

Degree of conversion of a flowable composite light-activated through ceramics of different shades and thicknesses

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Abstract

The cementation of thin ceramic veneers employing fluid light-activated resin-based materials is a common procedure in the dental practice. **Aim:** To evaluate the influence of ceramic thickness and shade on the degree of conversion (DC) of a flowable light-activated material. **Methods:** flowable resin composite (Tetric N-Flow – shade A1) was light-activated through ceramic discs of two shades (IPS Classic - A1 and A3) in three thicknesses (0.5, 0.7 and 1.0 mm). For control, the resin composite was light-activated without ceramic interposition. DC was evaluated by FTIR (n=5). Data were analyzed by one-way ANOVA and Dunnett's T3 test ($\alpha=0.05$). **Results:** Statistically significant differences between groups were observed ($p<0.001$). Control group (without the interposition of ceramic) showed the highest mean for DC (71.9 ± 1.7). Considering the interposed ceramic disc groups, the highest DC values were obtained when 0.5 and 0.7 mm A1 ceramics were used (64.6 ± 1.2 and 64.4 ± 1.5 , respectively) and the lowest DC values were obtained for 0.7 and 1 mm A3 ceramics (61.74 ± 0.9 and 62.0 ± 1.9 , respectively). **Conclusions:** No flowable resin composite group with interposing ceramics reached a DC similar to the control group.

Keywords: composite resins; polymerization; dental materials; ceramics.

Introduction

Dental ceramics have become well known due their great esthetic quality, capacity of mimicking the dental structure, high wear and staining resistances, color stability and biocompatibility¹. Conversely, it is well established that ceramic veneers should be firmly fixed to dental structure in order to achieve better clinical longevity. Thus, despite the superior physical-chemical properties of ceramic materials when compared to other dental esthetic restorative materials, such as resin composites, the clinical success of ceramic restorations depends on the properties of the cementation material as well as the cementation technique².

Luting materials are considered clinically acceptable if they present appropriate resistance to solubilization, high adhesion to dental substrates, high strength under tension, good manipulative properties, and biocompatibility in the oral environment and to the dental tissues²⁻³. In order to improve these properties, the material should be properly polymerized. Thus, one of the most important aspects related to the characteristics of resin-based materials is the

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polymerization level or degree of conversion (DC) of monomer chains into polymers^{4,5}. DC is important because properties such as strength, color stability and biocompatibility are closely related to it⁶⁻⁸. The biocompatibility is related to the concept that unreacted monomers have cytotoxic potential in contact with biological tissues⁹. Thus, since the physical/chemical properties of resin-based cements are related to how the polymerization occurs, it is important to study and understand the factors that may influence the DC, such as thickness and color of the ceramic material interposed between the light source and the resin cement.

In the case of the cementation of ceramic veneers, the use of light-activated resin-based materials has increased due to the working time control¹⁰. This clinical advantage, however, should not be the determinant factor for material choice in veneer cementation due to the possible attenuating effect provided by thickness, opacity and shades¹¹⁻¹³. Additionally, the type and microstructure of the interposing ceramic material are significant factors in the properties of polymerized luting materials¹⁴. In general, the use of these light-activated cements should be limited to some clinical situations such as inlays, veneers and onlays, in which the thickness and shade of restoration do not affect the ability of light to reach and activate the cement¹⁵.

Considering the light-activated resin cements for veneers and onlays cementation, the polymerization quality is related to several factors such as photo-activation light source, irradiance, irradiation time, material composition and light attenuation caused by ceramic^{11,13-14,16-18}. It was observed that the transmittance of light through ceramic decreases as function of the material interposed between the light source and the resin cement¹⁹.

Furthermore, for a single ceramic material with different shades and thickness, it can be hypothesized that the polymerization may vary due to differences in the transmission of photons through the ceramic. Therefore, the clinical performance would be determined by the amount of light transmitted through the restoration that reaches the resin-based cement. Thus, the aim of this study was to evaluate the influence of ceramic color and thickness on the DC of a flowable light-activated resin composite. The working hypothesis was that the shade and thickness of interposing ceramic material influence DC.

