as resistance, longevity and easy to remove without damaging the enamel surface. Those *in vitro* characteristics support the clinical practice through the shear bond strength and ARI scores²³. The correlation between *in vitro* and *in vivo* adhesive/resin interfaces and bond strength tests

has been shown elsewhere²⁵. It is a common belief that the clinically adequate SBS for a stainless steel bracket to enamel should be 6-8 MPa^{4,11,19}.

Moisture contamination is still a problem during direct bonding of orthodontic brackets, especially while bonding posterior teeth as well as surgically exposed teeth, so the saliva and the blood are the principal contaminant agents in this process²¹.

Previous studies demonstrated decrease on bond strength when self etching primers were used under dry conditions^{3,16,25,26}. In contrast, Webster, et al.²⁴ (2001) concluded that uncontaminated enamel surfaces resulted in the highest bond strengths for hydrophilic and hydrophobic adhesives. In the present study, no significant difference between conventional Transbond XT system and SEP/Transbond XT Color Change could be observed under dry conditions and both showed clinical satisfactory values of SBS.

The impact of blood contamination on bond strength has been tested before. The results of SBS tests indicate that human blood seems to be a great barrier for the adhesives to penetrate. This might be of concern when bonding orthodontic buttons or brackets during surgical exposure of impacted teeth. Often glass ionomer cements (GICs) are used for bonding brackets to the surface of unerupted teeth, because of their enhanced curing in a wet environment²². However, Reddy, et al.²² (2003) found that the beneficial wetting phenomenon of GICs is not achieved after blood contamination during curing. They stated that, without contamination, composite resins have greater bond strength than resin-reinforced GICs. After blood contamination, both materials showed a significant decrease in bond strength²².

Previous studies have demonstrated a decrease in the bond strength due to blood contamination during the bracket bond process^{7,10,12}. However these studies used the hydrophilic primer with a hydrophobic resin. In the present study a hydrophilic adhesive resin was tested associated to the self etching primer under blood contamination, it was possible to observe higher values than those observed when the hydrophobic resin was used.

In the present study, blood constituted a physical barrier preventing the mechanical retention of the adhesive to the etched tooth and the hydrophilic adhesive resin do not solve this problem. Thus, even with the application of a self-etching primer associated with a hydrophilic resin, the bond strength of bracket bonded under blood contamination is not capable to withstand clinical forces. Yet, the hydrophilic system showed significantly higher bond strength than the hydrophobic resin adhesive. Therefore, under a risk of blood contamination it is advisable to use the hydrophilic resin.

Relating to the bracket debonding, Bishara, et

al.² (1999) stated that when the failure occurs at the enamel/adhesive interface there is an increased risk of enamel fracture. However, if the failure occurs in the interface adhesive/bracket, the enamel is often preserved^{5,14,25}. When blood contaminated the enamel, ARI showed predominance of scores 0 and 1, indicating low adhesion to enamel, thus the adhesives used in this investigation do not present risk to enamel integrity. Moreover, this result indicates a minimum amount of adhesive remaining on teeth, clinically, this would imply a minimal clean-up time after debonding and no risk to damage the dental enamel.

Under dry conditions hydrophobic primers and resins can be applied, but if contamination during bonding is expected, we recommend the use of a hydrophilic primer associated with a hydrophilic resin. However, blood contamination is a serious problem for bond strength, so this type of contamination must be avoided during brackets bonding process.

CONCLUSIONS

There was no significant difference in the bond strength of Transbond XT and Transbond Plus Color Change under dry conditions.

Transbond XT and the Transbond Plus Color Change showed clinically acceptable bond strength for brackets bonded to dental enamel under dry conditions.

Blood contamination decreased the shear bond strength of orthodontic brackets bonded with Transbond XT hydrophobic adhesive resin and with the hydrophilic adhesive resin Transbond Plus Color Change.

Under blood contamination, the hydrophilic resin Transbond Plus Color Change associated to the Self Etching Primer led to significantly higher bond strength than the conventional Transbond XT system.

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