Material and methods

The materials used in this research are in Table 1. Feldspathic ceramic discs (IPS Classic, Ivoclar Vivadent,

Schaan, Liechtenstein) 12 mm diameter and 0.5, 0.7 and 1.0 mm thickness were prepared with the shades A1 and A3. All spacers were fabricated according to the manufacturer's instructions. The thickness was measured by a digital caliper (Starret, Jiangsu, China) with 0.01 mm accuracy.

For DC evaluation, a portion of approximately 0.05 g of the uncured shade A1 Tetric N-Flow (Ivoclar Vivadent, Schaan, Liechtenstein) flowable resin composite was dispensed onto a plastic film. Another plastic film was placed over the material and the set was pressed with a pneumatic press (Shimadzu, Kyoto, Japan) at 10 kN to obtain a thin film approximately 0.1 mm thick and 20.0 mm diameter (n=5). These composite films were light-activated through different interposed ceramic spacers with a 1200 mW/cm² LED curing light (Radii-Cal, SDI Limited, Bayswater, Australia) for 45 s. The light intensity was determined before the beginning of the experiments by a radiometer (Demetron, Kerr, Middleton, WI, USA) without the interposition of ceramic disks.

The samples were subjected to Fourier transformed infrared spectroscopy (FTIR) with a resolution of 4 cm⁻¹ and 32 scans ranging from 4,000 to 800 cm⁻¹. The absorption peaks of aromatic double bonds at 1608 cm⁻¹ (Abs 1608) and aliphatic double bonds at 1636 cm⁻¹ (Abs 1636) were recorded before and after the light-activation. Five measurements were performed for each condition.

The ratio between Abs 1636 and Abs 1608 was calculated for both cured and uncured materials. The percentage of remaining double bonds (RDB) was determined according to the formula:

$$\%RDB = (\text{Abs } 1636/\text{Abs } 1608 \text{ for cured resin}) \times 100 / (1636 \text{ Abs}/\text{Abs } 1608 \text{ for uncured resin})$$

The percentage of the degree of conversion of double bonds (DC) was calculated by the following formula:

$$\%DC = 100 - \%RDB$$

Data were submitted to one-way ANOVA. Multiple comparisons were performed using the Dunnett's T3 test. A global level of 0.05 significance was set.

Results

The DC mean values and standard deviations for the flowable resin light-activated through ceramic of different shades and thicknesses are shown in Table 2. Statistically significant differences were observed between groups (p<0.001). The control group (without interposition of ceramic) showed the highest mean percentage of DC (71.9±1.7). The lowest DC values were obtained for the 0.7

Table 1 - Materials used in the study.

Material	Type	Composition
Tetric N-Flow	Flowable resin composite	36 wt.% dimethacrylate (including TEGDMA), 63 wt.% fillers (barium glass, ytterbium trifluoride, highly dispersed silica and mixed oxide) and 1 wt.% catalysts, stabilizers and pigments. The total content of inorganic fillers is 39 vol.%. The particle size of inorganic fillers is between 40 and 3000 nm
IPS Classic	Feldspathic ceramic	SiO ₂ , BaO, Al ₂ O ₃ , CaO, CeO ₂ , Na ₂ O, K ₂ O, B ₂ O ₃ , MgO, ZrO ₂ , P ₂ O ₅ , TiO ₂ , and pigments (composition according to the Material Safety Data Sheet)

Table 2 - Mean values and standard deviations for DC. Different superscript letters represent statistically significant differences ($p < 0.05$).

Ceramic shade	Thickness (mm)	DC* (in %)
-	Control (without ceramic interposition)	71.9±1.7 ^a
A1	0.5	64.6±1.2 ^b
	0.7	64.4±5.0 ^{bc}
	1.0	62.7±4.7 ^{bc}
A3	0.5	62.7±1.4 ^{bc}
	0.7	61.7±0.9 ^c
	1.0	62.0±1.9 ^c

*DC degree of conversion

and 1 mm A3 ceramics (61.7 ± 0.9 and 62.0 ± 1.9 , respectively).

Discussion

This study confirmed the hypothesis that the shade and thickness of interposing ceramic material would influence the DC. Although no flowable resin composite group with interposing ceramics reached DC similar to the control group, little difference in the DC was observed when ceramics of different thicknesses and shades were compared. Possible explanations for this result are the high irradiance of the LED curing light used in this study, the reduced thickness of the ceramic veneers (up to 1 mm) and the thin films of flowable resin composite used to determine the DC. Thus, the possible attenuating effect of light by ceramic interposition was not sufficient to negatively affect DC.

It should be noted that only one feldspathic ceramic was evaluated in the present study. Ceramic systems with different levels of opacity are commercially available, and DC results could be different if ceramics presenting other opacities and microstructures were evaluated. More opaque ceramics tend to absorb more light, which would decrease the DC of light-cured resin-based materials²⁰. It has been reported that the DC of resin-based materials may change considerably as function of the type and opacity of the interposing ceramics¹³⁻¹⁴.

Another aspect to be addressed is that one single shade of flowable resin composite was evaluated. As recently observed, the shade is an important factor for the development of mechanical properties of resin-based cements. Darker shades may show inferior properties than the lighter ones²¹. Thus, the results of the present study could be different if other shades of resin composite (i.e. darker or bleached teeth) were evaluated. Additionally, the composition and irradiation time are important factors that influence DC of resin composites²²⁻²³. It should be noted that, according to the manufacturer, Tetric N-Flow is a radiopaque nano-hybrid light-activated flowable resin composite indicated for adhesive cementation of translucent ceramic and composite resin indirect restorations. Although the resin composite evaluated in the present study is indicated for the cementation of ceramic restorations, other light-activated materials (i.e.

the so called “veneer cements”) have been indicated for the cementation of thin veneers¹⁰ and also have shown good DC results when light-activated through ceramic materials¹³⁻¹⁴.

As seen in Table 2, the similar results for DC in most groups indicate that the shade and thickness of the evaluated interposed ceramic veneers did not influence the polymerization of the flowable resin composite. This result shows that a light-activated flowable resin may be used to fix minimum thickness ceramic veneers without a great effect on the DC level. This result is in agreement with another study that used the same method of the present study, in which the DC was not affected when 1.5-mm-thick ceramics were interposed¹³. Similar results were also observed by Cho et al.¹¹ (2015).

Other important factors to be considered are the exposure time and interposed ceramic opacity. Archegas et al.²⁰ (2011) observed that opaque ceramic resulted in lower degree of conversion, hardness and elasticity modulus of resin-based cements. An exposure time of 120 s produced higher degree of conversion values for all materials, regardless the opacity of the ceramic. Moreover, the exposure of 120 s promoted higher hardness and modulus of elasticity values than those obtained when the cements were light-activated for 40 s. Thus, the results of the present study could be different if longer light-activation times were used. It should be noted that, although the manufacturer of the resin composite evaluated in the present study recommends a 10-s light-activation time when a curing device with irradiance higher than 1000 mW/cm² is used, a 45-s light-activation time was used instead. This increased irradiance (1200 mW/cm²) and light-activation time (45 s) could have reduced the attenuation of light caused by the evaluated ceramics.

Besides the DC, it should be noted that the clinical longevity of all-ceramic restorations includes other factors, such as the used adhesive system, the mechanism of polymerization, the polymerization unit, and the microstructural characteristics and thickness of the ceramic material²⁴. For this reason, other studies should be conducted addressing the long-term behavior of light-activated resin cements cured through ceramics when different protocols of adhesive system application are employed.

There was no statistically significant difference between the evaluated thickness and shades, except when comparing 0.5 mm A1 and 1.0 mm A3 ceramics. These results indicate that this flowable resin may be used to cement minimum thickness laminate ceramic veneers without great impact on the conversion degree. Nevertheless, no flowable resin composite group with interposing ceramics reached a DC similar to the control group. It may be concluded that the shade and thickness of interposing glass-ceramic did not influence the DC of a flowable resin composite when ceramic was interposed.

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